

# **UNIVERSITI PUTRA MALAYSIA**

EFFECT OF WATER RATIO AND AGING TIME ON GLASS IONOMER CEMENT DERIVED FROM CALCIUM FLUOROALUMINOSILICATE-BASED GLASS

# MOHAMMAD ZULHASIF AHMAD KHIRI

ITMA 2022 7



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By

# MOHAMMAD ZULHASIF AHMAD KHIRI

Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia, in Fulfilment of the Requirements for the Degree of Doctor of Philosophy

October 2021

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#### DEDICATIONS

To my beloved parents, My inspiration father, Ahmad Khiri Takim My lovely mother, Zainun Musa Thank for your unlimited support and encouragement

To my wife, Fathiah Syazana and her family, For make my spiriting up throughout my studies journey until the end Thank for your thousand love and care

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Without all of them, this great success would not be possible Thank you everyone Abstract of thesis presented to the Senate of Universiti Putra Malaysia in fulfilment of the requirement for the Degree of Doctor of Philosophy

### EFFECT OF WATER RATIO AND AGING TIME ON GLASS IONOMER CEMENT DERIVED FROM CALCIUM FLUOROALUMINOSILICATE-BASED GLASS

By

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October 2021

Chair : Khamirul Amin Matori, PhD Institute : Nanoscience and Nanotechnology

Glass ionomer cement (GIC) is produced from a reaction between calcium fluoroaluminosilicate (CFAS) glass powder and polyacrylic acid (PAA). These kinds of cement are widely used primarily in dentistry for a long time ago for various applications such as adhesive and tooth restorative. In this research, the GIC is designed to perform good in mechanical and antibacterial properties. CFAS glass system is seen as a suitable combination due to its structure similar with natural tooth and ability to release fluoride ions for inhibiting the bacterial growth. The compound of SiO<sub>2</sub> and CaO in the glass system have been replaced by waste materials to achieve the usability of waste materials in this research. Soda-lime-silica (SLS) glass and clam shell (CS) are used to act as SiO<sub>2</sub> and CaO sources. The SLS-CS-CaF<sub>2</sub>-Al<sub>2</sub>O<sub>3</sub>-P<sub>2</sub>O<sub>5</sub> glass system was used to synthesized CFAS glass by the conventional melt-quench technique and act as a based-glass in the fabricating GIC. In this study, GIC B5 [25SLS-15CS-20CaF<sub>2</sub>-20Al<sub>2</sub>O<sub>3</sub>-20P<sub>2</sub>O<sub>5</sub>] with initial ratio of water at 1.2 revealed as the optimum sample based on the physical, structural, mechanical and antibacterial properties. From the mechanical results, the highest Vickers microhardness of GIC B5 is 191.33 HV while the highest compressive strength is 119.14 MPa at 28 days of aging time. Besides that, fluoride release by the GIC B5 was found directly proportional to the aging time between 1 to 28 days and recorded range from 74.62-194.82 ppm. The GIC also shows the antibacterial activity recorded the average diameter of the inhibition zone range between 19.33 and 28.00 mm. The antibacterial activity of GIC shows it is related to the fluoride ion release. It can be concluded that the fluoride release by GIC to the agar medium causes the inhibition of bacteria (S. mutans). Therefore, the GIC derived from CFAS glass in this study has high potential in dental material applications especially GIC B5 sample due to its good physical, structural and mechanical properties as well as its antibacterial activity.

Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Doktor Falsafah

### KESAN NISBAH AIR DAN MASA PENUAAN SIMEN IONOMER KACA YANG BERASASKAN DARI KACA KALSIUMFLUROALUMINOSILIKAT

Oleh

### MOHAMMAD ZULHASIF AHMAD KHIRI

Oktober 2021

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Simen ionomer kaca (GIC) atau dikenali sebagai simen polialkenoat kaca dihasilkan daripada tindak balas antara serbuk kaca kalsium fluoroaluminosilikat (CFAS) dan asid poliakrilik (PAA). Simen jenis ini banyak digunakan terutamanya dalam bidang pergigian sejak dulu untuk pelbagai aplikasi seperti pelekat dan pemulihan gigi. Dalam penyelidikan ini, GIC dirancang untuk memberikan sifat mekanikal dan sifat antibakteria yang baik. Sistem kaca CFAS dilihat sebagai kombinasi yang sesuai kerana strukturnya yang serupa dengan gigi semula jadi dan mempunyai keupayaan untuk melepaskan ion fluorida bagi menghalang pertumbuhan bakteria. SiO<sub>2</sub> dan CaO dalam sistem kaca telah digantikan dengan bahan buangan untuk mencapai kebolehgunaan bahan buangan dalam penyelidikan ini. Kaca soda-kapur-silika (SLS) dan shell clam (CS) masing-masing digunakan untuk bertindak sebagai sumber SiO<sub>2</sub> dan CaO. Sistem kaca SLS-CS-CaF<sub>2</sub>-Al<sub>2</sub>O<sub>3</sub>-P<sub>2</sub>O<sub>5</sub> digunakan untuk mensintesiskan kaca CFAS dengan teknik peleburan peleburan konvensional dan bertindak sebagai gelas berdasarkan pembuatan GIC. Dalam kajian ini, GIC B5 [25SLS-15CS-20CaF<sub>2</sub>-20Al<sub>2</sub>O<sub>3</sub>-20P<sub>2</sub>O<sub>5</sub>] dengan nisbah awal air pada tahap 1.2 dinyatakan sebagai sampel optimum berdasarkan sifat fizikal, struktur, mekanikal dan antibakteria. Dari hasil mekanikal, kekerapan mikro Vickers tertinggi GIC B5 ialah 191.33 HV sementara kekuatan mampatan tertinggi ialah 119.14 MPa pada 28 hari masa penuaan. Selain itu, pelepasan fluorida oleh GIC B5 didapati berkadar terus dengan masa penuaan antara 1 hingga 28 hari dan direkodkan dari julat 74.62-194.82 ppm. GIC juga menunjukkan aktiviti antibakteria mencatatkan purata diameter julat zon perencatan antara 19.33 dan 28.00 mm. Aktiviti antibakteria GIC menunjukkan ia berkaitan dengan pembebasan ion fluorida. Dapat disimpulkan bahawa pembebasan fluorida oleh GIC ke medium agar menyebabkan perencatan bakteria (S. mutans). Oleh itu, GIC dari kaca CFAS dalam kajian ini mempunyai potensi yang tinggi dalam aplikasi bahan pergigian terutama sampel GIC B5 kerana sifat fizikal, struktur dan mekanikalnya yang baik berserta juga dengan ciri aktiviti antibakterianya.

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This thesis was submitted to the Senate of Universiti Putra Malaysia and has been accepted as fulfilment of the requirement for the degree of Doctor of Philosophy. The members of the Supervisory Committee were as follows:

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# LIST OF ABBREVIATIONS AND SYMBOLS

	CS	Clam shell
	SLS	Soda–lime–silica
	НА	Hydroxyapatite
	FA	Fluorapatite
	CaCO <sub>3</sub>	Calcium carbonate
	CaO	Calcium oxide
	Ca(OH) <sub>2</sub>	Calcium hydroxide
	SiO <sub>2</sub>	Silica
	CaF <sub>2</sub>	Calcium fluoride
	Al <sub>2</sub> O <sub>3</sub>	Aluminium oxide
	P <sub>2</sub> O <sub>5</sub>	Phosphorus pentoxide
	Na <sub>2</sub> O	Sodium oxide
	CaAl <sub>2</sub> Si <sub>2</sub> O <sub>8</sub>	Anorthite
	3Al <sub>2</sub> O <sub>3</sub> ·2SiO <sub>2</sub>	Mullite
	Ca <sub>5</sub> (PO <sub>4</sub> ) <sub>3</sub> (OH)	Hydroxyapatite
	Ca <sub>5</sub> (PO <sub>4</sub> ) <sub>3</sub> F	Fluorapatite
	CFAS	Calcium fluoroaluminosilicate
	РАА	Polyacrylic acid
	GIC	Glass ionomer cement
	CaP	Calcium phosphate
	wt.	Weight
	wt.%	Weight percentage
	a.u.	Arbitrary unit
	Ppm	Parts per million

rpm	Revolutions per minute
Mm	Micrometer
$T_{g}$	Glass transition temperature
Tc	Glass crystallization temperature
T <sub>m</sub>	Glass melting temperature
V <sub>m</sub>	Molar volume
MPa	Megapascal
Kgf	Kilogram force
F	Force
ρ	Density
H <sub>v</sub>	Vickers hardness
XRF	X-ray fluorescence
XRD	X-ray diffraction
FTIR	Fourier transforms infrared
TGA	Thermal gravimetric analysis
DSC	Differential scanning calorimetry
FESEM	Field emission scanning electron microscopy
EDX	Energy dispersive X-ray
ISO	International Organization for Standardization
S. mutans	Streptococcus Mutans

