



UNIVERSITI PUTRA MALAYSIA

***MICROSTRUCTURAL AND MECHANICAL PROPERTIES OF
SiO₂-Na₂O-CaO-P₂O₅-CaF₂ BIOGLASS/HYDROXYAPATITE
COMPOSITE***

NOORFAUZANA BINTI ADNIN

ITMA 2018 18



**MICROSTRUCTURAL AND MECHANICAL PROPERTIES OF
SiO₂-Na₂O-CaO-P₂O₅-CaF₂ BIOGLASS/HYDROXYAPATITE COMPOSITE**

By

NOORFAUZANA BINTI ADNIN

**Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia,
in Fullfillment of the Requirement for the Degree of Philosophy**

May 2018

COPYRIGHT

All material contained within the thesis, including without limitation text, logos, icons, photographs and all other artwork, is copyright material of Universiti Putra Malaysia unless otherwise stated. Use may be made of any material contained within the thesis for non-commercial purposes from the copyright holder. Commercial use of material may only be made with the express, prior, written permission of Universiti Putra Malaysia.

Copyright © Universiti Putra Malaysia



Abstract of thesis presented to the Senate of Universiti Putra Malaysia in fulfilment
of the requirement for the degree of Doctor of Philosophy

**MICROSTRUCTURAL AND MECHANICAL PROPERTIES OF
SiO₂-Na₂O-CaO-P₂O₅-CaF₂ BIOGLASS/HYDROXYAPATITE COMPOSITE**

By

NOORFAUZANA BINTI ADNIN

May 2018

Chairman : Khamirul Amin Matori, PhD
Institute : Institute of Advance Technology

In spite of tremendous applications of bioactive glasses, their low mechanical properties such as low strength and high brittleness have limited their clinical applications as load-bearing implants. To overcome these limitation hence in this study, an alternative approaches proposed is by the development a novel composite of Bioglass (BG) and Hydroxyapatite (HA) via thermal treatment method. However, under such sintering conditions, the poor thermal stability of HA (dehydration and decomposition process) which occurred remarkably should be taken into account, since it declines the mechanical properties of the composite. Therefore, Calcium Fluoride (CaF₂) was incorporate into BG composition to improve the thermal stability of HA. In this research work, the purpose is to investigate the microstructure and mechanical properties and also their relationship of new BG-HA biocomposite with the incorporation of CaF₂ in BG system. Such observation is not documented in the literature in this scope of research since investigations on the microstructure, mechanical properties and also their relationship of based BG have remained pointing only towards the effect of heat treatment and liquid phase sintering (LPS), without considering the role of CaF₂ on the microstructure and mechanical properties of BG-HA composite. In addition, in this study, the observation of parallel relation of microstructure and mechanical properties of the BG-HA composites at each stages of sintering temperature was also elucidated.

SiO₂-Na₂O-CaO-P₂O₅-CaF₂ were prepared by conventional melt quenching method and were mixed with HA through solid state reaction, in proportion of 0, 10, 20, 30 and 40 wt% respectively. Each composition was sintered from 500 to 1000 °C with 50 °C increments. The samples were characterized by Thermal Gravimetric Analysis-Differential Scanning Calorimetry (TGA-DSC), Fourier Transform Infrared Spectroscopy (FTIR), X-ray Diffraction (XRD), Field Effect Scanning Electron Microscopy coupled with Energy Dispersive Spectroscopy (FESEM-EDAX), density, grain size, microhardness and compressive strength measurement. FTIR

analysis showed the evidence of non-bridging oxygens (NBO's) with the increase of the network-modifying species content (CaF_2), which responsible for the decrease in the volume of network structure thus increase the value of density. The XRD analysis indicated that BG with 10 wt% HA content sintered at 800 °C show high thermal stability by the presence of $\text{Na}_2\text{Ca}_3\text{Si}_2\text{O}_8$, $\text{Na}_4\text{CaSi}_3\text{O}_9$, $\text{Na}_2\text{Ca}_3\text{Si}_6\text{O}_{16}$, HA, FA and with the absence of β -TCP phases. FESEM micrograph illustrated increasing of grain size by the increasing of sintering temperature. The result shows that density, hardness and compressive strength improved from 500-800 °C sintering temperature. However, at 850-1000 °C sintering temperature the density, hardness and compressive strength significantly decreased. Finally, density of 2.95 g/cm^3 , hardness of 250 HV and compressive strength value of 103 MPa has been attained for BG with 10 wt% HA content sintered at 800 °C. The superior mechanical strength was attributed to the improved densification by heat treatment, LPS and also by the improvement of HA thermal stability through the incorporation of CaF_2 .

Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk Ijazah Doktor Falsafah

**SIFAT STRUKTUR – MIKRO DAN MEKANIKAL KOMPOSIT
SiO₂-Na₂O-CaO-P₂O₅-CaF₂ BIOGLASS/HYDROXYAPATITE**

Oleh

NOORFAUZANA BINTI ADNIN

Mei 2018

Pengerusi : Khamirul Amin Matori, PhD
Institut : Institut Teknologi Maju

Walaupun kaca bioaktif mempunyai aplikasi yang menarik, sifat mekaniknya yang lemah seperti sifat kekerasan yang rendah dan kerapuhan yang tinggi telah membataskan aplikasi klinikalnya sebagai implan pembawa beban. Bagi mengatasi had tersebut, pendekatan alternatif yang dicadangkan adalah dengan penyediaan komposit baru iaitu Bioglass (BG) dan Hydroxyapatite (HA) melalui teknik rawatan haba. Walau bagaimanapun, di bawah pembabitan keadaan persinteran, kestabilan haba HA yang rendah (proses dehidrasi dan penguraian) yang belaku secara luar biasa harus dititik beratkan, memandangkan ianya menyebabkan kemerosotan sifat mekanikal komposit tersebut. Oleh itu, Calcium Fluorida (CaF₂) telah diperkenalkan dalam komposisi BG untuk meningkatkan kestabilan haba HA. Penyelidikan ini adalah bertujuan untuk menyiasat sifat struktur mikro dan mekanikal serta hubungan kait antara kedua sifat tersebut terhadap biokomposit BG-HA yang baru melalui pengenalan CaF₂ dalam sistem BG. Pemerhatian ini tiada dalam kesusasteraan bidang penyelidikan ini dan kajian mengenai sifat struktur mikro, mekanik dan juga hubungan kait antara keduanya terhadap BG hanya memberi tumpuan kepada kesan rawatan panas dan persinteran fasa cecair, tanpa mempertimbangkan peranan CaF₂ pada struktur mikro dan sifat mekanikal komposit BG-HA. Di samping itu, dalam kajian ini, pemerhatian terhadap hubungan struktur mikro dengan sifat mekanikal komposit BG-HA pada setiap peringkat suhu persinteran juga diperjelaskan.

SiO₂-Na₂O-CaO-P₂O₅-CaF₂ disediakan melalui kaedah kebiasaan iaitu pencairan pelindap kejutan dan dicampur dengan HA melalui tindak balas keadaan pepejal masing-masing dengan kadaran 0, 10, 20, 30 dan 40 wt%. Setiap komposisi disinter dari 500 hingga 1000 °C dengan kenaikan 50 °C. Sampel tersebut dicirikan oleh Pengukuran Haba Gravimetrik-Kalorimetri Pengesanan Berbeza (TGA-DSC), Spektroskopi Inframerah Transformasi Fourier (FTIR), Pembelauan Sinar-X (XRD), Mikroskopi Elektron Pengesanan Kesan Medan dan Spektroskopi Penyebaran Tenaga (FESEM-EDAX), pengukuran ketumpatan, saiz butiran, kekerasan mikro dan

kekuatan mampatan. Analisis FTIR membuktikan kewujudan oxygen yang tidak bersambung (NBO's) dengan peningkatan kandungan spesies rangkaian pengubahsuaian (CaF_2), yang bertanggungjawab terhadap pengurangan isipadu struktur rangkaian lalu meningkatkan nilai ketumpatan. Analisis XRD menunjukkan bahawa BG dengan 10 wt% HA yang disinter pada $800\text{ }^\circ\text{C}$ mempunyai kestabilan terma yang tinggi dengan pembentukan fasa $\text{Na}_2\text{Ca}_3\text{Si}_2\text{O}_8$, $\text{Na}_4\text{CaSi}_3\text{O}_9$, $\text{Na}_2\text{Ca}_3\text{Si}_6\text{O}_{16}$, HA, FA tanpa kehadiran fasa β -TCP. Mikrograf FESEM menunjukkan peningkatan saiz butiran dengan peningkatan suhu persinteran. Keputusan ini menunjukkan bahawa ketumpatan, kekerasan dan kekuatan mampatan meningkat dengan suhu persinteran dari $500\text{-}800\text{ }^\circ\text{C}$. Walau bagaimanapun, pada $850\text{-}1000\text{ }^\circ\text{C}$ ketumpatan, kekerasan dan kekuatan mampatan menurun. Akhirnya, nilai ketumpatan pada 2.95 g/cm^3 , kekerasan pada 250 HV dan kekuatan mampatan pada 103 MPa dicapai oleh BG dengan 10 wt% HA, disinter pada $800\text{ }^\circ\text{C}$. Keunggulan kekuatan mekanikal adalah disebabkan oleh peningkatan ketumpatan oleh rawatan haba, sintering fasa cecair serta peningkatan kestabilan haba HA melalui pengenalan CaF_2 .

ACKNOWLEDGEMENT

My profound gratitude goes to Allah S.W.T, all the praise and glory are to him alone for giving me the wisdom, knowledge, health, time, resources and opportunity to see this dream a reality. Peace and blessings of Allah S.W.T upon our noble prophet, Muhammad (SAW), his family, his companions and those who follow his right path till the day of resurrection.

Undertaking this PhD has been truly life-changing experience for me and it would not have been possible to do without the support and guidance that I received from many people. This thesis would not have been achievable without the inspiration and support from a number of wonderful individuals. My thanks and appreciation to all of them for being part of this successful journey.

Firstly, I'd like to give a heartfelt, special thanks to my supervisor, Assoc. Prof. Dr. Khamirul Amin Matori, for all the understanding, support and encouragement he gave me, especially during my hard time. His patience, flexibility, genuine, caring, concern and have faith in me during the dissertation process enable me in earning my PhD. He has never judged nor pushed when he know I needed to juggle priorities and I could not have imagined having a better supervisor for my PhD study. I cannot thank him enough, I am forever grateful, thank you Dr.Khamirul! My thanks also go out to the remaining members of my PhD committee, Dr. Norhazlin, Dr. Raba'ah and not to forget the late Assoc. Prof. Dr. Mansor Hashim. Their academic support, input and personal cheering are greatly appreciated, thank you.

