

UNIVERSITI PUTRA MALAYSIA

DESIGN OF CMOS POTENTIOSTAT FOR LOW-CONCENTRATION HEAVY METAL DETECTION

MEHRAN RAEISINAFCHI

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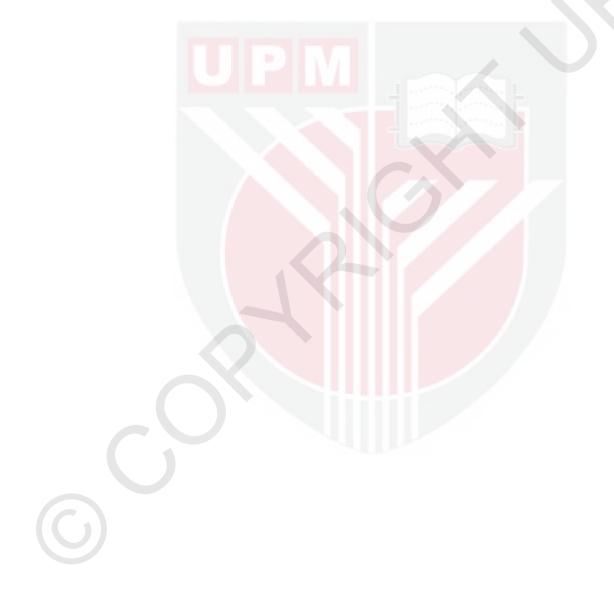
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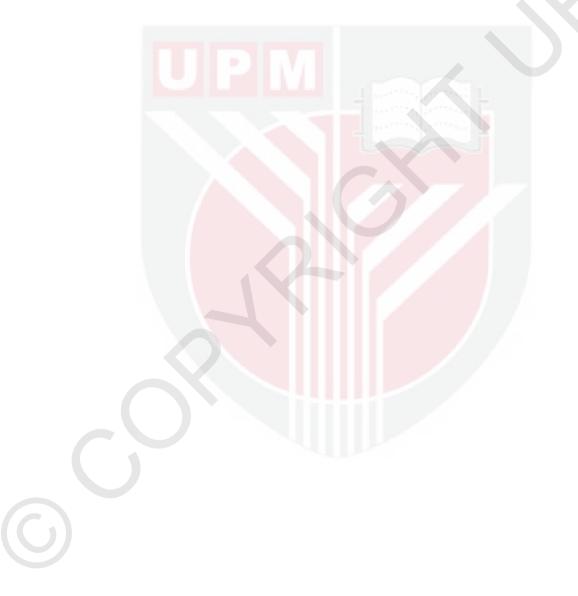
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DEDICATION

First and foremost I would like to thank God, my creator, for giving me the intellectual capacity to learn about His creation. I dedicate my thesis work to my loving parents, KEFAYAT and BAHMAN, whose words of encouragement and push for tenacity ring in my ears. In addition, I have a special feeling of gratitude to my loving brother(Mehdi) and sister(Sara) for supporting me entire my life. I also dedicate this grateful work to my loving wife, BITA whose motivate me to complete my research efficiently. I also would like to thanks her for love, encouragement, admiration, kindness and support.



Abstract of thesis presented to the Senate of Universiti Putra Malaysia in fulfilment of the requirement for the degree of Master of Science

DESIGN OF CMOS POTENTIOSTAT FOR LOW CONCENTRATION HEAVY METAL DETECTION

By

MEHRAN RAEISINAFCHI

August 2015

Chairman: Assoc. Prof. Roslina bt. Mohd. Sidek, PhDFaculty: Engineering

Metal toxicity is a critical concern in both human and ecosystem health. Many heavy metals are lethal at high concentration. They can also be harmful at trace concentration since accumulating such materials in human organs lead to long-term negative health effects such as heart disease and high blood pressure. Therefore, heavy metal detection of trace concentration is very important. Electrochemical detection system consists of electrodes as transducer, potentiostat as electrical signal detector and data converter for signal processing blocks. The potentiostat detects and amplifies the current generated by the transducer, and it controls the potential of the electrodes. With the advancement of micro- and nano-technology, microelectrochemical system provides feasible solution for sensitive detection and miniaturized platform.