### **CHAPTER 1**

#### **INTRODUCTION**

### 1.1 General Introduction

This chapter focus on the introduction of the research background of the biomaterial, Calcium Fluroaluminosilicate (CFAS) glass derived from vitreous waste, Fluorapatite (FA) and Glass Ionomer Cement (GIC). The vitreous wastes such as Soda–Lime–Silica (SLS) glass and Clam Shell (CS) are used in these studies to synthesized CFAS glass and then fabricated the GIC for a potential material used in dental material application. The specific characteristic of GIC is needed to ensure the materials can function in excellent condition for dentistry. Thus, detailed information about the fabrication and uses of the GIC is explained to ensure the objectives of the studies are successful at the end of the research.

### 1.2 Research Background

Biomaterials are referred to as biological or synthetic materials that have replaced any defective part of the human body, such as cell tissue, organs and body function, by means of an implantation method. Many researchers have defined biomaterials in specific ways in terms of biological content. According to the American National Institute of Health, the term biomaterials is defined as any substance or combination of substances, other than drugs, of synthetic or natural origin, which may be used for any period of time which increases or replaces, in part or in whole, any tissue, organ or function of the body in order to maintain or improve the quality of life of the individual (Bergman and Stumpf, 2013). Biomaterials must be biofunctional and biocompatible in order to perform the specific function of the host, either as implants or devices (Patel and Gohil, 2012). Biofunctional term is defined as the compensation for loss of function in diseased or damaged tissues, the complete replacement of the function of such tissues or the use for diagnostic purposes (Hudecki et al., 2019). According to Williams (1987), biocompatibility in terms of implantable means any material that has the ability to respond appropriately to the host in a specific application without harm occurring in the surrounding area. The use of biomaterials is currently widely used in various applications such as tissue, orthopedic and dental engineering applications. Biomaterials are usually produced in different types of materials, such as natural, glass, ceramic, metallic and polymer, depending on their specific function in medical applications (Shackelford, 1996).

Biomaterials can be categorized into three main functions, namely inert, reactive and resorbable (Hulbert et al., 1982). Bioinert materials have high chemical stability that is not triggered by a reaction or interacts with a biological reaction. Bioinert materials have high chemical stability that does not initiate a response or interact when introduced into a biological system (Hulbert et al., 1982; Yamamuro, 2004). Simply put, the introduction of bioinert material into the biological system, such as the body, will not cause the host to react. On the other hand, bioactive materials can be defined as a material that shows

reactivity to the biological effect, including interfacial bonding, and allows the tissue to ingest into the surrounding cells. While bioresorbable materials can be explained as a chemical reaction by dissolving materials to the body's host, and then absorbed by the body (Hulbert et al., 1982).

Bioglass is a type of biomaterials that can apply in the biosystem of living things such as in the human body nor animal. It also acts as a specific biological response at an interface of a material that results in the formation of a bond between the tissues and materials (Hench 1993; Hench, 1998). Bioglass 45S5 was introduced by Hench in the late 1960's at University of Florida, United State. Bioglass 45S5 has been in clinical use since 1985 (Hench, 2006). This bioglass consist of 45% SiO<sub>2</sub>, 24.5% CaO, 24.5% Na<sub>2</sub>O and 6% P<sub>2</sub>O<sub>5</sub> (Hench and Paschall, 1974; Hench, 2006). The formulation of Bioglass 45S5 was successful used as an artificial material in the human body due to its excellent biocompatibility and bioactivity (Li et al., 2017). Until now, various type of bioglass was created with different formula composition and method according to their role in biological function. It is seen as one of the optimal compositions in biomedical applications especially in orthopedic. Bioglass 45S5 is commonly used as a reference to other bioglass due to its ability to integrate with the biological host in suitable conditions (Hench, 2013; Fiume et al., 2018). However, Bioglass 4585 has low in mechanical applications due to its intrinsic brittleness characteristic and poor load-bearing application (Baino et al., 2019). Thus, it usually will be reinforced with other materials such as metal to improve the mechanical properties without affecting the bioglass properties itself. The CFAS glass is seen as a suitable glass system that can be featured in the biological application due to its improvised mechanical properties by elemental addition such as fluorine and aluminum.