My gratitude is also extended to GCCM and research group team members for their excellent helping during my labwork and data collection that has made an invaluable contribution toward my PhD. I am also very grateful to all my friends at ITMA and who were always so helpful in numerous ways, during various stages of my PhD. Special thanks to Pishah, Idza, Rodi, Nora, Dila and Hafiz who has always been a tremendous help no matter the task or circumstance. All of you shall always be remembered as a warm and friendly heart who assisted me in completing my doctoral program.

My deep appreciation goes out to my family for their continuous and unparallel love, help and support. I am forever indebted to my mother and my late father for giving me the opportunities and experienced that have made me who I am. They selflessly encouraged me to explore new direction in life and seek my own destiny. This journey would not have been possible if not for them, and I dedicate this PhD to them. And finally to my fiancé, Sallehudin who has been my side throughout this PhD, and without whom, I would not have the courage to embark on this journey and making it possible for me to complete what I started.

I certify that a Thesis Examination Committee has met on 7 May 2018 to conduct the final examination of Noorfauzana binti Adnin on her thesis entitled "Microstructural and Mechanical Properties of $\text{SiO}_2\text{-Na}_2\text{O-CaO-P}_2\text{O}_5\text{-CaF}_2$ Bioglass/Hydroxyapatite Composite" in accordance with the Universities and University Colleges Act 1971 and the Constitution of the Universiti Putra Malaysia [P.U.(A) 106] 15 March 1998. The Committee recommends that the student be awarded the Doctor of Philosophy.

Members of the Thesis Examination Committee were as follows:

Mohd Nizar bin Hamidon, PhD

Associate Professor
Faculty of Engineering
Universiti Putra Malaysia
(Chairman)

Jumiah binti Hassan, PhD

Associate Professor
Faculty of Science
Universiti Putra Malaysia
(Internal Examiner)

Sidek bin Hj. Ab Aziz, PhD

Professor
Faculty of Science
Universiti Putra Malaysia
(Internal Examiner)

Cheikhrouhou Abdelwaheb, PhD

Professor
University of Sfax
Tunisia
(External Examiner)



RUSLI HAJI ABDULLAH, PhD

Professor and Deputy Dean
School of Graduate Studies
Universiti Putra Malaysia

Date: 30 July 2018

This thesis was submitted to the Senate of Universiti Putra Malaysia and has been accepted as fulfilment of the requirement for the degree of Doctor of Philosophy. The members of the Supervisory Committee were as follows:

Khamirul Amin Matori, PhD

Associate Professor
Faculty of Science
Universiti Putra Malaysia
(Chairman)

Raba'ah Syahidah Azis, PhD

Senior Lecturer
Faculty of Science
Universiti Putra Malaysia
(Member)

Norhazlin Zainuddin, PhD

Senior Lecturer
Faculty of Science
Universiti Putra Malaysia
(Member)

ROBIAH BINTI YUNUS, PhD

Professor and Dean
School of Graduate Studies
Universiti Putra Malaysia

Date:

Declaration by graduate student

I hereby confirm that:

- this thesis is my original work;
- quotations, illustrations and citations have been duly referenced;
- this thesis has not been submitted previously or concurrently for any other degree at any other institutions;
- intellectual property from the thesis and copyright of thesis are fully-owned by Universiti Putra Malaysia, as according to the Universiti Putra Malaysia (Research) Rules 2012;
- written permission must be obtained from supervisor and the office of Deputy Vice-Chancellor (Research and Innovation) before thesis is published (in the form of written, printed or in electronic form) including books, journals, modules, proceedings, popular writings, seminar papers, manuscripts, posters, reports, lecture notes, learning modules or any other materials as stated in the Universiti Putra Malaysia (Research) Rules 2012;
- there is no plagiarism or data falsification/fabrication in the thesis, and scholarly integrity is upheld as according to the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) and the Universiti Putra Malaysia (Research) Rules 2012. The thesis has undergone plagiarism detection software.

Signature: _____ Date: _____

Name and Matric No.: _____

Declaration by Members of Supervisory Committee

This is to confirm that:

- the research conducted and the writing of this thesis was under our supervision;
- supervision responsibilities as stated in the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) are adhered to.

Signature: _____
Name of
Chairman of
Supervisory
Committee: _____

Signature: _____
Name of
Member of
Supervisory
Committee: _____

Signature: _____
Name of
Member of
Supervisory
Committee: _____

TABLE OF CONTENTS

	Page
ABSTRACT	i
ABSTRAK	iii
ACKNOWLEDGEMENT	v
APPROVAL	vi
DECLARATION	viii
LIST OF TABLES	xiii
LIST OF FIGURES	xv
LIST OF ABBREVIATIONS	xviii
LIST OF SYMBOLS	xxiii
CHAPTER	
1. INTRODUCTION	
1.1 Introduction	1
1.2 Background of the study	1
1.3 Selection of materials	2
1.4 Problem statement	3
1.5 Objective of the study	5
1.6 Outline of the thesis	5
2. LITERATURE REVIEW	
2.1 Introduction	6
2.2 Review on BG-based composites and as reinforced material	6
2.3 Synthesis method of BG-based composite	8
2.4 Influence of microstructural properties on mechanical properties of BG-HA composite	10
2.5 Recent advancement in microstructure and mechanical properties of BG-HA composite	11
2.5 New approach from this research work	14
3 THEORY	
3.1 Introduction	16
3.2 Biomaterials	16
3.3 Bioceramics	18
3.4 Bioglass (BG)	19
3.4.1 Discovery of BG	19
3.4.2 The background and properties of BG	20
3.4.3 Glass and their structure	21
3.5 Hydroxyapatite (HA)	23
3.5.1 Discovery of HA	23
3.5.2 Background of HA	24
3.5.3 Structure and properties of HA	24
3.6 BG-HA Composite	26
3.7 Potential application of BG-HA composite as hip joint replacement for load bearing implant	28

3.8	Bone	
3.8.1	Bone's function and structure	29
3.8.2	Bone's composition	30
3.8.3	Bone's mechanical properties	31
3.8.4	Bone's remodeling (Wolff's Law)	31
3.9	Thermal stability and decomposition of HA	32
3.10	Thermal stability improvement by CaF ₂	33
3.10.1	Background of CaF ₂	33
3.10.2	The role of CaF ₂	34
3.11	Sintering	35
3.11.1	Solid state sintering	36
3.11.1.1	Driving force of solid state sintering	36
3.11.1.2	Stage of sintering	37
3.11.1.3	Mechanims of sintering	37
3.11.1.4	Grain growth coarsening	38
3.11.2	Liquid phase sintering	39
3.12	Microstructure properties of BG-HA composite	42
3.13	Temperature dependence on microstructure	44
3.14	Mechanical properties of BG-HA composite	46
3.14.1	Mechanical requirements for load bearing implant	46
3.14.2	Stress shielding	47
3.14.3	Role of mechanical properties of implant	47
3.15	Thermal stability - microstructure - mechanical properties relationship of BG-HA composite	48
3.16	Characterization of good microstructure-mechanical properties of BG-HA composite as load bearing implant	50
4	METHODOLOGY	
4.1	Introduction	52
4.2	Melt quenching technique for BG synthesizing	52
4.3	Sample description	53
4.4	Raw material	53
4.5	Sample's preparation	53
4.5.1	Weighing	55
4.5.2	Melting and quenching	55
4.5.3	Drying, milling and sieving	55
4.5.4	Addition of HA, miling and mixing	55
4.5.5	Palletizing	55
4.5.6	Sintering condition	56
4.6	Characterization of final sintered samples	56
4.7	Sample's composition	57
4.8	Sample's characterization technique	58
4.8.1	Microstructure's characterization	58
4.8.1.1	Thermogravimetric analysis (TGA)- differential scanning calorimetry (DSC)	58
4.8.1.2	Fourier transform infrared spectroscopy (FTIR)	59
4.8.1.3	X-ray diffraction (XRD)	59
4.8.1.4	Field emission scanning electron microscope (FESEM)	60

4.8.1.5	Energy dispersive X-ray analysis (EDAX)	60
4.8.1.6	Density measurement	61
4.8.1.7	Average grain size measurement	62
4.8.2	Mechanical's characterization	62
4.8.2.1	Vickers hardness test	62
4.8.2.2	Compressive strength test	63
4.9	Error of measurements	63
5.	RESULTS AND DISCUSSION	
5.1	Introduction	65
5.2	Microstructure analysis	65
5.2.1	Thermal critical point analysis by thermogravimetric-differential scanning calorimetry (TGA-DSC)	65
5.2.2	Functional group analysis by fourier transform infrared spectroscopy (FTIR)	72
5.2.3	Phase analysis by X-ray diffraction (XRD)	82
5.2.4	Microstructure observation by field emission scanning electron microscope (FESEM)	102
5.2.5	Grain size analysis for all BG composition	125
5.2.6	Density analysis for all BG composition	129
5.2.7	Elemental compound analysis by energy dispersive X-ray analysis (EDAX)	136
5.3	Mechanical analysis	139
5.3.1	Hardness analysis for all BG composition	139
5.3.2	Compressive strength analysis for all BG composition	143
5.3.3	Typical trend of hardness and compressive strength for all BG composition sintered at 800 °C	151
6	CONCLUSION AND FUTURE WORK	
6.1	Introduction	154
6.2	Conclusions	154
6.3	Suggestions for future work	155
	REFERENCES	156
	APPENDICES	171
	BIODATA OF STUDENT	175
	PUBLICATION	176