Studies have shown that to detect trace concentration of heavy metals, the potentiostat should be able to detect low current typically in the range of nA to μA and a different types of heavy metals can be detected at the potential between -1V and +1V. Researchers have developed CMOS- based potentiostat for detection of limited type of heavy metals and current detection level in µA range using CMOS technology nodes of 0.18µm and above. The research is aimed to design a potentiostat that can detect nA to μ A range current and -1V to +1V range of the voltage using $0.13\mu m$ CMOS technology with ± 1.2 V supply voltage. By using down-scaled technology, the area consumption is expected to decrease. Dual power supply of $\pm 1.2V$ are used in the design to detect the potential between -1V to +1V. To ensure the linearity of output signal, the potentiostat is designed using fully differential operational amplifier and rail-to-rail common-mode range buffer. A new circuit configuration is also proposed to read nA range of current. By using downscaled 0.13 μ m CMOS technology, the physical layout is reduced to 0.041mm², about 10 times smaller than design area reported particularly using 0.18µm CMOS technology. The post-layout simulation results shows that the proposed design is able to read the input current in the range of nA to μ A. The linearity is $R^2 = 0.999$ and also the maximum voltage swing obtained is 2.4 V from -1.2V to +1.2V. The Signal to Noise Ratio (SNR) of CMOS potentiostat for 1nA and 1uA sensor current is equal to 38.91 dB and 47.96 dB, respectively. The circuit developed in this

research is verified by using published experimental data for $3mgL^{-1}$ Cu(II) and 0.6 mM Cd(II). The results shows that the values of current peaks and potentials at which current peaks occur are close to experimental results for these types of heavy metals.



Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Master Sains

REKA BENTUK POTENTIOSTAT CMOS UNTUK PENGESANAN LOGAM BERAT KEPEKATAN RENDAH

Oleh

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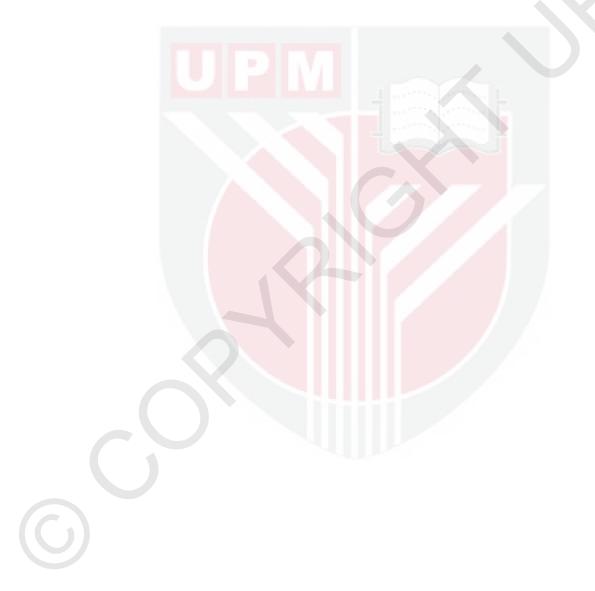
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Ketoksikan logam adalah satu isu yang penting dalam kehidupan manusia dan kesihatan ekosistem. Banyak logam berat merbahaya pada kepekatan yang tinggi. Ia juga merbahaya pada konsentrasi rendah, oleh kerana pengumpulan bahan-bahan berkenaan dalam organ badan manusia boleh membawa kepada kesan negatif jangka panjang pada kesihatan seperti sakit jantung dan tekanan darah tinggi. Oleh itu, pengesanan logam berat pada konsentrasi rendah sangatlah penting. Sistem pengesanan elektrokimia terdiri dari elektrod sebagai transduser, potentiostat sebagai pengesan isyarat elektrik dan pengubah data untuk blok pemprosesan isyarat. Potentiostat mengesan dan menguatkan lagi arus yang dijana oleh transduser dan ia mengawal potensi elektrod. Dengan kemajuan makro dan nano-teknologi, sistem mikro-elektrokimia memberikan satu kaedah penyelesaian yang praktikal untuk pengesanan sensitif dan landasan bersaiz kecil.