The CFAS glass system is first introduced by Hill in 1991 during studies on ionomer dental glass as a potential bioactive glass in the biomaterial application (Hill et al., 1991). The CFAS glass consists of five core chemical compounds which are SiO<sub>2</sub>, CaO, CaF<sub>2</sub>, Al<sub>2</sub>O<sub>3</sub> and P<sub>2</sub>O<sub>5</sub>. The SiO<sub>2</sub> and CaO are two main chemical composition that can be replaced by waste materials in this research. Both SiO<sub>2</sub> and CaO are easily available everywhere due to their abundance dump and less used. Therefore, the idea to replace the SiO<sub>2</sub> and CaO with waste materials such as SLS glass and CS in the synthesis of the CFAS glass is one of the novelties in this research.

According to Sinton and Course (2001), SLS glass consists of more than 66 mol.% of silicon dioxide, SiO<sub>2</sub> which is ideal for the extraction element of silicon, Si from the SLS glass for a new production of glassware. The development of the glass industry in Malaysia seen has positive economic growth for the past 5 years (Sunder, 2019). Recently, two largest glass producer companies from Japan and China were invested heavily in the Malaysian market economy for glass processing activities. Malaysia was focused on the factory industry to increase the financial income by participating in manufacturing glass production and leading to the consumption of glass containers for packaged food and beverages. However, the dump of glass which is commonly used for glass sheet, window glass panes and glass containers (Sehgal and Ito, 1998; Sheng et al., 2002). Therefore, the use of SLS glass in synthesizing CFAS glass directly can overcome the dumping problem of glass every year.

The shell marine species consist of rich calcium sources in form of calcium carbonate (CaCO<sub>3</sub>) which is composed of more than 98 wt.% of calcium (Buasri et al., 2013). Thus, shell marine species are seen as an alternative source of high calcium content from waste materials. In Malaysia, the fisheries industry has been played an important role as a major supplier of animal protein sources to the Malaysian population due to the wide surface area of Malaysia's sea (Oon, 1986; Mohamed et al., 2012; Hussin, 2016). The Malaysia's fisheries industry has dynamic and competitive developments, and even has the potential to be developed, especially in contributing to the country's export earnings. High demand on seafood sources causes the fisheries activities in Malaysia become one of the important sectors (FAO, 2006). As a result, the dumping of shells from shell marine species such as clam shell, crab and horseshoe crab increase by the years (Chee et al., 2011). Therefore, the usability of the CS is provenly high in calcium sources and a suitable candidate for the replacement of commercial calcium in synthesizing CFAS glass for reducing the dumping problem of the shells. Moreover, the cost of CS is not only cheap but also easy to get in Malaysia.

The CFAS glass system can be crystallized to form a glass-ceramic and known as FA. The FA crystal is slightly similar to the chemical composition of hydroxyapatite, HA present in enamel composition (Wei et al., 2003; Jantová et al., 2008). The FA crystal with the chemical formula of  $(Ca_{10}(PO_4)_6F)$  can be substituted the fluoride ion, F<sup>-</sup> with hydroxide ion, OH<sup>-</sup> to form HA crystal (Ca<sub>10</sub>(PO<sub>4</sub>)<sub>6</sub>(OH)) (Wei et al., 2003; Jantová et al., 2008; Rahman et al., 2019). Both FA and HA are categorized in calcium phosphate salt group which is widely used in biomedical applications due to excellence in biocompatibility properties (Tung, 1998).