LIST OF TABLES

Table		Page
3.1	Biomaterials in organs	17
3.2	Advantages & disadvantages of biomaterials	17
3.3	Mechanical performance requirement for biomaterials	18
3.4	Types of bioceramics-tissue attachment and bioceramics classification	19
3.5	Composition of bioactive glasses and a glass ceramic used for medical and dental application	20
3.6	Mechanical properties of bone and dense HA	25
3.7	Bone composition (%) of adults	30
3.8	Mechanical properties of skeletal system	31
3.9	Significant physical properties of HA and BG biomaterials	48
4.1	Prepared samples of BG-HA composites	57
4.2	Estimated errors for characterization	64
5.1	General band assignment and wavenumber (cm^{-1}) of FTIR analysis for all BG compositions	81
5.2	Lattice parameters, crystal structure and volume of pure BG sintered from 500 to 1000 °C	86
5.3	Lattice parameters, crystal structure and volume of BG with 10 wt% HA content sintered from 500 to 1000 °C	90
5.4	Lattice parameters, crystal structure and volume of BG with 20 wt% HA content sintered from 500 to 1000 °C	93
5.5	Lattice parameters, crystal structure and volume of BG with 30 wt% HA content sintered from 500 to 1000 °C	96
5.6	Lattice parameters, crystal structure and volume of BG with 40 wt% HA content sintered from 500 to 1000 °C	99
5.8	Grain size for all BG composition sintered from 500 to 1000 °C	128

5.9	Experimental density, relative density and porosity of pure BG sintered from 500 to 1000 °C	133
5.10	Experimental density, relative density and porosity of BG with 10 wt% HA content sintered from 500 to 1000 °C	133
5.11	Experimental density, relative density and porosity of BG with 20 wt% HA content sintered from 500 to 1000 °C	134
5.12	Experimental density, relative density and porosity of BG with 30 wt% HA content sintered from 500 to 1000 °C	134
5.13	Experimental density, relative density and porosity of BG with 40 wt% HA content sintered from 500 to 1000 °C	135
5.14	Density, grain size, hardness and compressive strength for pure BG content	148
5.15	Density, grain size, hardness and compressive strength for BG with 10 wt% HA content	148
5.16	Density, grain size, hardness and compressive strength for BG with 20 wt% HA content	149
5.17	Density, grain size, hardness and compressive strength for BG with 30 wt% HA content	149
5.18	Density, grain size, hardness and compressive strength for BG with 40 wt% HA content	150

LIST OF FIGURES

Figure		Page
3.1	Glasses poses a continuous random network in (a) crystalline, (b) amorphous glass form	22
3.2	Modifications of random network modifier by formation of NBO's	22
3.3	Schematic of crystal structure of HA	25
3.4	Schematic of crystal structure of HA for various substitutions	26
3.5	Schematic of hip joint replacement in human body	28
3.6	Structure of a long bone in longitudinal section	29
3.7	Crystal structure of CaF_2	33
3.8	Arrangement of OH groups and F ions in HA, FHA and FA crystal structure	34
3.9	Basic phenomena occurring during sintering under the driving force during sintering	36
3.10	Schematic of sintering mechanism	38
3.11	Schematic of overlapping events in LPS	39
3.12	The three mechanism of neck growth during solution precipitation controlled LPS densifications; (a) contact flattening, (b) dissolutions of small grain, and (c) solid state bonding	40
3.13	(a) Large pore during the sintering, where A and B is grain, (b) elimination of pores by instantaneous filling with liquid and (c) elimination of the liquid pocket by grains growth toward the liquid pocket center upon prolonged sintering	41
3.14	Tensile stress which leading to expansion	42
3.15	Large pores as stress concentration which initiates cracks	43
3.16	Dissolution reprecipitation mechanism during LPS	44
3.18	Pressure in a gas	48

3.19	General trend between bond length and bond strength	49
4.1	Flowchart of sample preparation	54
4.2	Image of eleven pellets which was sintered from 500 to 1000 °C.	56
4.3	“Bloating” phenomenon due to the generation of high porosity.	57
5.1	TGA-DSC curve for pure BG	66
5.2	TGA-DSC curve for BG with 10 wt% HA content	67
5.3	TGA-DSC curve for BG with 20 wt% HA content	68
5.4	TGA-DSC curve for BG with 30 wt% HA content	69
5.5	TGA-DSC curve for BG with 40 wt% HA content	71
5.6	FTIR spectra of pure BG sintered from 500 to 1000 °C	73
5.7	FTIR spectra of pure BG with 10 wt% HA content sintered from 500 to 1000 °C	75
5.8	FTIR spectra of pure BG with 20 wt% HA content sintered from 500 to 1000 °C	77
5.9	FTIR spectra of pure BG with 30 wt% HA content sintered from 500 to 1000 °C	78
5.10	FTIR spectra of pure BG with 40 wt% HA content sintered from 500 to 1000 °C	80
5.11	XRD patterns of pure BG for as-prepared continued with sintering from 500 to 1000 °C	84
5.12	XRD patterns of pure BG with 10 wt% HA content for as-prepared continued with sintering from 500 to 1000 °C	88
5.13	XRD patterns of pure BG with 20 wt% HA content for as-prepared continued with sintering from 500 to 1000 °C	92
5.14	XRD patterns of pure BG with 30 wt% HA content for as-prepared continued with sintering from 500 to 1000 °C	95
5.15	XRD patterns of pure BG with 40 wt% HA content for as-prepared continued with sintering from 500 to 1000 °C	98
5.16	XRD patterns of all BG composition sintered at 800 °C	101

5.17 (a)-(k)	FESEM micrograph of Pure BG sintered from 500 to 1000 °C	105
5.18 (a)-(k)	FESEM micrograph of BG with 10 wt% HA content sintered from 500 to 1000 °C	109
5.19 (a)-(k)	FESEM micrograph of BG with 20 wt% HA content sintered from 500 to 1000 °C	113
5.20 (a)-(k)	FESEM micrograph of BG with 30 wt% HA content sintered from 500 to 1000 °C	117
5.21 (a)-(k)	FESEM micrograph of BG with 40 wt% HA content sintered from 500 to 1000 °C	121
5.22 (a)-(e)	FESEM micrograph of all BG composition sintered at 800 °C	124
5.23	Variation of grain size for all BG composition sintered from 500 to 1000 °C	127
5.24	Variation of density for all BG composition sintered from 500 to 1000 °C	132
5.25 (a)-(j)	FESEM images-EDAX analysis of all BG composition sintered at 800 °C	138
5.26	Variation of hardness value for all BG composition sintered from 500 to 1000 °C	142
5.27	Typical trend of density and hardness value of all BG composition sintered at 800 °C	142
5.28	Variation of compressive strength value for all BG composition sintered from 500 to 1000 °C	147
5.29	Typical trend of density and compressive strength of all BG composition sintered at 800 °C	147
5.30	Typical trend of hardness and compressive strength value of all BG composition sintered at 800°C	153

LIST OF ABBREVIATIONS

BG	Bioglass
HA	Hydroxyapatite
β -TCP	Beta-tricalcium phosphate
α -TCP	Alpha-tricalcium phosphate
SiO ₂	Silicon oxide
CaO	Calcium oxide
CaCO ₃	Calcium carbonate
Na ₂ O	Natrium oxide
Na ₂ CO ₃	Natrium carbonate
P ₂ O ₅	Phosphorus pentoxide
CaF ₂	Calcium fluoride
BG-HA	Bioglass-hydroxyapatite
LPS	Liquid phase sintering
Ca/P	Calcium/phosphate
OH	Hydroxyl
F	Fluorine
FA	Fluoroapatite
FHA	Fluorohydroxyapatite
Na	Natrium
TCP	Tricalcium phosphate
ZrO ₂	Zirconia
Y-TZP	Yttrium-trizirconia phosphate
Mg	Magnesium

CNT	Carbon nanotubes
Co-Cr-Mo	Cobalt-chromium-molybdenum
PVA	Polyvinyl alcohol
COL-BG	Collagen-bioglass
Al ₂ O ₃	Aluminium oxide
SPS	Spark plasma sintering
45S5	45 wt% silicate, 24.5 wt% calcium oxide, 24.5 wt% sodium oxide and 6.0 wt% phosphate
SLS	Selective laser sintering
Ca ₂ P ₂ O ₇	Calcium phosphate
H ₂ O	Water molecule
HA-BG	Hydroxyapatite-bioglass
K ₂ O	Potassium oxide
ZnO	Zinc oxide
Zn	Zinc
Ca	Calcium
MgO	Magnesium oxide
SrO	Strontium
CAD	Computer-aided design
CPT	Camptothecin
SLS	Soda lime silica
CS	Clam shell
Ti	Titanium
Co-Cr	Cobalt-chromium
C	Carbon

CaP	Calcium phosphate
A-W	Apatite-wollastonite
S53P4	53 wt% silicone oxide, 4 wt% phosphate, 23 wt% natrium oxide and 20 wt% calcium oxide
SiO	Silicone monoxide
HCA	Hydroxycarbonated apatite
MPa	Mega pascal
SiO ₄	Silica
NBO	Non bridging oxygens
Ca ₁₀ (PO ₄) ₆ F ₂	Fluoroapatite
β-Ca ₃ (PO ₄) ₆	Beta-tricalcium phosphate
Ca ₁₀ (PO ₄) ₆ (OH) ₂	Hydroxyapatite
HIV	Human immunodeficiency virus
BSE	Bovine spongiform encephalopathy
HCl	Hydrochloric acid
P	Phosphorus
pH	Power of hydrogen
Mpa.m	Mega pascal. meter
Cm	Centimeter
N/A	Not applicable
Nm	Nanometer
PO ₄	Phosphate
Cl	Chlorine
Co	Cobalt
PO ₄ ³⁻	Phosphate ion

GPa	Giga pascal
N.mm	Newton millimetre
SrF ₂	Strontium fluoride
MgF ₂	Magnesium fluoride
NaF	Sodium fluoride
KF	Potassium fluoride
H ⁺	Hydrogen ion
O ⁻²	Oxygen ion
μm	Micrometer
J	Joule
Na ₂ Ca ₂ Si ₃ O ₉	Natrium calcium silicate
g	Gram
Ca ₁₀ (PO ₄) ₆ O	Oxygen phosphorite
CaNaPO ₄	Calcium natrium phosphate
Ca ₃ (PO ₄) ₂	Calcium phosphate
wt	Weight
rpm	Revolutions per minute
TGA	Thermogravimetric analysis
DSC	Differential scanning calorimetry
FTIR	Fourier transform infrared spectroscopy
XRD	X-ray diffraction
FESEM	Field effect scanning electron microscope
HV	Hardness vickers
EDAX	Energy dispersive analysis x-ray
T _g	Transition temperature

T_c	Crystallization temperature
Cu	Copper
Kg	Kilogram
F	Force
N	Newton
ATR	Attenuated total reflection
ZnSe	Zinc selenide
Ge	Germanium
IR	Infrared light