Kajian telah menunjukkan bahawa untuk mengesan logam berat berkepekatan rendah, potentiostat dapat mengesan arus yang lebih rendah biasanya dalam lingkungan nA ke µA dan pelbagai logam berat boleh dikesan pada potensi antara -1V dan +1V. Penyelidik telah membangunkan potentiostat berasaskan CMOS untuk mengesan logam berat dan tahap pengesanan arus dalam jalat µA menggunakan nod teknologi CMOS dari 0.18µm dan ke atas. Kajian ini bertujuan untuk mereka bentuk potentiostat yang boleh mengesan julat arus dari nA kepada μ A dan julat voltan dari -1V kepada + 1V julat voltan yang menggunakan teknologi CMOS 0.13µm dengan voltan bekalan ±1.2V. Dengan menggunakan teknologi berskala rendah, penggunaan kawasan ini dijangka akan berkurangan. Dua bekalan kuasa ± 1.2V digunakan dalam reka bentuk untuk mengesan potensi antara -1V ke +1V. Untuk memastikan kelelurusan isyarat keluaran, potentiostat direka menggunakan penguat operasian kebezaan penuh dan penimbal mod sepunga landasan ke landasan. konfigurasi litar baru juga dicadangkan untuk membaca arus dalam julat nA. Dengan menggunakan teknologi berskala rendah CMOS 0.13µm, bentangan fizikal dikurangkan kepada 0.041 mm^2 , kira-kira 10 kali lebih kecil daripada kawasan reka bentuk dilaporkan terutamanya menggunakan teknologi CMOS 0.18µm. Keputusan simulasi pasca susun atur menunjukkan bahawa reka bentuk yang dicadangkan mampu untuk membaca arus masukan dalam julat nA ke μ A. kelelurusan ialah R^2 =



0.999 dan juga voltan maksimum diperolehi ialah 2.4 V daripada -1.2V kepada +1.2V. Isyarat kepada Nisbah Bunyi (SNR) daripada CMOS potentiostat untuk 1nA dan 1uA sensor arus semasa adalah sama dengan 38.91 dB dan 47.96 dB. Litar yang dibangunkan dalam kajian ini disahkan dengan menggunakan diterbitkan data eksperimen untuk $3mgL^{-}$ Cu (II) dan 0.6 mM Cd (II). Keputusan menunjukkan bahawa nilai puncak arus dan potensi hampir dengan keputusan eksperimen untuk jenis logam berat tersebut.



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Roslina bt. Mohd. Sidek, PhD Associate Professor Faculty of Engineering Universiti Putra Malaysia (Chairman)

Maryam Binti Mohd Isa, PhD Senior Lecturer Faculty of Engineering Universiti Putra Malaysia

(Member)

BUJANG BIN KIM HUAT, PhD Professor and Dean School of Graduate Studies Universiti Putra Malaysia

Date:

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LIST OF ABBREVIATIONS

A_V	Differential Gain
A_{cm}	Common Mode Gain
C_{C}	Double Layer capacitance associated with the
C_C	Counter Electrode
C	
C_W	Double Layer capacitance associated with the
.	Working Electrode
I_f	Faradic Current
R_{C}	Faradic Resistance
V_{ref}	Reference Voltage
ADC	Analog to Digital Converter
ASV	Anodic stripping Voltammetry
Cd	Cadmium
CE	Counter Electrode
CMOS	Complementary Metal Oxide Semiconductor
CMRR	Common Mode Rejection Ratio
Cu	Copper
CV	Cyclic Voltammetry
DAC	Digital to Analog Converter
DPASV	Differential Pulse Anodic Stripping
	Voltammetry
DPV	Differential Pulse Voltammetry
FD	Fully Differential
Hg	Mercury
ITRS	International Technology Roadmap for
	Semiconductor
Ni	Nickel
OP	Operational Amplifier
Pb	Lead
RE	Reference Electrode
SE	Single Ended
TIA	Trance Impedance Amplifier
Vb	Bias Voltage
VCMFB	Common Mode Feedback Voltage
VDD	Positive supply voltage
Vo	Output Voltage
VSS	Negative supply voltage
WE	Working electrode
Vcell	Cell Voltage
	č

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CHAPTER 1

INTRODUCTION

1.1 CMOS Technology for Monitoring System

Developments in Complementary Metal Oxide Semiconductor (CMOS) processing technologies and biomedical sensors have led to the realization of monitoring devices such as implantable biosensors for monitoring patients for example to reduce the risk of poison [1, 2]. The integration of transistor with CMOS technology enables development of miniaturized systems with higher throughput, lower cost and reliable performances. Figure 1.1 illustrates the overview of CMOS technology in patients monitoring. Hence, several physiological phenomena are monitored by body sensors. Then the data sent to a personal server through the internet. As the data is stored in a medical server, long term and short term patient term patient treatment can be optimized based on the medical history.