This SiO<sub>2</sub>–CaO–CaF<sub>2</sub>–Al<sub>2</sub>O<sub>3</sub>–P<sub>2</sub>O<sub>5</sub> glass system has shown a positive development in dentistry application, especially for dental cement purposes (Hill et al., 1991). The fabrication of glass ionomer cement, GIC derived from SiO<sub>2</sub>–CaO–CaF<sub>2</sub>–Al<sub>2</sub>O<sub>3</sub>–P<sub>2</sub>O<sub>5</sub> glass system is seen as an acceptable effort for considering the GIC is applied in the dentistry. One of the reasons is the additive of fluoride ion in the CFAS glass system act as an anti-cariogenic agent which is can prevent the formation of plaque on the surface of the enamel (Wiegand et al., 2007; Moreau and Xu, 2010). Anti-cariogenic effects of fluoride involved variety of mechanisms including enhancement of remineralization, reduction of demineralization, interference of pellicle and inhibition of microbial growth in the oral cavity (Featherstone and Ten Cate, 1988; Fejerskov and Ckarkson, 1996; Hamilton, 1996; Rölla and Ekstrand, 1996). In addition, it is also noted that fluoride ions present in blood plasma and saliva are essential for normal development in human body especially for hard tissue development (Jha et al., 1997; Stanton and Hill, 2000).

The glass polyalkenoate cement or commonly known as GIC was first introduced in the late 1960's by Wilson and Kent at the English Laboratory of the Government Chemist, London (Wilson and Kent, 1971; Nicholson et al, 1998; Khoroushi et al., 2013; De Caluwé et al., 2017). From a previous report, the GIC was invented and developed for dental application in the response to the increasing cases of tooth decay (Forss et al., 2013). Dental caries causes serious tooth problems especially pits and fissures on occlusal surfaces among children and adolescents. Thus, the GIC is widely used in various clinical branches of dental application such as restorative, sealant, luting, base and liner to prevent the caries effect problem (Yli-Urpo et al., 2005; Khoroushi and Keshani, 2013).

The GIC is water-based cement which is formed by the reaction of acid and base between aqueous polymer (acid) and glass powder (Wilson and Kent, 1971). According to Fennell and Hill (2001), the most of glasses used for GIC are based on the calcium-aluminosilicate glass system reported by Wilson and Kent. Commonly, the additive of fluoride ion,  $F^-$  and PO<sub>4</sub><sup>3-</sup> were added to the glass system to improve the properties of the GIC for dental application (De Caluwé et al., 2017). The present of fluoride ion in the glass system increases the mechanical properties of GIC especially in compressive strength but decreases the setting time of cement. While, phosphate group, PO<sub>4</sub><sup>3-</sup> increases the working time and setting time but decrease the compressive strength of GIC (De Caluwé et al., 2017).

The setting reaction of GIC occurs as soon as the glass powder and liquid are mixed. During the acid-base reaction, ions such  $Ca^{2+}$ ,  $Al^{3+}$  and  $F^-$  are leaching out from the glass powder and then, cross-linking between polyacid and the surface of the calcium-aluminosilicate glass is immediately occurred (Nicholson et al, 1998). At this stage, the water molecule being an important role for hardening process. The reaction between metal ion on the glass surface continued to linking with polyacid slowly against the aging time up to years. As the reaction progress, the hydrogen bond originated from polymer acid in the liquid is replaced by a metal ionic bond. Then, formation of gelation is formed and the GIC started to hardening against aging time. From the previous researchers, the mechanical properties of the GIC depend on the type of the initial glass powder and aqueous polyacid (Yli-Urpo et al., 2005; Khoroushi and Keshani, 2013).

### 1.3 Problem Statement

In recent years, glass, glass-ceramics, and ceramics have widely attracted prodigious interest in a medical material application due to their properties toward the biological reaction (Rezaie et al., 2015). This kind of material is a biomaterial, which shows the compatibility properties in a biological system. In the medical, biomaterials such as bioglass are commonly used in various applications such as medicine, dentistry and orthopedic (Skallevold et al., 2019). Among the bioglass that received the most attention in dentistry was the CFAS glass with the  $SiO_2$ -CaO-CaF<sub>2</sub>-Al<sub>2</sub>O<sub>3</sub>-P<sub>2</sub>O<sub>5</sub> glass system due to similarity to enamel composition crystallized into FA crystal and consist of fluoride ion to prevent the formation of caries from the microbial growth.

At present, the manufacturing cost for medical applications, especially in dentistry is increased highly over the years due to the increasing cost of production, including the cost of raw materials, labor, manufacture, and development. Due to the high-cost production of bioglass, especially for CFAS glass, the compound of SiO<sub>2</sub> and CaO can be replaced by alternative potential sources to utilize the unwanted materials as one way of recycling.