LIST OF SYMBOLS

α	Alpha
β	Beta
wt%	Weight percentage
$^{\circ}\text{C}$	Degree celsius
<	Less than
a, b and c	Lattice parameter
%	Percentage
γ	Specific surface (interface) energy
A	Total surface (interface) area
γA	Total interfacial energy of a powder compact
$\Delta\gamma$	Change in interfacial energy
r_1 and r_2	Radii of curvature
σ	Effective stress on the atoms under the surface
μ	Diffusion potential
Ω	Atomic or molar volume
Υ	Vacancy
$^{\circ}\text{C}/\text{min}$	Heating/cooling rate
d	Spacing between the lattice planes in the crystals
θ	Angle of diffraction
n	Order of diffraction (an integer)
λ	Wavelength of the x- ray (0.154nm)
W_{air}	Weight of pellet in air
W_{water}	Weight of pellet in water

ρ	Density
ρ_{water}	Density of water (1 g cm ⁻³)
ρ_{xrd}	Theoretical density from XRD density
ρ_r	Relative density
P	Amount of porosity
Z	Number of molecules per unit cell
M	Molecular weight of a sample
N_a	Avogadro's number (6.022140857 x 10 ²³)
V	Volume of the crystal structure
ρ_{exp}	Experimental density
136°	Interfacial angle of pyramid shape indenter
d_1 and d_2	Average of the two diagonals
a.u	Arbitrary unit
2 θ	2 theta degree
Å	Angstrom (10 ⁻¹⁰ m)
(h, k, l)	Miller indexes
(α , β , γ)	Angle between lattice parameter in crystal structure
P	Pressure
σ	Compressive strength

CHAPTER 1

INTRODUCTION

1.1 Introduction

In this chapter, the author's motivation for embarking upon research into the specific area is introduced and explained. Background and research topic is presented first, followed by selection of materials, problems statement, objectives of study and outline of the thesis.

1.2 Background of Study

Over the last several decades, an increase in longevity and life expectancy has raised the average age of the world's population. It is projected that by 2050 there will be more than 1 billion people alive on earth aged 60 years old or older (Gunduz and Oktar, 2014). Currently, there are a large number of older people aged at 70 and 80 years old compared to previous years. This improvement may be related to better nutrition and improvement in medical care, improved vaccinations, drugs and water treatment. Moreover, in the light of human life expectancy up to 90 years, the improvements in life care and the increase of accidents, due to sport activities and car accidents, the need for effective and inexpensive biomaterials available to everyone such as those produced from biologically derived HA and BG, is in great demand. This has resulted in an urgent need for improved biomaterials and processing technologies for implants, more so for orthopaedic and dental applications.

Owed to this, implants or transplants can be utilized to preserve human's quality of life due to illnesses disorder and accidents. Bone and joint degenerative and inflammatory problems affect millions of people worldwide. In fact, they account for half of all chronic disease in people over 50 years in developed countries. In addition, it is predicted that the percentage of person over 50 years of age affected by bone diseases will double up by 2020. The number of treated skeletal deficiencies steadily increases in a global state. Effective ways for bone replacements and enhancement of bone formation together with research directed to find ideal biomaterials for grating purposes, which will feature biocompatibility and productive simplicity and economy are required.

Medical technologies benefit the lives of people in many ways. Through the use of biomaterial technologies, people can live healthier, more productive and independent life. Many individuals who previously may have been chronically ill, disabled, or suffering chronic pain can now look forward to leading normal or close to normal life. Worldwide health care problem are including defects and functional disorder of bone (Carrington, 2005). With the increasing of aging people and illness, bone repair

has turn out to be the main clinical and socioeconomic necessity (Cancedda et al., 2003). Research into novel materials for biomedical applications is ever increasing as the medical community look to improve their way in which disorders and trauma are treated. Many new materials have been developed in an attempt to address these concerns but there are still issues surrounding the appropriateness of their mechanical properties, the ability of degradable materials to retain their properties once implanted and the ability to form the material in situ to the requirements of the surgeon.

1.3 Selection of Materials

To date, with the advancement of medicine, biology and materials science, metal, polymers and natural materials have been utilized as biomedical implant. Nevertheless, some of them are bioinert materials (stainless steel, titanium alloy and aluminium ceramics) which restricted their clinical applications owing to their non-active bond with human tissue (Younger and Chapman, 1989). Therefore, selection of appropriate bioceramics is significantly important. Among various kinds of materials, bioactive ceramics such as BG and HA are considered as the most promising biomaterials, due their ability to form direct bonds with living bone and afterwards implantations in bone defects (Liu, 2012). Consequently, in the previous decades BG and HA has turn into research hotspot for bone repair.

BG ceramics open up new possibilities for medical treatment and constitute a new area of research in the natural science and medicine. Owing to their widely variable combinations of properties, BG ceramics can be more easily adapted to suit medical requirements that can customary implant. BG extensively used in various ways as in replacement of hips, knees, tendons and ligaments due to the appropriate such us compatibility, chemical stability and high wear resistance. Bioactive glass-ceramics are establish to have superior mechanical properties corresponding to bending strength, fracture toughness and young's modulus, allowing to be used in load bearing applications (Hashmi et al., 2013). Bioactive glass-ceramics has been used successfully in more than 60,000 clinical cases including vertebral replacement and iliac creast repair.

In 2016, a research team from University of Milano-Bicoccu and Imperial Collage of London have developed BG, a material that mimics the properties of natural cartilage and might support its regrowth to benefit persons suffering severe pain due to osteoarthritis. The material can be formulated to be shock absorbent and also imitates the load bearing quality of real cartilage. Engineering synthetic cartilage disc implants from BG would be the alternative to conventional treatment. The BG would act similarly to real cartilage without the need for metal or plastic devices employed at present. These achievements thus demonstrate that it is possible to design bioactive glass-ceramics with improved microstructure and mechanical properties that should be possible to use clinically as load bearing applications. Glass ceramics obtained by sintering process and it is well documented that during the incident of crystallization and densification, the parent glass microstructure's shrinks, hence

reducing the porosity and the solid structure improves in mechanical strength. Brittleness as well as low fracture toughness continues as main problem of these materials. Due to this drawback, bioactive glass is limited in use as implant devices for load bearing applications.

Numerous techniques have been investigated in attempts to improve the mechanical properties of BG ceramics, by formation of BG composites reinforced with other bioactive ceramics which is HA. Owing to its structural and compositional resemblance to the mineralized matrix of natural bone, HA was identified as unique bioceramics for implants. The bone bonding capacity of HA may help cementless fixation of orthopaedic prosthesis. Despite this criteria, it is also known for its stimulating effect of bone formation, termed as osteoconductive (Natasha et al., 2011). HA was identified as the ultimate stable calcium phosphate (Sinha et al., 2008) and have been comprehensively studied for its numerous potential in medical applications. The main reason for developing and producing composite materials is to achieve a combination of properties not achievable by any of the elemental materials alone. Approaches to achieving enhanced mechanical properties including the incorporation of CaF_2 into the BG composition. In recent years, increasing interest has been shown in sintering of BG with HA. Such composites come to retain their useful bioactive properties whilst providing more suitable mechanical properties for load bearing application.

1.4 Problem Statement

The enormous progress made in the field of medicine over the past few decades has been partly due to the introduction of new instruments but also a result of the use of new materials. It is impossible to imagine modern medicine without bioceramic materials. BG ceramics open up new possibilities for medical treatment and constitute a new area of research in the natural science and medicine. Owing to their widely variable combination of properties, BG ceramics can be more easily adapted to suit medical requirements that can customize implants. BG on the other hand, exhibit excellent biocompatibility, but their poor mechanical properties (low strength, toughness and high brittleness) are a significant hindrance for load-bearing applications.

Recently, several attempts have been made to combine bioactive glasses with HA of different composition, in order to develop composites with improved mechanical performance. Unfortunately, the production of such composite systems implies in several drawbacks, including decomposition of HA phase/ or reactions between the constituent phases and also crystallization of the original phase, with non-trivial consequences in terms of microstructure and mechanical properties of the final samples. In addition, poor thermal stability of HA in the sintered composite induced a weaker mechanical strength of BG-HA composite as implant for load-bearing applications.

Therefore, research is in development on the preparation, microstructure and mechanical characterization of BG-HA composites and it is essential to prepare new biocomposites using every potential compositional changes and changes of preparation parameter since microstructure and mechanical properties of this composite are identified to be critically influenced by these significant variations. Instead of the influence of sintering temperature and LPS, it is also possible to enhance the microstructure and mechanical properties of the composite by thermal stability improvement of HA through the incorporation of CaF₂ into BG composition. Furthermore, it is expected that the composites have superior microstructure and mechanical properties, could be attributed by sintering the composites at low temperature, and hence much reduces the porosity.

Since there were only little studies on the effect of HA additions on BG composition, the exact role of “CaF₂” incorporation in BG and how it can improve the microstructure and mechanical properties of the composite have not yet been clarified. Moreover, most of the work has been devoted to heat treatment and LPS effect in order to improve the microstructure and mechanical properties, while no reports can be found on the role of CaF₂ in BG-HA composite. Also, in spite of many investigation carried out on BG, investigation concern about the parallel relation of microstructure and mechanical properties of the BG-HA composites at each stages of sintering temperature has not been sufficiently elucidated.

Based on the problem statement, the hypothesis of this research project is the observation of high densification, less porosity and small grain size microstructure would result in the increase of mechanical properties in the samples. Nevertheless, the existence of pores, large and abnormal grain size would deteriorate the microstructure and mechanical properties. The microstructure and mechanical properties would be enhanced due to the sintering at relatively low sintering temperature and the influences of LPS as well as major improvement of HA thermal stability with low tendency of HA thermal decomposition, resulting less formation of pores and small grain size observed in the sample. Another hypothesis of this research project is the observations of microstructure changes would greatly influence the mechanical properties of BG-HA composites at each stage of sintering temperature. It is also expected that the incorporation of CaF₂ would be remarkable in terms of microstructure and mechanical properties improvements for BG-HA composites in this study.