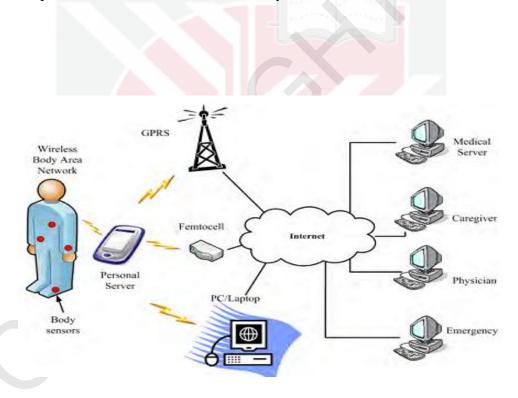


Figure 1.1 Overview of Patient Monitoring System based on CMOS Technology[2]

Economic and functional needs stimulate a progressive increase of the number of transistors integrated on a single chip. Until now the electronic technologies have been able to satisfy these needs through dimension scaling and reliability improvement of electronic components. Figure 1.2 shows the International Technology Roadmap for Semiconductor (ITRS) [3]. According to ITRS, Scaling (which is also known as more Moore) refers to not only the continued shrinking of transistors but also includes non-geometrical process techniques such as study of new materials that affect the electrical performance of the chip, as well as design technologies that enable high performance, high reliability, low cost, and high design productivity. Functional diversification (which is also known as more than Moore) aims to provide additional value, in particular non-digital functionalities (Analog/RF communication), to be migrated from the system board level into package-level (system-in-package, SiP) or chip-level (System-on-Chip, SoC) [4].

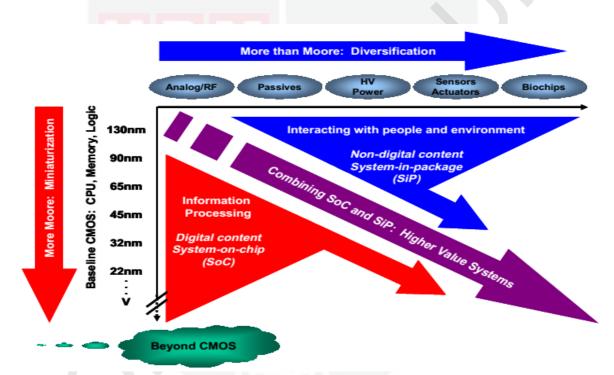


Figure 1.2 International Technology Roadmap for Semiconductor (ITRS)[3]

In environmental application CMOS technology is used for monitoring and measuring electrochemical analaytes. Figure 1.3 illustrates the block diagram of the electrochemical instrumentation system [5]. This electrochemical instrument includes electrochemical sensor, data conversion, microcontroller and potentiostat. Basically, a potentiostat has two main functions, controlling the potential difference between working electrode (WE) and reference electrode (RE) and measuring the current flowing between working electrode and counter electrode. The signal is generated by the microcontroller in digital form and is then converted to analogue form using a digital to analogue converter (D/A) [6]. It is applied to the counter electrode (CE) and reference electrode (RE) via a potentiostat which acts to control the applied potential. The signal output, in the form of a current, is obtained from working electrode (WE).

In the data acquisition process, the current is digitized by an analog to digital converter (A/D) under the control of the microcontroller. These binary numbers are then stored in the microcontroller memory for storage and further processing.

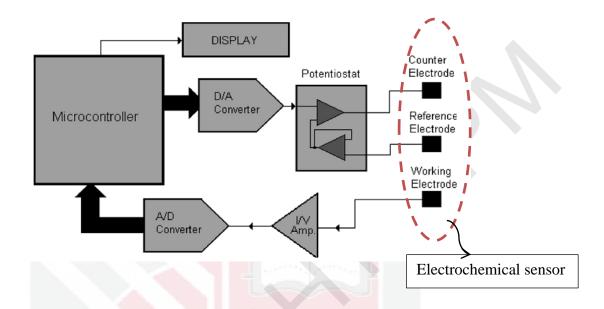


Figure 1.3 Block Diagram of the Electrochemical Instrumentation System[5]

1.2 Heavy Metal

Metal toxicity is a critical concern in both human and ecosystem health. Many heavy metals are lethal at high concentrations. They can also be harmful at trace concentration since accumulating such materials in human organs lead to long-term negative health effects such as heart disease and high blood pressure [7-9]. Heavy metals are namely mercury, lead, cadmium, nickel. Danger of heavy metals is their ability for bioaccumulation. Some heavy metals may also play a role in the development of various cancers. Environmental pollution from industry is the main source of high amount of heavy metals in the environment. In fact, after the penetration of these metals into the body, they accumulate in tissues such as fat, muscle, bones and joints and cause many diseases and bring various other aggravating problems to human [10, 11]. As is shown in the following Figure 1.4, the accumulation of heavy metals in the human body is often associated with some complications as in the following: Getting cold feet, immunodeficiency, skin rashes, digestive problems, fatigue, heart disease, high blood pressure, irritability, allergy, forgetfulness and dizziness.