Usually, the primary compound to produce glass is a pure raw material of  $SiO_2$  compound. Pure  $SiO_2$  is a very expensive cost, and it has a high melting point. Thus, by considering the SLS glass, it consists of a  $SiO_2$  compound with a low cost of raw materials and low melting point compared to the pure  $SiO_2$ . According to previous research, SLS glass acts as an alternative source of  $SiO_2$  to produce a new optical application production. CS is also a waste material that is rich in calcium sources. CS is easily obtained from various seashell types and not used causes it is low in cost. However, CS can be contaminated with heavy metals from factory waste into the sea. As a precautionary step, avoid using or collecting CS from the factory areas near the seaside for dental material applications. In addition, CS can be tested using XRF analysis to confirm the presence of heavy metals contamination.

Therefore, the usability of SLS glass and CS act as the  $SiO_2$  and CaO sources in producing CFAS glass is a suitable way to reduce the production cost and indirectly reduce the landfill waste materials. Besides, there are limited reports and systematic research of physical, structural, thermal, and morphology properties of CFAS glass system derived from vitreous waste materials such as SLS glass and CS. In addition, there are no optimum properties of CFAS glass has been reported especially mechanical properties which are important to apply in dental application.

The fabrication of GIC derived from the CFAS glass by using partially waste material is one of the opportunities to discover the behavior of the GIC itself. GIC is usually used widely in various dental applications for the past 50 years, such as luting, restorative, sealant, lining, and base. Before the existence of GIC, amalgam is made of alloy metal and mercury liquid. It is most widely used to fill a cavity caused by tooth decay. Until now, the uses of amalgam in dentistry are still gaining popularity due to its low cost, ease of application, durability against force, and high strength in mechanical properties. Nevertheless, the uses of amalgam are declining in developed countries. One reason behind this is amalgam has a controversial issue due to the concern about mercury ion release and can cause toxicity in the human body. The GIC seen as the most advantageous and suitable material compared to other materials that used in the dental application.

Basically, GIC shows impressive characteristics such as biocompatible, bioactive, esthetical, anti-cariogenic, rough surface texture, and low solubility. However, GIC has poor mechanical properties. Thus, several studies on GIC related to modifying glass phases to improve the GIC properties, especially in mechanical properties. Besides that, the setting reaction is an important part where gives an effect to the properties of GIC, especially to mechanical properties. The setting reaction started when the glass powder is mix with PAA and then aging at a specific time such as 7, 14, 21, and 28 days in the deionized water. It generally weak and not stable in water after setting reaction; however, as the progression of reaction is complete, it becomes stronger and more resistant against moisture. The previous research reported that the longer time aging of GIC could improve the resistance to moisture, the cement's compressive strength. Another factor that can be considered to enhance the properties of GIC is the ratio of Glass:Polymer:Water during the setting reaction. The ratio is very important, especially during the cement's initial reaction due to the fast reaction between acid and base reaction. Water is the role important in setting time and aging time of GIC. Thus, previous researchers' various ratio of initial water was studied to identify water's role in the fabrication of GIC.

For that reason, this research has focused on the comprehensive study of GIC fabricated from precursor CFAS glass system to use as a biomaterial in dental material for wide application. In this study, the compound's suitable composition to produce the CFAS glass with SLS–CS–CaF<sub>2</sub>–Al<sub>2</sub>O<sub>3</sub>–P<sub>2</sub>O<sub>5</sub> glass system is modified based on the previous research. Two series of compositions prepare the CFAS glass to determine the effect of SLS glass, CS, and CaF<sub>2</sub> in the glass system. Moreover, the initial water ratios while fabricating the GIC from the CFAS glass vary at suitable values. Furthermore, the fabricated GIC has been experienced an aging time from 7 to 28 days to improve the physical, structural, and mechanical properties of GIC. The antibacterial activity of GIC related to fluoride release during the aging time will identify as an excellent potential of the GIC in this research. Thus, this study's findings will anticipate finding a potential application as a dental material application for various types of tooth restoration in dentistry.