1.5 Objective of Study

In this present research work, five different compositions of $\text{SiO}_2\text{-Na}_2\text{O-CaO-P}_2\text{O}_5\text{-CaF}_2$ BG/HA composite with eleven sintering temperatures were performed. The aim of this research is to investigate the microstructure and mechanical properties of novel BG/HA composite with the inclusion of CaF_2 in the BG composition. With the main aim of this research, the following objectives are:

- i. To investigate the microstructure properties of BG-HA composites.
- ii. To evaluate the mechanical properties of BG-HA composites.
- iii. To study the relationship between microstructure and mechanical properties of BG-HA composites.

1.6 Outline of Thesis

This thesis is divided into six chapters. Chapter 1 provides general introduction about biomaterials and also the importance of this significant study in our lives. Chapter 2 reviews related literature which is compulsory to understand the objective of the project. This chapter associates with previous work and gives motivation for the work performed in this thesis. Chapter 3 concentrates on the basic concepts and theory of biomaterials. This chapter focuses more on process, reaction, properties, application and further details about materials involved in this study. Chapter 4 describes the methodology used in the design of the experiments. It also includes the characterization techniques and instruments used in this research field. Chapter 5 present the findings of the study in the order of the specific problem as stated in the problem of statement. This chapter also discussed the significance of the results. Finally, chapter 6 summarizes a brief, generalized statement to answer the general and each of the specific sub-problems and presents an outlook for future work.

REFERENCES

- Abdulrahman, I., Ibiyeye, H., Mohammed, B. A., Saidu, H., Yusuf, H., Ndejiko, M., and Mohammad, S. (2014). From garbage to biomaterials: an overview on egg shell based hydroxyapatite. *Journals of Materials*, 2014, 1-6.
- Adams, L. A., Essien, E. R., Shaibu, R. O., and Oki, A. (2013). Sol gel synthesis of $\text{SiO}_2\text{-CaO-Na}_2\text{O-P}_2\text{O}_5$ bioactive glass ceramic from sodium metasilicate. *New Journal of Glass and Ceramics*, 3, 11-15.
- Adibnia, S., Nemati, A., Fathi, M. H., and Baghshahi, S. (2011). Synthesis and characterization of sol-gel desired HA-BG composite nanopowders for biomedical applications. *Journal of Biomimetics, Biomaterials and Tissue Engineering*, 12, 51-57.
- Adolfsson, E., Nygren, M., and Hermauson, L. (1999). Decomposition mechanism in aluminium oxide-apatite systems. *Journal American Ceramic Society*, 8, 2909-2912.
- Ahn, A. C., and Gradzinsky, A. J. (2009). Relevance of collagen piezoelectricity to wolff's law: a critical review. *Medical Engineering Physics*, 31, 733-741.
- Akao, M., Aoki, H., and Kato, K. (1981). Mechanical properties of sintered hydroxyapatite for prosthetic application. *Journal Material Science*, 16(3), 809-812.
- Andrievskii, R. A. (1982). Strength of sintered bodies. *Powder Metallurgy*, 1, 37-42.
- Aoki, H. (1991). *Science and Medical Applications of Hydroxyapatite*. Tokyo: Takayama Press System Centre.
- Ashley, A. W., Serena, M. B., and Ian, A. K. (2007). Hydroxyapatite-carbone nanotube for biomedical applications: a review. *International and Apply Ceramic Technology*, 4, 1-13.
- Bang, H. G., Kim, S. K., and Park, S. Y. (2008). Biocompatibility and the physical properties of bio-glass ceramics in the $\text{Na}_2\text{O} - \text{CaO} - \text{SiO}_2 - \text{P}_2\text{O}_5$ system with CaF_2 and MgF_2 additives. *Journal of Ceramics Processing Research*, 9(6), 588-590.
- Barinov, S., Ran, J., Nunziante, C. S., Durisin, J., Fadeera, I., Medvecky, L., and Trionfetti, G. (2006). Carbonate released from carbonated hydroxyapatite in the wide temperature range. *Journal Material Science Material Medical*, 17, 596-604.
- Batal, H. A. E., Azooz, M. A., Khalil, E. M. A., Manem, A. S., and Hamdy, Y. M. (2003). Characterization of some bioglass ceramics. *Materials Chemistry and Physics*, 80(3), 599-609.

- Beckham, G. A., Greenle, T. K., and Crebo, A. R. (1971). Bone formation at a ceramic implant interface. *Calcified Tissue Research*, 8(1), 165-171.
- Belluci, D., Canillo, V., and Sola, A. (2011). A new highly bioactive composite for scaffold application: a feasibility study. *Materials*, 4, 339-354.
- Belluci, D., Sola, A., and Canillo, V. (2017). Role of magnesium oxide and strontiumoxide as modifiers in silicate based bioactive glasses: effects on thermal behaviour, mechanical properties and in-vitro bioactivity. *Materials Science and Engineering C*, 72, 556-575.
- Belucci, D., Sola, A., and Canillo, V. (2015). Bioactive glass/hydroxyapatite composite: mechanical properties and biological evaluation. *Materials Science and Engineering C*, 51, 196-205.
- Belucci, D., Sola, A., and Cannillo, V. (2013). Bioactive glass/ZrO₂ composites for orthopaedic applications. *Biomedical Materials*, 9(1), 1-12.
- Best, S. M., Porter, A. E., Thian, E. S., and Huang, J. (2008). Bioceramics: past, present and for the future. *Journal of the European Ceramic Society*, 28, 1319-1327.
- Bigi, A., Pazarolta, S., Roveri, N., and Rubini, K. (2001). Bonelike apatite growth on hydroxyapatite-gelatin sponges from stimulated body fluid. *Journal of Biomedical Materials Research Part A*, 59(4), 709-715.
- Boilet, L., Descamps, M., Rguiti, E., Tricoteaux, A., Lu, J., Petit, F., Lardot, V., Cambier, F., and Leriche, A. (2013). Processing and properties of transparent hydroxyapatite and β -tricalcium phosphate obtained by HIP process. *Ceramic International*, 39, 283-288.
- Bonfield, W. (1998). Hydroxyapatite-reinforced-polyethylene as an analogous materials for bone replacement. *Bioceramics*, 523, 173-177.
- Bousslama, N., Chavelier, Y., Bouaziz, J., and Ayed, F. B. (2013). Influence of the sintering temperature on young's modulus and the shear modulus of tricalcium phosphate-fluoroapatite composites evaluated by ultrasound technique. *Material Chemistry Physics*, 141, 289-297.
- Brauer, D. S., Karpukhina, N., Seah, D., Law, R. V., and Hill, R. G. (2008). Fluoride-containing bioactive glasses. *Advanced Materials Research*, 39-40, 299-304.
- Brinker, C. J., and Scherer, G. W. (1990). *Sol-Gel Science, The Physics and Chemistry of Sol - Gel Processing*. Boston: Academic Press.
- Brunner, T. J., Grass, R. N., and Stark, W. J. (2006). Glass and bioactive glass nanopowder by flame synthesis. *European Cells and Materials*, 11(2), 1-18.

- Caliskan, F. (2016). Apatite wollastonite-reinforced hydroxyapatite biocomposite. *Acta Physicapolonica A*, 129(4), 665-668.
- Calver, A., Hill, R. G., and Stamboulis, A. (2004). Influence of fluorine content on the crystallization behavior of apatite-wollastonite glass-ceramics. *Journal Material Science*, 39(7), 2601-2603.
- Cancedda, R., Dozin, B., Gianoni, P., and Quarto, R. (2003). Tissue engineering and cell therapy of cartilage and bone. *Matrix Biology*, 22, 81-91.
- Carrington, J. L. (2005). Aging bone and cartilage. *Biochemical, Biophysics Research Communication*, 328, 700-708.
- Chanshetti, U. B., Shelke, V. A., Jadhav, S. M., Shankarwar, G., Chondhekar, T. K., Shankarmar, A. G., Sudarsan, V., and Jogad, M. S. (2011). Density and molar volume studies of phosphate glasses. *Physics, Chemistry, Technology*, 9(1), 29-36.
- Chatzistarrou, X., Chrissafis, K., Kontonasaki, E., Zobra, T., Koidis, P., and Paraskeropoulos, K. M. (2006). Sintered hydroxyapatite/bioactive glass composites: thermal analysis and bioactivity. *Key Engineering Materials*, 309-311, 167-170.
- Chatzistavrou, X., Zarba, T., Kontonasaki, E., Chrissafis, K., Koidis, P., and Paraskeropoulos, K. M. (2004). Following bioactive glass behaviour beyond melting temperature by thermal and optical methods. *Physic State Solid*, 201(5), 944-951.
- Chen, S. Y., Chou, P. F., and Lin, H. M. (2017). Preparation and characterization of mesoporous bioactive glass from agricultural waste rice husk for targeted anticancer drug delivery. *Ceramics International*, 43(2), 2239-2245.
- Chen, Y., and Miao, X. (2005). Thermal and chemical stability of fluorohydroxyapatite ceramics with different fluorine contents. *Biomaterials*, 26(11), 1205-1210.
- Chevelier, J., and Gremillard, L. (2009). Ceramics for medical applications: a picture for the next 20 years. *Journal European Ceramic Society*, 29, 1245-1255.
- Cho, Y. K., Yoon, D. Y., and Kim, B. K. (2004). Surface roughening transitions and coarsening of NbC grains in Liquid cobalt-rich matrix. *Journal American Ceramic Society*, 87(3), 443-448.
- Damrawi, G. E., Hassan, A. K., Kamal, H., Aboelez, M., and Labeeb, S. (2016). Structural investigations on $\text{Na}_2\text{O} - \text{CaO} - \text{V}_2\text{O}_5 - \text{SiO}_2$ bioglass ceramics. *British Journal of Applied Science and Technology*, 16(3), 1-9.