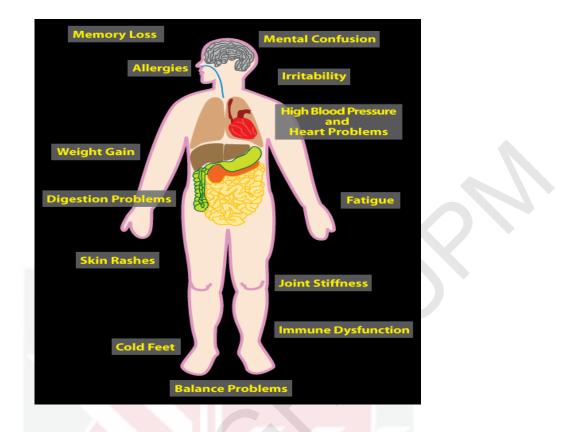


Figure 1.4 Human problems Caused by Accumulation Heavy Metals in Body

1.3 Problem Statement

Researchers have developed potentiostat based on CMOS technology but for the detection of limited type of heavy metals and current detection level in μ A range [18, 46]. In order to detect trace concentration of heavy metals, the potentiostat should be able to detect lower current typically in the range of nA to μ A. Therefore, previous CMOS potentiostat due to detection current in μ A range cannot be used for low concentration heavy metal detection. Scaled down CMOS technology which tends to operate at lower current may be useful for detecting low concentration of heavy metals. Down-scaling trend of CMOS technology has significantly improved the performance of digital system. However, the decreasing supply voltage imposes challenges to analog design. In addition, the requirement for analog-digital integration required by study fully on-chip electrochemical sensor system demands for feasibility of adopting smaller node CMOS technology.



1.4 Research Objective

This research investigates the design and performance of CMOS potentiostat that can detect heavy metals at low concentration using 130nm CMOS technology with low supply voltages of $\pm 1.2V$. The CMOS potentiostat is aimed to support voltage range from -1V to +1V in order to detect different types of heavy metals. It is also aimed to sense current in nA range for low concentration detection. Therefore, the CMOS potentiostat is aimed to detect Cu(II) and Cd(II).

1.5 Research Scope

The research focuses on the design and simulation phases of $0.13\mu m$ CMOS technology. The design has been verified through post-layout simulation and is ready for next step which is chip fabrication. Therefore, chip fabrication and experimental measurement are excluded for scope of this thesis.

1.6 Thesis Organization

Chapter 1 specified the research area explains the motivation of this research. Next, the problem statement and also research objective are introduced prior to our brief explanation of the whole system. In chapter 2, the literature review which helps to understand the rated aspect of the thesis is explained. It includes the overview of electrochemistry. Then, the electrochemical analysis techniques are presented. In this chapter the potentiostat is introduced. Potentiostat topologies and their performance are also presented. In chapter 3, the methodology of this research is presented. In this chapter, design procedure, simulation setup and physical layout of this research is explained. The simulation result is discussed in chapter 4. Chapter 5 presents the conclusion of this work.