### 1.4 Significant of Study

Nowadays, the dump of waste materials generated drastically and increased by every year is one of the problems for every country due to the limited space area of the landfill. The excessive and uncontrolled dumping of waste materials causes environmental pollution consequently the spread of infectious diseases. The usability of waste material such as SLS glass and CS are widely reported by other researchers as precursor of SiO<sub>2</sub> and CaO to respectively to reduce solid wastes. A great deal of research has been focused on the preparing and characterization of the SLS–CS–CaF<sub>2</sub>–Al<sub>2</sub>O<sub>3</sub>–P<sub>2</sub>O<sub>5</sub> based glass system using commercial high-grade chemical composition for dental application such as restorative, filling, luting, liner and base for enamel defect. In this study, the CFAS glass based on SLS–CS–CaF<sub>2</sub>–Al<sub>2</sub>O<sub>3</sub>–P<sub>2</sub>O<sub>5</sub> glass system is prepared using waste materials by replacing SiO<sub>2</sub> and CaO to SLS glass and CS respectively.

The GIC has been identified as the most widely uses of restorative material besides amalgam in dentistry. The major component in the GIC is consists of glass powder and polymer acid that can be changed based on its suitable function. The glass system commonly used as the glass component in the GIC is aluminosilicate glass. The additional elements are added to the glass system to improve the performance of the GIC such as calcium, fluorine, zinc, phosphate, lithium and others. Besides that, the presence of the crystal phase in the glass system of GIC might be can enhanced the properties of the GIC itself such as HA and FA crystal which is similar to the composition of enamel. According to the previous researches, the presence of the Crystal phase in the glass system will be improved the mechanical properties of the GIC and it is very useful for the dental application.

To the best of the author's knowledge, there are very few available literature reports on the production of CFAS glass using waste materials such as SLS glass and CS. In the present research, the CFAS based glass system is used as the initial glass for the fabrication of GIC. The presence of the FA crystal phase in the CFAS glass system is expected to provide significant useful in the physical, structural, thermal and mechanical properties of the GIC. Furthermore, the GIC is fabricated with varying different initial ratios of water and aging times in order to enhance the properties and the quality of the GIC as the final products. Consequently, it is expected that the optimum physical, structural and mechanical properties as well as antibacterial activity properties of GIC derived from CFAS glass have

a high potential for various dental material applications. It is also could contribute as new knowledge in modifying GIC for the dentistry area.

# 1.5 Research Objectives

The main objective of this study is to develop and enhance the GIC which fabricated from the CFAS glass and PAA with specific ratio of water. Two series of CFAS glass based on  $SLS-CS-CaF_2-Al_2O_3-P_2O_5$  system are designed with different glass composition. The working objectives of this research are:

- 1) To synthesis the CFAS glass from combination of commercial grade chemicals and vitreous waste materials via conventional melt-quenching technique.
- 2) To study the effect of difference batch formulation of SLS glass, CS and CaF<sub>2</sub> toward CFAS glass system on structural, thermal and microstructural properties.
- 3) To investigate the influences of initial ratios of water and aging times on physical, structural and mechanical properties of GIC derived from CFAS glass system.
- 4) To evaluate antibacterial properties of GIC against *S. mutans*.

### 1.6 Scope of Study

In order to achieve the objective of this study, the scopes of the study as following:

- 1) A series of precursor CFAS glass (Series 1) based on the stoichiometric equation of  $[(45-x)SLS \cdot xCS \cdot 15CaF_2 \cdot 20Al_2O_3 \cdot 20P_2O_5]$  where x = 5, 10, 15 and 20 (wt.%), has been prepared using SLS glass, CS, CaF<sub>2</sub>, Al<sub>2</sub>O<sub>3</sub> and P<sub>2</sub>O<sub>5</sub> powder by conventional melt-quenching method.
- 2) A series of precursor CFAS glass (Series 2) based on the stoichiometric equation of [(45-x)SLS·15CS·xCaF<sub>2</sub>·20Al<sub>2</sub>O<sub>3</sub>·20P<sub>2</sub>O<sub>5</sub>] where x = 5, 10, 15 and 20 (wt.%), has been prepared using SLS glass, CS, CaF<sub>2</sub>, Al<sub>2</sub>O<sub>3</sub> and P<sub>2</sub>O<sub>5</sub> powder by conventional melt-quenching method.
- 3) The chemical composition of SLS glass and CS are been measured using the XRF spectroscopy in order to confirm the percentage of the chemical oxide before use in the synthesis of CFAS glass.
- 4) The thermal properties of CFAS glass have been measured using DSC and TGA spectroscopy in order to identify the glass transition temperature (T<sub>g</sub>) and glass crystallization temperature (T<sub>c</sub>)
- 5) The chemical composition of the CFAS glass has been measured using XRF and EDX spectroscopy in order to confirm the chemical compound in weight percentage.
- 6) The GIC has been fabricated from the CFAS glass system in Series 1 and Series 2 at different initial ratios of water and aging times between 7 to 28 days.
- 7) The physical, structural, thermal, morphology and mechanical properties of CFAS glass and GIC have been analyzed using the Archimedes method, molar volume equation, XRD, FTIR, Raman spectroscopy, DSC/TGA, FESEM, EDX, Vickers microhardness and Universal testing machine for compressive strength.

