

# **UNIVERSITI PUTRA MALAYSIA**

# SYNTHESIS AND CHARACTERIZATION OF POLYHYDROXYETHYL-ACRYLATE AND POLYHYDROXYETHYLMETHACRYLATE GEL DOSIMETERS

# KHALID AHMED MAJALI RABA'EH

FS 2007 40



#### SYNTHESIS AND CHARACTERIZATION OF POLYHYDROXYETHYL-ACRYLATE AND POLYHYDROXYETHYLMETHACRYLATE GEL DOSIMETERS

By

#### KHALID AHMED MAJALI RABA'EH

Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia, in Fulfilment of the Requirements for the Degree of Doctor of Philosophy

October 2007



In the Name of Allâh, the Most Gracious, the Most Merciful

ان الله يمسك السماوات والارض ان تزولا ولئن زالتا ان امسكهما من احد من بعده انه كان حليما غفورا

Surely Allah upholds the heavens and the earth lest they come to naught; and if they should come to naught, there is none who can uphold them after Him; surely He is the Forbearing, the Forgiving.

Al-Quran, 35:41



# DEDICATION

# To the Memory of my Lovely Son Malik



Abstract of the thesis presented to the Senate of Universiti Putra Malaysia in fulfilment of requirement for the degree of Doctor of Philosophy

#### SYNTHESIS AND CHARACTERIZATION OF POLYHYDROXYETHYL-ACRYLATE AND POLYHYDROXYETHYLMETHACRYLATE GEL DOSIMETERS

By

#### KHALID AHMED MAJALI RABA'EH

October 2007

Chairman: Professor Elias Saion, PhD

Faculty: Science

Polymer gel dosimeters in conjunction with the nuclear magnetic resonance imaging (MRI) are potentially used for verification of complex dose distributions in three dimensions (*3D*) for radiotherapy treatment planning. The radiation-induced polymerization of hydroxyethylacrylate (HEA) and hydroxyethylmethacrylate (HEMA) polymer gel dosimeters has been studied using Raman spectroscopy, nuclear magnetic resonance (NMR) and MRI scanner. The HEA polymer gels were synthesized from 2-hydroxyethylacrylate (HEA) monomer (2 to 5% w/w), *N*,*N*<sup>-</sup> methylene-bis-acrylamide (BIS) cross-linker (2 to 5% w/w), gelatin (3 and 5%) and de-ionized water in oxygen free environment. The HEMA polymer gels were synthesized from 2-hydroxyethylmethacrylate (HEMA) monomer (2 to 5% w/w), BIS (2 to 5% w/w), 5% gelatin and de-ionized water. The dosimeters were irradiated with <sup>60</sup>Co teletherapy  $\gamma$ -ray source at a constant dose rate of 0.43 Gy/min, receiving



doses up to 20 Gy for a single point dose measurement and up to 30 Gy for 3D dose distributions scanning.

Raman spectroscopy was used to investigate directly the degree of radiation-induced polymerization and the rate of elapsed polymerization, targeting the COO stretching Raman shift at vibrational band of 1415 cm<sup>-1</sup> assigned for HEA polymer gels and the OH stretching Raman shift at vibrational band of 3358 cm<sup>-1</sup> assigned for HEMA polymer gels. The Raman intensity *y* corresponding to the amount of polymerization in both HEA and HEMA polymer gels increases with absorbed dose *D* in the dose range between 0 and 20 Gy and follows mono-exponential equation given as  $y = y_0 + A(1 - e^{-D/D_0})$ . The rate of elapsed polymerization in HEA and HEMA polymer gels decreases with absorbed dose in the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows for the dose range between 0 and 20 Gy and follows exponential equation given as  $\frac{dy}{dt} = \frac{A\kappa}{D_0} e^{-D/D_0}$ . The dose sensitivity,  $D_0$ 

of polymerization and the half dose,  $D_{1/2}$  of the rate of elapsed polymerization in HEA and HEMA polymer gels increase strongly with increasing the cross-linker concentration than that of the monomer concentration where the dose correlation factor for the cross-linker is always greater than the dose correlation factor for the monomer. At 3% gelatin the  $D_0$  and  $D_{1/2}$  values of the HEA polymer gels always greater than at 5% gelatin, indicating that the polymerization and the rate of elapsed polymerization of HEA polymer gels increases with decreasing the amount of gelatin. The consumption of co-monomer in HEA and HEMA polymer gels decreases mono-exponentially with absorbed dose in the dose ranges between 0 and 20 Gy and it follows mono-exponential equation of the form  $y = y_0 - A(1 - e^{-D/D_0})$ .



The result shows that the cross-linker consumption increases more significantly with absorbed dose than the monomer consumption.