REFERENCES

- [1] M. M. Ahmadi and G. A. Jullien, "A wireless-implantable microsystem for continuous blood glucose monitoring," *IEEE Transactions on Biomedical Circuits and Systems*, vol. 3, pp. 169-180, 2009.
- [2] A. Islam, M. Haider, A. Atla, S. Islam, R. Croce, S. Vaddiraju, F. Papadimitrakopoulos, and F. Jain, "A potentiostat circuit for multiple implantable electrochemical sensors," in *International Conference on Electrical and Computer Engineering (ICECE)*, , 2010, pp. 314-317.
- [3] W. Arden, M. Brillouët, P. Cogez, M. Graef, B. Huizing, and R. Mahnkopf, ""More-than-Moore" "*International Technical Roadmap for Semiconductors*, 2010.
- [4] I. R. Committee, "International Technology Roadmap for Semiconductors, 2011 Edition," Semiconductor Industry Association, <u>http://www</u>. itrs. net/Links/2011ITRS/2011Chapters/2011ExecSum. pdf, 2011.
- [5] K. Christidis, P. Robertson, K. Gow, and P. Pollard, "Voltammetric in situ measurements of heavy metals in soil using a portable electrochemical instrument," *Measurement*, vol. 40, pp. 960-967, 2007.
- [6] B. Baś, M. Jakubowska, F. Ciepiela, and W. W. Kubiak, "New multipurpose electrochemical analyzer for scientific and routine tasks," *Instrumentation Science and Technology*, vol. 38, pp. 421-435, 2010.
- [7] A. Baysal, N. Ozbek, and S. Akman, "Determination of Trace Metals in Waste Water and Their Removal Processes," 2013.
- [8] V. Mudgal, N. Madaan, A. Mudgal, R. Singh, and S. Mishra, "Effect of toxic metals on human health," *The Open Nutraceuticals Journal*, vol. 3, pp. 94-99, 2010.
- [9] N. Madaan, V. Mudgal, S. Mishra, A. Srivastava, and R. Singh, "Studies on biochemical role of accumulation of heavy metals in Safflower," *Open Nutraceuticals J*, vol. 4, pp. 199-204, 2011.
- [10] L. Järup, "Hazards of heavy metal contamination," *British medical bulletin*, vol. 68, pp. 167-182, 2003.
- [11] P. Zhuang, M. B. McBride, H. Xia, N. Li, and Z. Li, "Health risk from heavy metals via consumption of food crops in the vicinity of Dabaoshan mine, South China," *Science of the Total Environment*, vol. 407, pp. 1551-1561, 2009.
- [12] Anodic Stripping Voltammetry-ASA Analytics, http://www.asaanalytics.com
- [13] A. Zeng, E. Liu, S. Tan, S. Zhang, and J. Gao, "Stripping voltammetric analysis of heavy metals at nitrogen doped diamond-like carbon film electrodes," *Electroanalysis*, vol. 14, pp. 1294-1298, 2002.
- [14] G. H. Hwang, W. K. Han, J. S. Park, and S. G. Kang, "Determination of trace metals by anodic stripping voltammetry using a bismuth-modified carbon nanotube electrode," *Talanta*, vol. 76, pp. 301-308, 2008.
- [15] K.-S. Yun, J. Gil, J. Kim, H.-J. Kim, K.-H. Kim, D. Park, J. Y. Kwak, H. Shin, K. Lee, and J. Kwak, "A miniaturized low-power wireless remote environmental monitoring system using microfabricated electrochemical sensing electrodes," in *Actuators and Microsystems, 12th International Conference on transducers, Solid-State Sensors,*, 2003, pp. 1867-1870.
- [16] C.-C. Liu, "Electrochemical sensors," *The Biomedical Engineering Handbook:*, 2000.

- [17] J. Janata, *Principles of chemical sensors*: Springer, 2009.
- [18] S. M. Martin, F. H. Gebara, T. D. Strong, and R. B. Brown, "A low-voltage, chemical sensor interface for systems-on-chip: the fully-differential potentiostat," in *International Symposium on Circuits and Systems*, 2004. *ISCAS'04.*, 2004, pp. IV-892-5 Vol. 4.
- [19] M. M. Ahmadi and G. A. Jullien, "A very low power CMOS potentiostat for bioimplantable applications," in *Proceeding fifth International Workshop on System-on-Chip for Real-Time Applications* 2005, pp. 184-189.
- [20] A. J. Bard and L. R. Faulkner, "Fundamentals and applications," *Electrochemical Methods*, vol. 2, 1980.
- [21] S. P. Kounaves, "Voltammetric techniques," *Handbook of instrumental techniques for analytical chemistry*, pp. 709-726, 1997.
- [22] A. W. Bott, "Voltammetric determination of trace concentrations of metals in the environment," *Current Separations*, vol. 14, pp. 24-30, 1995.
- [23] K. T. Kawagoe, J. B. Zimmerman, and R. M. Wightman, "Principles of voltammetry and microelectrode surface states," *Journal of neuroscience methods*, vol. 48, pp. 225-240, 1993.
- [24] C. M. Brett and A. M. O. Brett, *Electrochemistry: principles, methods, and applications* vol. 4: Oxford university press Oxford, 1993.
- [25] Q. Li, "Miniaturized Electrochemical Immunosensors for the Detection of Growth Hormone," 2012.
- [26] J. Barón-Jaimez, M. Joya, and J. Barba-Ortega, "Anodic stripping voltammetry–ASV for determination of heavy metals," in *Conference Series Journal of Physics*, 2013, p. 012023.
- [27] H. Zhuang, C. Wang, N. Huang, and X. Jiang, "Cubic SiC for trace heavy metal ion analysis," *Electrochemistry Communications*, vol. 41, pp. 5-7, 2014.
- [28] E. P. Achterberg and C. Braungardt, "Stripping voltammetry for the determination of trace metal speciation and in-situ measurements of trace metal distributions in marine waters," *Analytica chimica acta*, vol. 400, pp. 381-397, 1999.
- [29] K. C. Armstrong, C. E. Tatum, R. N. Dansby-Sparks, J. Q. Chambers, and Z.-L. Xue, "Individual and simultaneous determination of lead, cadmium, and zinc by anodic stripping voltammetry at a bismuth bulk electrode," *Talanta*, vol. 82, pp. 675-680, 2010.
- [30] A. H. Alghamdi, "Applications of stripping voltammetric techniques in food analysis," *Arabian Journal of Chemistry*, vol. 3, pp. 1-7, 2010.
- [31] D. Sparks, A. Page, P. Helmke, and R. Loeppert, "Differential Pulse Voltammetry," 1996.
- [32] X. He, Z. Su, Q. Xie, C. Chen, Y. Fu, L. Chen, Y. Liu, M. Ma, L. Deng, and D. Qin, "Differential pulse anodic stripping voltammetric determination of Cd and Pb at a bismuth glassy carbon electrode modified with Nafion, poly (2, 5-dimercapto-1, 3, 4-thiadiazole) and multiwalled carbon nanotubes," *Microchimica Acta*, vol. 173, pp. 95-102, 2011.
- [33] T. A. Silveira, D. F. D. Araujo, L. C. Marchini, A. C. Moreti, and R. A. Olinda, "Detection of metals by differential pulse anodic stripping voltammetry (DPASV) in pollen collected from a fragment of the atlantic forest in Piracicaba/SP," *Ecotoxicology and Environmental Contamination*, vol. 8, pp. 31-36, 2013.