8) The optimum GIC sample based on the structural and mechanical properties has been measured for fluoride ion release by ion chromatography and tested for antibacterial activity by disk diffusion method.

In the current study, two different series of CFAS glass are prepared from a combination of the high grade of commercial chemical and vitreous waste materials. Series 1 was varying the weight composition of SLS and CS while Series 2 varying the weight composition of SLS and CaF<sub>2</sub>. Both SLS glass and CS act as compound sources of SiO<sub>2</sub> and CaO respectively. The CFAS glass is synthesized by a conventional melt-quenching technique at a temperature of 1450 °C. The properties of SLS glass, CS and CFAS glass have been characterized such as structural, thermal and morphological in order to study the behaviour of CFAS glass derived from waste materials. Next, the fabrication of GIC is derived from CFAS glass in Series 1 and Series 2 experiences two conditions which are varying the initial ratios of water and the aging times. The initial ratio of water for fabricating GIC was controlled at 1.0, 1.2 and 1.4. While, the period of aging time for GIC in the deionized water was varies at 7, 14, 21 and 28 days. The temperature of aging time is also controlled at 37 °C. The structural, thermal, morphological, and mechanical properties of GIC for both Series 1 and Series 2 are characterized to determine the optimum properties of GIC. The optimum condition of GIC in mechanical properties is selected for further characterization based on the results of Vickers microhardness and compressive strength.

The selected GIC was characterized with further study on physical properties, fluoride ion release and antibacterial activity. The structural, thermal, morphological, physical properties in this study were analyzed by X-ray Fluorescence (XRF), X-ray Diffraction (XRD), Fourier Transform Infrared (FTIR) and Raman Spectroscopy, Differential Scanning Calorimetry (DSC), Thermogravimetric Analysis (TGA), Field Emission Scanning Electron Microscopy (FESEM), Energy Dispersive X-Ray Analysis (EDX), density and molar volume. While, the fluoride ion release and antibacterial activity of the GIC was determined by Ion Chromatography and antimicrobial disk method respectively.

### 1.7 Outline of Thesis

The thesis designed and arranged as follows. Chapter 1 gives an introduction background of CFAS glass, FA and GIC derived from vitreous waste (SLS glass and CS). This chapter also including the problem statements, the objectives of research, the scopes of study and also the significant of the study. The review of the previous and current works reported on the uses of SLS glass and CS as a precursor, production of CFAS glass and fabrication GIC has been discussed in Chapter 2. This chapter also reviewed the physical, structural, thermal, mechanical and antibacterial properties of CFAS and GIC for current and previous works. The details on research designed, methodology and characterization used in this study were described in Chapter 3. Next, Chapter 4 represent the results and discussions concerning on the properties of CFAS glass in Series 1 and Series 2 with different chemical composition of SLS glass, CS and CaF<sub>2</sub>. This chapter also represent the findings and focusing on the properties of GIC derived from CFAS glass in Series 1 and Series 2 at different initial ratios of water and aging times. Besides that, the physical, structural, mechanical and antibacterial properties of CFAS glass and GIC are deeply discussed in

Chapter 4. Finally, the conclusion had been made based on the results obtained from Chapter 4, the suggestion and recommendation for future works presented in Chapter 5. The references, publications and conferences attended by the author were placed at the last part of the thesis.



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### LIST OF PUBLICATIONS

- Khiri, M. Z. A., Matori, K. A., Zainuddin, N., Abdullah, C. A. C., Alassan, Z. N., Baharuddin, N. F., & Zaid, M. H. M. (2016). The usability of ark clam shell (Anadara granosa) as calcium precursor to produce hydroxyapatite nanoparticle via wet chemical precipitate method in various sintering temperature. *SpringerPlus*, 5(1), 1-15.
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