- Demirkian, H., Hu, Y., Zuin, L., and Aswath, P. B. (2008). XANES study of bioglass 4555-hydroxyapatite Co-sintered bioceramics. *Chemical and Materials Science*, 11, 50-51.
- Du, R. L., Chang, J., Wan, S. Y. N., Zhai, Y., and Wang, J. Y. (2006). Characterization and in vitro bioactivity of zinc-containing bioactive glass-glass-ceramics. *Journal of Biomaterials Applications*, 20(4), 341-360.
- Duan, S., Feng, P., Guo, C., Xiao, T., Yu, K., Shuai, C., and Peng, S. (2015). Microstructure evolution and mechanical properties improvement in liquid-phase-sintered hydroxyapatite by laser sintering. *Materials*, 8, 1162-1175.
- Durgalaksmi, D., and Balakumar, S. (2013). Nano bioglass (NBG) for bone regeneration applications preparations and its characterization. *Solid state physics*, 1512, 122-123.
- Eraba, K. M. T., Hassan, M. Y., Hamazawy, E., Hadad, A., and Ayoub, H. A. (2015). Characterization of bioglass ceramic after addition of fluorine $\text{Na}_2\text{O} - \text{CaO} - \text{SiO}_2$ system. *Advances in Applied Science Research*, 6(3), 191-195.
- Essien, E. R., Atasie, V. N., and Udabong, E. U. (2015). Microwave energy-assisted formation of bioactive CaO-MgO-SiO_2 ternary glass from bio-wastes. *Bulletin Material Science*, 39(4), 989-995.
- Frost, H. M. (2000). The utah paradigm of skeletal physiology: an overview of its insight for bone, cartilage and collagenous tissue organs. *Journal Bone Mineral Metabolism*, 18(6), 305-316.
- Fu, L., Wen, J., Zhang, H., Guo, Y., and Yang, F. (2015). *International Conference on Material, Enviromental and Biological Engineering: Selected Paper on the Conference Held in China*. Atlantis Press.
- Gan, F. X. (1988). *Science and Technology for Modern Glass*. Shanghai: Shanghai Sciences and Technology Press.
- Gao, C., Deng, Y., Feng, P., Mao, Z., Li, P., Yang, R., Deng, I., Cao, Y., Shuai, C., and Peng, S. (2014). Current progress in bioactive ceramic scaffolds for bone repair and regeneration. *International Journal Molecular Science*, 15, 4714-4732.
- Georgion, G., Knowles, J. C., Barralet, J. E., Kong, Y. M., and Kim, H. E. (2004). The effect of hot pressing on the physical properties of glass reinforced hydroxyapatite. *Journal Material Scimaterial Medical*, 15(6), 705-710.

- Georgiou, G., and Knowles, J. C. (2001). Glass reinforced hydroxyapatite for hard tissue surgery part 1: mechanical properties. *Biomaterials*, 22(20), 2811-2815.
- German, R. M. (1985). *Liquid Phase Sintering*. New York: Plenum Press.
- German, R. M., Suri, P., and Park, S. J. (2009). Review: liquid phase sintering. *Journal Material Science*, 44, 1-39.
- Goller, G., Demirkhan, H., Oktar, F. N., and Demirkesan, E. (2003). Processing and characterization of bioglass reinforced hydroxyapatite composite. *Ceramics International*, 29, 721-724.
- Greenlee, T. K., Bekham, C. A., Crebo, A. R., and Malmborg. (1972). Glass ceramic bone implant. *Journal of Biomedical Materials Research*, 6(3), 235-244.
- Greenspan, D. C., Zhong, J. P., and Wheeler, D. L. (1998). Bioactivity and biodegradability melt by sol gel derived glasses in vitro and in vivo. *Bioceramics*, 11, 348-354.
- Greish, Y. E., and Brown, P. W. (2000). Characterization of bioactive glass-reinforced polymer composites. *Journal Biomedical Material Research*, 52(4), 687-694.
- Groh, D., Dohler, F., and Brauer, D. S. (2014). Bioactive glasses with improved processing, part 1, thermal properties, ion release and apatite formation. *Acta Biomaterial*, 10(10), 4463-4473.
- Guillon, O., Cao, S., and Boaccaccini. (2011). Effects of uniaxial lead on the sintering behaviour of 45S5 bioglass powder compacts. *Journal of the European Ceramic Society*, 31(6), 999-1007.
- Gultekin, N. (2002). *Preparation and characterization of hydroxyapatite and polymer composite biomaterials*, Master Thesis, Izmir Institute of Technology.
- Gunduz, C., and Oktar, F. N. (2014). Preparation of scaffolds and new biomaterials for health care industries. *Bioceramics Development and Applications*, 4(1), 100-104.
- Guo, H. B., Miao, X., Chen, Y., Cheang, P., and Khor, K. A. (2004). Characterization of hydroxyapatite-bioglass-316L fibre composite prepared by spark plasma sintering. *Materials Letters*, 58(3-4), 304-307.
- Habibe, A. F., Maeda, L. D., Souza, R. C., Barboza, M. J. R., Daguano, J. K. M. F., Rogero, S. O., and Santos, C. (2009). Effect of bioglass additions on the sintering of Y-TZP bioceramics. *Materials Science and Engineering C*, 29, 1959-1964.

- Han, J. K., Song, H. Y., Saito, F., and Lee, B. T. (2006). Synthesis of high purity nano-sized HA powder by microwave hydrothermal method. *Materials Chemistry and Physics*, 99, 235-239.
- Hapishah, N. A. (2017). *Parallel evolution of morphology and multiferroic properties of polycrystalline holmium and yttrium manganite (HoMnO₃) and (YMnO₃) synthesized via mechanical alloying*, Phd Thesis, University Putra Malaysia.
- Hashmi, M. U., Shah, S. A., Umer, F., and Alkedy, A. S. (2013). Effect of sintering temperature on microstructure and in vitro behaviour of bioactive glass-ceramics. *Ceramics-Silikaty*, 57(4), 313-318.
- Hench, L. L. (2013). Chronology of bioactive glass development and clinical applications. *New Journal of Glass and Ceramic*, 3, 67-73.
- Hench, L. L., and Ethridge, E. C. (1982). *Biomaterials: An Interfacial Approach*. New York: Academic Press.
- Hench, L. L., Splinter, R. J., Allen, W. C., and Greenlee, T. K. (1971). Bonding mechanism at the interface of ceramic prosthetic materials. *Journal of Biomedical Materials*, 2, 171-141.
- Hench, L., and Wilson, J. (1993). *An Introduction to Bioceramics*. London: World Scientific.
- Hing, K. (2005). Bioceramics bone graft substitutes: influence of porosity and chemistry. *International Journal of Applied Ceramic Technology*, 2, 184-199
- Hing, K. A., Best, S. M., and Tanner, K. A. (1999). Quantification of bone ingrowth within bone derived porous hydroxyapatite implants of varying density. *Journal of Material Science: Materials in Medical*, 10(10), 663-670.
- Huppmann, W, J. (1975). *Sintering and Catalysis*. New York: Plenum Press.
- Izadi, S., Hesaraki, S., and Ardakani, M. H. (2014). Evaluation nanostructure properties of bioactive glass scaffolds for bone tissue engineering. *Advanced Material Research*, 829, 289-293.
- Jonghe, L. C. D., and Rahaman, M. N. (2003). *Sintering of Ceramics*. New York: Elsevier.
- Julian, R. J. (2009). New trends in bioactive scaffolds: the importance of nanostructure. *Journal European Ceramic Society*, 29, 1275-1281.
- Jurczyk, K., Niespodziana, K., Jurczyk, M, U., and Jurczyk, M. (2011). Synthesis and characterization of titanium-4555 bioglass nanocomposites. *Materials and Design*, 32, 2554-2560.

- Kammler, H. K., Madler, L., and Pratsinis, S. E. (2001). Flame synthesis of nanoparticles. *Chemical Engineering and Technology*, 24(6), 583-596.
- Kang, S. J. L. (2005). *Sintering: Densification, Grain Growth and Microstructure*. Oxford: Elsevier.
- Kang, S. J. L., Lee, M. G. and An, S. M. (2009). Microstructural evolution during sintering with control of the interface structure. *Journal American Ceramic Society*, 92(7), 1464-1471.
- Kangasniemi, I., Groot, D. K., Wolke, J., Luklinska, Z., Becht, J. G. M., Lakkisto, M., and Urpo, Y. A. (1991). The stability of hydroxyapatite in an optimized bioactive glass matrix at sintering temperatures. *Journal Material Science*, 20, 133-137.
- Kapoor, S., and Batra, U. (2010). Preparation and bioactivity evaluation of bone like hydroxyapatite-bioglass composite. *International Journal of a Civil, Environmental, Structural, Construction and Architectural Engineering*, 4(1), 37-41.
- Katz, J. L. (1980). *The Mechanical Properties of Biological Materials*. Cambridge: Cambridge University Press.
- Killion, J. A., Kehoo, S., and Higginbotham, C. L. (2013). Hydrogel/bioactive glass composites for bone regeneration applications: synthesis and characterisation. *Material Science and Engineering C*, 33(7), 4203-4212.
- Kim, H. W., Koh, Y. H., Yoon, B. H., and Kim, H. E. (2002). Reaction sintering and mechanical properties of hydroxyapatite-zirconia composites with calcium fluoride additions. *Journal American Ceramic Society*, 85(6), 1634-1636.
- Kim, S. K., Kim, Y. S., Bang, H. G., and Park, S. Y. (2007). Synthesis of bio-glass ceramics in $\text{Na}_2 - \text{CaO} - \text{SiO}_2 - \text{P}_2\text{O}_5$ system with fluoride additives. *Solid State Phenomena*, 124-126, 759-762.
- Kiran, P., Udayanshankar, N. K., and Shashikata, H. D. (2016). The effective role of P_2O_5 on structural and morphological properties of $\text{SiO}_2 - \text{CaO} - \text{P}_2\text{O}_5$ dried gels. *International Advanced Research Journal in Science, Engineering and Technology*, 3(12), 179-182.
- Kivrak, N., and Tas, A. C. (1998). Synthesis of calcium hydroxyapatite tricalcium phosphate (HA-TCP) composite bioceramics powders and their sintering behavior. *Journal of the American Ceramic Society*, 81(9), 2245-2252.
- Ko, C. C., Kohn, D. H., and Hollister, S. (1995). Micromechanics of implants/tissue interfaces. *Journal Oral Implantol*, 18, 220-230.
- Kokubo, T., Huang, Z. T., Sakka, S., Kitsugi, T., and Yamamura, T. (1993). Ca-P-rich layer formed on high-strength bioactive glass-ceramic A-W. *Journal Biomedical Material Research*, 24(3), 31-43.