- [34] P. R. Prasad, C. N. Reddy, and N. Y. Sreedhar, "Differential pulse anodic stripping voltammetric determination of Ni (II) and Co (II) in water and vegetable samples using analytical reagent 2, 2'-{benzene-1, 2-diylbis (nitrilomethylylidene]} diphenol," 2011.
- [35] Y. Bonfil, M. Brand, and E. Kirowa-Eisner, "Trace determination of mercury by anodic stripping voltammetry at the rotating gold electrode," *Analytica Chimica Acta*, vol. 424, pp. 65-76, 2000.
- [36] S. Hwang, "CMOS VLSI Potentiostat for Portable Environmental Sensing Applications," *IEEE SENSORS*, April 2010.
- [37] C.-Y. Huang, Y.-C. Wang, H.-C. Chen, and K.-C. Ho, "Design of a portable potentiostat for electrochemical sensors," in *Intelligent Sensors, Sensor Networks and Information Processing Conference, 2004.*, 2004, pp. 331-336.
- [38] M. M. Ahmadi and G. A. Jullien, "Current-mirror-based potentiostats for three-electrode amperometric electrochemical sensors," *IEEE Transactions* on Circuits and Systems I: Regular Papers, vol. 56, pp. 1339-1348, 2009.
- [39] W.-S. Wang, W.-T. Kuo, H.-Y. Huang, and C.-H. Luo, "Wide Dynamic Range CMOS Potentiostat for Amperometric Chemical Sensor," *Sensors*, vol. 10, pp. 1782-1797, 2010.
- [40] L. Busoni, M. Carla, and L. Lanzi, "A comparison between potentiostatic circuits with grounded work or auxiliary electrode," *Review of scientific instruments*, vol. 73, pp. 1921-1923, 2002.
- [41] J. P. Villagrasa, J. Colomer-Farrarons, and P. L. Miribel, "Bioelectronics for Amperometric Biosensors," 2013.
- [42] R. Greef, "Instruments for use in electrode process research,"J. Phys. E, Sci. Instrum., vol. 11, no. 1, pp. 1–12, Jan. 1978.
- [43] R. Doelling, *Potentiostats*. inBank Elektronik Application Note, 2nd. Clausthal-Zellerfeld, Germany, 2000.
- [44] M. R. Haider, S. K. Islam, S. Mostafa, M. Zhang, and T. Oh, "Low-power low-voltage current readout circuit for inductively powered implant system," *IEEE Transactions on Biomedical Circuits and Systems*, vol. 4, pp. 205-213, 2010.
- [45] M. Huque, M. Haider, M. Zhang, T. Oh, and S. K. Islam, "A Low Power, Low Voltage Current Read-Out Circuit for Implantable Electro-Chemical Sensors," *IEEE* in *Sensors*, 2007, pp. 64-67.
- [46] S. M. Martin, F. H. Gebara, T. D. Strong, and R. B. Brown, "A fully differential potentiostat," *Sensors Journal, IEEE*, vol. 9, pp. 135-142, 2009.
- [47] D. Zhao, X. Guo, T. Wang, N. Alvarez, V. N. Shanov, and W. R. Heineman, "Simultaneous Detection of Heavy Metals by Anodic Stripping Voltammetry Using Carbon Nanotube Thread," *Electroanalysis*, vol. 26, pp. 488-496, 2014.
- [48] L. E. Han, V. B. Perez, M. L. Cayanes, and M. G. Salaber, "CMOS Transistor Layout KungFu," *Lee Eng Han*, 2005.
- [49] R. F. Turner, D. Harrison, and H. P. Baltes, "A CMOS potentiostat for amperometric chemical sensors," *Solid-State Circuits, IEEE Journal of,* vol. 22, pp. 473-478, 1987.
- [50] M. Y. Ng and Y. Yusoff, "Variable gain CMOS potentiostat for dissolved oxygen sensor," in *Symposium on Quality Electronic Design (ASQED)*, , 2010, pp. 80-83.

- [51] G. Raikos and S. Vlassis, "0.8 V bulk-driven operational amplifier," *Analog integrated circuits and signal processing*, vol. 63, pp. 425-432, 2010.
- [52] F. Castaño, G. Torelli, R. Perez-Aloe, and J. M. Carrillo, "Low-voltage railto-rail bulk-driven CMFB network with improved gain and bandwidth," in *IEEE International Conference on Electronics, Circuits, and Systems* (*ICECS*), 2010 17th 2010, pp. 207-210.
- [53] R. L. Beal, "A low voltage rail-to-rail operational amplifier with constant operation and improved process robustness," 2009.
- [54] B. Song, O. Kwon, I. Chang, H. Song, and K. Kwack, "A 1.8 V self-biased complementary folded cascode amplifier," in *The First IEEE Asia Pacific Conference on ASICs, 1999. AP-ASIC'99.*, 1999, pp. 63-65.
- [55] M. Razzaghpour, S. Rodriguez, E. Alarcon, and A. Rusu, "A highly-accurate low-power CMOS potentiostat for implantable biosensors," in *Biomedical Circuits and Systems Conference (BioCAS)*, 2011, pp. 5-8.
- [56] R. J. Baker, *CMOS: circuit design, layout, and simulation* vol. 18: John Wiley & Sons, 2011.
- [57] S. M. Martin, T. D. Strong, and R. B. Brown, "Design, implementation, and verification of a CMOS-integrated chemical sensor system," in *International Conference on MEMS, NANO and Smart Systems, 2004. ICMENS 2004.* 2004, pp. 379-385.
- [58] D. Harvey, *Electrochemical Methods*, *In Modern analytical chemistry*: McGraw-Hill New York, 2000.
- [59] X. Wang, L. Yu, and L. Wang, "A Compact High-Accuracy Rail-to-Rail CMOS Operational Amplifier," in *International Conference on Bioinformatics and Biomedical Engineering (iCBBE)*, 2010, pp. 1-4.
- [60] T. W. Fischer, A. I. Karsilayan, and E. Sanchez-Sinencio, "A rail-to-rail amplifier input stage with±0.35% g m fluctuation," *IEEE Transactions Circuits and Systems I: Regular Papers.*, vol. 52, pp. 271-282, 2005.
- [61] A. J. Bard and L. R. Faulkner, *Electrochemical methods: fundamentals and applications* vol. 2: Wiley New York, 1980
- [62] J. Wang, Analytical electrochemistry: John Wiley & Sons, 2006.
- [63] N. H. Rahman, "Voltammetric studies of lead (ll), cadmium (ll), copper (ll) and chromium (lll) ions in the presence of selected n-heterocyclic compound," Universiti Putra Malaysia, 2011.
- [64] H. Shahbaazi, A. Safavi, and N. Maleki, "Determination of sub-parts per billion levels of copper in complex matrices by adsorptive string voltammetry on a mercury electrode" Malaysian Journal of Analytical Sciences, vol. 12, pp. 384-396, 2008.
- [65] A. B. Nepomnyashchii, M. A. Alpuche-Aviles, S. Pan, D. Zhan, F.-R. F. Fan, and A. J. Bard, "Cyclic voltammetry studies of Cd 2+ and Zn 2+ complexation with hydroxyl-terminated polyamidoamine generation 2 dendrimer at a mercury microelectrode," Journal of Electroanalytical Chemistry, vol. 621, pp. 286-296, 2008.
- [66] X. Li and A. R. Barron, "Introduction to Cyclic Voltammetry Measurements." https://cnx.org/contents/m34669/1.1/
- [67] E. Rajni, "Design of High Gain Folded-Cascode Operational Amplifier Using 1.25 um CMOS Technology," *International Journal of Scientific & Engineering Research*, vol. 2, 2011.