- Komath, M., and Varma, H. K. (2003). Development of fully injectable calcium phosphate cement for orthopaedic and dental applications. *Bulletin of Materials Science*, 26, 415-422.
- Kumar, G. S., Thamizharel, A., and Girija, E. K., (2012). Microwave conversion of eggshells into flower-like hydroxyapatite nanostructured for biomedical applicationn. *Materials Letters*, 76, 198-200.
- Kumar, M. (2010). *Study of optical and structural properties of silicon borate glasses*, Master Thesis, Thapar University.
- Kutbay, I., Yilmaz, B., Evis, Z., and Usta, M. (2014). Effect of calcium fluoride on mechanical behavior and sinterability of nano-hydroxyapatite and titania composites. *Ceramics International*, 40, 14817-14826.
- Lee, E., Kim, H., and Kim, H. (2006). Production of hydroxyapatite/bioactive Glass Biomedical composites by the Hot-Processing technique. *Journal of the American Ceramic Society*, 89(11), 3593-3596.
- Lee, S, M and Kang, S, J. (1998). Theoretical analysis of liquid-phase sintering pore filling theory. *Acta Material*, 46(9), 3191-3202.
- Lefebvre, L, Chevalier, J., Gremillard, Zenati, R., Thollet, G., Assolant, D. B., and Govin, A. (2007). Structural transformation of bioactive glass 45S5 next term with thermal treatments. *Acta Materialia*, 55(10), 3305-3313.
- Lefebvre, L., Gremillard, L., Chevalier, J., and Assolant, D. B. (2008). Sintering behavior of 45S5 bioglass. *Key Engineering Materials*, 361, 265-268.
- Legeros, R. Z., Silverstone, L. M., Daculsi, G., and Kerebel, L. M. (1983). In vitro caries- like lesion formation in F-containing tooth enamel. *Journal Dental Research*, 62, 138-144.
- Li, H. C., Wang, D. G., Hu, J. H., and Chen, C, Z. (2014). Influences of fluoride additions on biological and mechanical properties of $\text{Na}_2\text{O} - \text{CaO} - \text{SiO}_2 - \text{P}_2\text{O}_5$ glass ceramics. *Materials Science and Engineering C*, 35, 171-178.
- Lin, L., Zhang, L., Wang, J., Xie, K., Yang, X., Chen, X., Yang, G., and Gau, Z. (2014). Low temperature sintering of 45555 bioglass-based glass ceramics: effects of biphasic mixing approach on the mechanical and biological properties. *Materials Letters*, 126, 154-158.
- Liu, D. M. (1997). Influence of porosity and pore size on the compressive strength of porous hydroxyapatite ceramic. *Ceramics International*. 23(2), 135-139.
- Liu, D. M., Troczynsk., and Tseng, W. J. (2001). Water-based sol-gel synthesis of hydroxyapatite: process development. *Biomaterials*, 22, 1721-1730.

- Liu, F. H. (2012). Synthesis of bioceramics scaffold for bone tissue engineering by rapid prototyping technique. *Journal Sol-Gel Science Technology*, 64, 704-710.
- Liu, H., and Webster, T. J. (2007). Nanomedicine for implants: a review of studies and necessary experimental tools. *Biomaterials*, 28(2), 354-369.
- Liu, Z., Huang, H., Guo, X., Yu, H., Zhong, X., Zhu, J., and Zeng, D. (2011). Microstructure and property evolution of isotropic and anisotropic NdFeB magnets fabricated from nanocrystalline ribbons by spark plasma sintering and hot deformation. *Journal Physics D*, 44(2), 25-30.
- Lopez, M. A., Monteiro, F. J., and Santos, J. D. (1999a). Glass reinforced hydroxyapatite composite: fracture toughness and hardness dependence on microstructural characteristics. *Biomaterials*, 20(21), 2085-2090.
- Lopez, M. A., Monteiro, F. J., and Santos, J. D. (1999b). Glass-reinforced hydroxyapatite composite: secondary phase proportions and densification effect on a biaxial bending strength. *Journal Biomedical Material Research*, 48(5), 734-740.
- Lopez, M. A., Monteiro, F. J., and Santos, J. D. (2002). Microstructural dependence of young's and shear moduli of P₂O₅ glass reinforced hydroxyapatite for biomedical application. *Biomaterials*, 21(7), 749-754.
- Lupulescu, A. C., and Glicksman, M. E. (2000). Diffusion-limited crystal growth in silicate systems: similarity with high-pressure liquid-phase sintering. *Journal Crystal Growth* 211, 49-61.
- Ma, J., Chen, C. Z., Wang, J. Z., and Shi. (2010). Textural and structural studies of sol-gel derived SiO₂ – CaO – P₂O₅ – MgO glasses by substitution MgO and CaO. *Material Science Engineering C*, 30, 886-890.
- Ma, P. X., and Choi, J. W. (2001). Biodegradable polymer scaffolds with well defined interconnected spherical pore network. *Tissue Engineering*, 7, 23-33.
- Majhi, M. R., Pyare, R., and Singh, S. P. (2011). Studies on preparation and characterizations of CaO – Na₂O – SiO₂ – P₂O₅ bioglass ceramics substituted with Li₂O, K₂O, ZnO, MgO and B₂O₃. *International Journal of Scientific and Engineering Research*, 2(9), 1-9.
- Mami, M., Oudadesse, H., and Sridi, D. R. (2008). Synthesis and vitro characterization of melt derived 47S CaO – P₂O₅ – SiO₂ – Na₂O bioactive glass. *Ceramic-Silikaty*, 52(3), 121-129.

- Martin, R. A., Twyman, H., Qiu, D., Knowles, J.C., and Newport, R. J. (2009). A study of the formation of amorphous calcium phosphate and hydroxyapatite on melt quenched bioglass using surface sensitive shallow angle X-ray diffraction. *Journal Materials Science: Material Medical*, 20, 883-888.
- Martin, R. B. (1999). Bone as a ceramic composite material. *Material Science Forum*, 7(1), 5-16.
- Martin, R. I., and Brown, P. W. (1995). Mechanical properties of hydroxyapatite formed at physiological temperature. *Journal Material Science, Material and Medical*, 6(3), 138-143.
- Mehdikhani, B., and Borhani, G. H. (2013). Crystallization behaviour and microstructure of bioglass ceramic system. *International Letter of Chemistry, Physics and Astronomy*, 19, 58-68.
- Miao, S., Weng, W., and Cheng, K. (2007). In-vitro bioactivity and osteoblast-like cells test on zinc containing fluoridated hydroxyapatite films. *Journal of Materials Science: Materials in Medicine*, 18, 2101-2105.
- Miao, X. (2003). Observation of microcraks formed in HA-316L composites. *Materials Letter*, 57(12), 1848-1857.
- Mirhadi, B., and Mehdikhani, B. (2012). Effect of calcium fluoride on sintering behavior of $\text{SiO}_2 - \text{CaO} - \text{Na}_2\text{O} - \text{MgO}$ glass ceramic system. *Processing and Application of ceramics*, 6(3), 159-164.
- Monmaturapoj, N., and Yatonchai, C. (2010). Effect of sintering on microstructure and properties of hydroxyapatite produced by different synthesizing method. *Journal of Metals, Materials and Minerals*, 20(2), 53-61.
- Nandi, S. K., Kundu, B., and Dutta, S. (2011). *Biomaterials Applications for Nanomedicine*. Croatia: InTech Open Science.
- Natasha, A. N., Asep, S. F., Alqab., and Lis, S. (2011). Recent progress on hydroxyapatite-based dense biomaterials for load bearing bone substitutes. *Recent patents on Materials Science*, 4, 63-80.
- Nia, A. F. (2013). Preparation of apatite-wollastonite-phlogopite glass-ceramic composites by powder sintering method. *Science of Sintering*, 45, 331-339.
- Nilen, R. W., and Richter, P. W. (2008). The thermal stability of hydroxyapatite in biphasic calcium phosphate ceramic. *Journal Material Science Material Medical*, 19(4), 1697-1702.

- Noaman, A., Rawlinson, S. C. F., and Hill, R. G. (2012). The influence of CaF_2 content on the physical properties and apatite formation of bioactive glass coatings for dental implants. *Journal of Non-Crystalline Solids*, 358, 1850-1858.
- Oksiuta, Z., Dabrowski, J. R., and Olszyna, A. (2009). Co-Cr-Mo-based composite reinforced with bioactive glass. *Journal of Materials Processing Technology*, 209(2), 978-985.
- Oktar, F. N. (2007) Microstructure and mechanical properties of sintered enamel hydroxyapatite. *Ceramics International*, 33, 1309-1314.
- Oktar, F. N., and Goller, G. (2002). Sintering effects on mechanical properties of glass reinforced hydroxyapatite composites. *Ceramics International*, 28, 617-621.
- Orlovskii, V. P., Ionov, S. P., and Rusakora, R. A. (1992). Hydroxyapatite phase relations in the system $\text{CaCl}_2\text{-(NH}_4)_2\text{HPO}_4\text{-NH}_4\text{OH-H}_2\text{O}$. *Dokl Akad Nauk*, 325(5), 522-525.
- Orlovskii, V. P., Komlev, V. S., and Barinov, S. M. (2002). Hydroxyapatite and hydroxyapatite-based ceramics. *Inorganic material*, 38(10), 973-984.
- Padilla, S., Roman, J., Salcedo, S., and Regi, M. V. (2006). Hydroxyapatite/ SiO_2 – $\text{CaO} - \text{P}_2\text{O}_5$ glass materials: In-vitro bioactivity and biocompatibility. *Acta Biomaterialia*, 2, 331-342.
- Pallan, N. F., Matori, K. A., Lim, W. F., Quah, H. J., Fauzana, A. N., Rosnah, N., Khiri, M. Z. A., Farhana, S., Norhazlin, Z., Zarifah, N. A., Nurzilla, M., Hafiz, M. Z., Loy, C. W., and Zamratul, M. I. M. (2016). Preparation of $\text{SiO}_2\text{-Na}_2\text{O-CaO-P}_2\text{O}_5$ glass-ceramic from waste materials and heat treatment effects on its morphology. *Materials Science Forum*, 846, 189-192.
- Park, J., and Lakes, R. S. (1992). *Biomaterials: An Introduction*. New York: Plenum Press.
- Peitl, O., Zanutto, E. D., and Hench, L. L. (2012). Compositional and microstructural design of highly bioactive $\text{P}_2\text{O}_5\text{-Na}_2\text{O-CaO-SiO}_2$ glass-ceramics. *Acta Biomaterial*, 8(1), 321-332.
- Rajendran, V., Begum, A. N., Azooz, M. A., and Batal, F. H. E. (2002). Microstructural dependence on relevant physical-mechanical properties of $\text{SiO}_2 - \text{Na}_2\text{O} - \text{CaO} - \text{P}_2\text{O}_5$ biological glasses. *Biomaterials*, 23, 4263-4275.
- Ramesh, S., Tan, C. Y., Baiduri, S. B., and Teng, W. D. (2007). Rapid densification of nanocrystalline hydroxyapatite for biomedical application. *Ceramic International*, 33, 1363-1367.

- Rameshbabu, N., Kumar, T. S. S., and Rao, K. P. (2006). Synthesis of nanocrystalline fluorinated hydroxyapatite by microwave processing and its in vitro dissolution study. *Bulletin of materials Science*, 29, 611-615.
- Ravarian, R., Moztarzadeh, F., Hashjin, M. S., Rubiee, S. M., Khoshakhlagh, P., and Tahriri, M. (2010). Synthesis, characterization and bioactivity investigation of bioglass-hydroxyapatite composite. *Ceramics International*, 36, 291-297.
- Rezwan, K., Chen, Q., Blaker, J., and Boacaccini, A. (2006). Biodegradable and bioactiveporous polymer/inorganic composite scaffolds for bone tissue engineering. *Biomaterials*, 27, 3413-3431.
- Rich, J., Jaakkola, T., Tirri, T., Narhi, T., Urpo, A. Y., and Sepphala, J. (2002). In vitro evaluation of polymer/bioactive glass composites. *Biomaterials*, 23, 2143-2150.
- Rizkalla, A. S., Jones, D. W., Clarke, D. B., and Hall, G. C. (1996). Crystallization of experimental bioactive glass composition. *Journal of biomedical materials research part A*, 32(1), 119-124.
- Sandler, N., and Lammens, R. F. (2011). Pneumatic dry granulation: potential to improve roller compacting technology in drug manufacture. *Expert Opin Drug Delivery*, 8(2), 225-236.
- Santos, C., Souza, R. C., Habibe, A. F., Maeda, L. D., Barboza, M. J. R., and Elias, C. N. (2008). Mechanical properties of Y-TPZ ceramics obtained by liquid phase sintering using bioglass as additive. *Materials Science and Engineering*, 478, 257-263.
- Santos, J. D., Knowles, J. C., Reis, R. L., Monteiro., and Hastings, G. W. (1994). Microstructural characterization of glass-reinforced hydroxyapatite composites. *Biomaterials*, 15(1), 5-10.
- Santos, J. D., Reis, R. L., and Monteiro, F. J. (1995). Liquid phase sintering of hydroxyapatite by phosphate and silicate glass additions: structure and properties of the composites. *Journals of Materials Science: Materials in Medicine*, 6, 348-352.
- Sarker, B., Hum, J., Nazhat, S. N., and Boccaccini. (2014). Combining collagen and bioactive glasses for bone tissue Engineering. *Advanced Healthcare Materials*, 4(2), 176-194.
- Sebdani, M, M., and Fathi, M. (2012). Preparation and characterization of hydroxyapatite-fosferite-bioactive glass nanocomposite coatings nanopowder for biomedical applications. *Ceramics International*, 38(2), 1325-1330.

- Seo, D. S., Hwang, K. H., and Lee, J. K. (2008). Nanostructured hydroxyapatite by microwave sintering. *Journal Nanoscience Nanotechnology*, 8, 944-948.
- Shankwar, N., Kumar, M., and Srinivasan, A. (2016). Novel polyvinyl alcohol-bioglass 45S5 based composite nanofibrous membranes as bone scaffolds. *Materials Science and Engineering C*, 69, 1167-1174.
- Shelby, J. E. (2007). *Introduction to Glass Science and Technology*. Cambridge: Royal Society and Chemistry.
- Sinha, A., Ingle, A., Munim, K. R., Viadya, S. N., Sharma, B. P., and Bhisey, A. N. (2001). Development of calcium phosphate based bioceramics. *Bulletin Material Science*, 24, 653-657.
- Sinha, A., Mishra, T., and Ravishkandar, N. (2008). Polymer assisted hydroxyapatite microspheres suitable for medical applications. *Journal Material Science Medical*, 19, 2009-2013.
- Suchanek, W., and Yoshimura, M. (1998). Processing and properties of hydroxyapatite-based biomaterials for use as hard tissue replacement implants. *Journal of Materials Research*, 13(1), 94-117.
- Tan, C. Y., Ramesh, S., Hamdi, M., and Sopyan, I. (2006). *3rd International Conference on Biomedical Engineering: Selected Papers from the Conference Held in Kuala Lumpur*. Springer.
- Tancred, D. C., McCormack, A. J. (1998). A quantitative study of the sintering and mechanical properties of hydroxyapatite/phosphate glass composites. *Biomaterials*, 19, 1735-1743.
- Tang, C. Y., Uskokovic, P. S., Tsui, C. D., Veljovic, D., Petrovic, R., and Janakovic, D. (2009). Influence of microstructure and phase composition on the nanoindentation characterization of bioceramics materials based on hydroxyapatite. *Ceramics International*, 35, 2171-2178.
- Tavangarian, F., and Emadi, R. (2011). Preparation of bioactive nanostructured scaffold with improved compressive strength. *Ceramics-Silikaty*, 55(1), 49-53.
- Thamaraiselvi, T. V., and Rajeswari, S. (2004). Biological evaluation of bioceramic materials - a review. *Trends Biometal Artificial Organs*. 18(1), 9-17.
- Theodorou, G., Goudouri, O. M., Kontonasaki, E., Chatzistarrou, X., Papadopolou, L., Kantiranis, N., and Paraskevopoulos, K. M. (2011). Comparative bioactivity study of 4555 and 585 bioglasses in organic and inorganic environment. *Bioceramics Development and Application*, 1, 1-4.
- Thompson, I., and Hench, L. (1998). Mechanical Properties of bioactive glasses, glass-ceramics and composites. *Journal of Engineering in Medicine*, 212(2), 127-136.

- Touri, R., Moztaarzadeh, F., Sadeghian, Z., Bizari, D., Tahriri, M., and Mozafari, M. (2013). The use of carbon nanotubes to reinforce 45S5 bioglass-based scaffolds for tissue engineering applications. *Biomedical Research International*, 2013, 1-8.
- Vichery, C., and Nadelec, J. M. (2016). Bioactive glass nanoparticles from synthesis to materials design for medical applications. *Materials*, 9, 1-17.
- Vinet, A., and Caine, M. (2012). Development of traction features in sprint spikes SLS nylon sole units. *Procedia Engineering*, 2, 2769-2774.
- Wan, Y., Cui, T., Li, W., Li, C., Xiao, J., Zhu, Y., Xiong, G., and Luo, H. (2016). Mechanical and biological properties of bioglass/magnesium composite prepared via microwave sintering route. *Materials and Design*, 99, 521-527.
- Wang, C. K., Ju, C. P., and Lin, J. H. C. (1998). Effect of doped bioactive glass on structure and properties of sintered hydroxyapatite. *Material Chemistry Physic*, 53(2), 138-149.
- Wang, L. L., Wang, X. F., Ding, X., and Jiang, H. T. (2013). Preparation of HA-Bioglass- Al_2O_3 biological composite. *Materials and Manufacturing Process*, 8(9), 980-983.
- Wang, L. L., Wang, X. F., Xu, D., and Zhu, J. F. (2012). Sintering behaviour and property of bioglass modified HA- Al_2O_3 composite. *Science of Sintering*, 44, 265-270.
- Wang, L. L., Wang, X. F., Zhu, J. F., and Yu, C. L. (2011). The effects of calcium fluoride addition on crystallization characteristics of hydroxyapatite-zirconia composites. *Advanced Materials Research*, 197, 74-78.
- Wei, W., Chen, K., and Ge, U. (2013). Strongly coupled nanorod vertical arrays for plasmonic sensing. *Advance Material*, 25, 3863-3868.
- Yang, X., Zhang, L., Chan, X., Sun, X., Yang, G., Guo, X., Yang, H., Gao, C., and Gou, Z. (2012). Incorporation of B_2O_3 in $\text{CaO} - \text{SiO}_2 - \text{P}_2\text{O}_5$ bioactive glass system for improving strength of low-temperature co-fired porous glass ceramics. *Journal of Non-Crystalline Solids*, 358, 1171-1179.
- Younger, E. M., and Chapman, M. W. (1989). Morbidity at bone graft donor sites. *Journal Orthopaedic Trauma*, 3, 192-195.
- Yuan, H., and Groot, K. D. (2005). *Learning from Nature How to Design New Implantable Biomaterials*. Portugal: Springer Science and Business Media.
- Zeimarau, E., Sara, P., Ivan, D., Belinda, P. M., Kadri, N. A., and Towler, M. R. (2015). Bioactive glass reinforced elastomer composites for skeletal regeneration: a review. *Materials Science and Engineering C*, 53, 175-188.

- Zheng, W. (2010). *Preparation and characterization of tri-calcium phosphate scaffolds with tunnel-like macro-pores for bone tissue engineering*, Master Thesis, Queensland University of Technology.
- Zhou, Y., Li, H., Lin, K., Zhai, W., Gu, W., and Chang, J. (2012). Effect of heat treatment on the properties of $\text{SiO}_2 - \text{CaO} - \text{MgO} - \text{P}_2\text{O}_5$ bioactive glasses. *Journal Material Science Material Medical*, 23, 2101-2108.
- Zhu, R., Yu, R., Yao, J., and Wang, D. L. (2008). Morphology control of hydroxyapatite through hydrothermal process. *Journal Alloy composite*, 457(1-2), 555-559.
- Zia, R., Riaz, M., and Afifa, A. (2017). The effects of K_2O on the microstructure of $\text{Na}_2\text{O}-\text{CaO}-\text{P}_2\text{O}_5-\text{SiO}_2$ based ceramics systems. *Optic-International Journal for Light and Electron Optics*, 129, 15-20.
- Zilm, M., Thomson, S. D., and Wei, M. (2015). A comparative study of the sintering behaviour of pure and manganese - substituted hydroxyapatite. *Materials*, 8, 6419-6436.
- Zouai, S., Harabi, A., Karbou, N., Harabi, E., Chehlatt, S., Barama, S. E., Zaioui, S., Bouzerara, F., and Guerta, F. (2016). A new and economic approach to synthesize and fabricate bioactive dropside ceramics using a modified domestic microwave oven. Part 2: Effect of P_2O_5 addition on dropside bioactivity and mechanical properties. *Materials Science and Engineering C*, 61, 553-563.