The nuclear magnetic resonance (NMR) spin–spin relaxation rate,  $R_2$  for water proton surrounding the polymer formation has been used to investigate indirectly the degree of polymerization and the rate of elapsed polymerization of HEA and HEMA polymer gels. The dose response of the change in relaxation rate,  $\Delta R_2$  is also monoexponential function and for the rate of elapsed polymerization it is normal exponential function. The dose sensitivity,  $D_0$  for the change in relaxation rate  $\Delta R_2$ and the half dose,  $D_{1/2}$  for the rate of elapsed polymerization of HEA and HEMA polymer gels have produced results of similar trend to that of Raman spectroscopy method.

The radiological film obtained from the clinical MRI scans of polymer gel phantom to simulate radiotherapy treatment planning was analyzed using a densitometer. The optical density of the polymer gels was found to increase with the increase of absorbed dose and decreases with the increase of depth inside the phantom. The dose-depth map for HEA polymer gels was derived for different concentrations of HEA and BIS co-monomers. The results suggest that for a clinical radiotherapy treatment planning the dose correction for tumour deep within the body should be implemented with knowledge of the amount of applied dose, tumour volume, skin to tumour distance, and tissue equivalent nature of the body. The percentage of depth dose was also evaluated which leads to a good agreement with the ionization chamber measurements.



The indirect measurements of HEA and HEMA polymer gels using NMR have shown more dose sensitivity than that for direct measurements using Raman spectroscopy. In general the dose sensitivity and half dose of HEA polymer gels are grater than that for HEMA, indicating that the HEA polymer gels are more radiosensitive than that of HEMA polymer gels at a given dose. The dose-depth map has been achieved using HEA polymer gels in conjunction with MRI scanning which led to introduce a fit equation between dose and depth inside HEA polymer gels.



Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Doktor Falsafah

#### SINTESIS DAN PENCIRIAN POLIHYDROXYETHYLACRYLATE DAN POLIHYDROXYETHYLMETHACRYLATE DOSIMETER GEL

By

#### KHALID AHMED MAJALI RABA'EH

Oktober 2007

Pengerusi: Profesor Elias Saion, PhD

Fakulti: Sains

Dosimeter polimer gel dan imej resonan magnet nuclear (MRI) mampu digunakan untuk menentusahkan taburan dos komplek tiga dimensi (3D) untuk kegunaan pelan rawatan radioterapi. Pempolimaran induksi sinaran bagi dosimeter polymer gel hydroxyethylacrylate (HEA) and hydroxyethylmethacrylate (HEMA) telah dikaji dengan menggunakan Raman spectroskopi, resonan magnet nuklear (NMR) dan monomer imbas MRI. Polymer HEA disentisis menggunakan gel 2hydroxyethylacrylate (HEA) (2% hingga 5% w/w), petautsilang  $N_{,N}$ -methylene-bisacrylamide (BIS) (2% hingga 5% w/w), gelatin (3% dan 5%) dan air tak berion dalam keadaan bebas oksigen. Manakala polimer gel HEMA disentisis dengan menggunakan monomer 2-hydroxyethylmethacrylate (HEMA) (2 hingga 5% w/w), BIS (2% hingga 5% w/w), 5% gelatin dan air tak berion. Semua dosimeter didedahkan kepada sinar gama daripada sumber <sup>60</sup>Co teletherapy pada kadar dos 0.43



Gy/min dan menerima dos hingga kepada 20 Gy bagi pengukuran dos titik tunggal dan hingga kepada 30 Gy bagi pengukuran imbasan taburan dos 3*D*.

Darjah pempolimeran induksi sinaran dan kadar pempolimeran lepasan telah dikaji secara terus menggunakan spectroskopi Raman dengan mensasarkan kepada anjakan Raman rengangan COO pada jalur getaran 1415 cm<sup>-1</sup> yang ditujukan kepada polimer gel HEA dan anjakan Raman rengangan OH pada jalur getaran 3358 cm<sup>-1</sup> yang ditujukan kepada polimer gel HEMA. Keamatan Raman y sepadan dengan amaun polimeran bagi kedua HEA and HEMA bertambah dengan dos terserap D dalam julat dos di antara 0 dan 20 Gy dan memenuhi persamaan mono-eksponen dinyatakan sebagai  $y = y_0 + A(1 - e^{-D/D_0})$ . Kadar polimeran lepasan HEA dan HEMA berkurang dengan dos terserap dalam julat dos di antara 0 dan 20 Gy dan memenuhi persamaan eksponen diberi sebagai  $\frac{dy}{dt} = \frac{A\kappa}{D_0} e^{-D/D_0}$ . Kepekaan dos,  $D_0$  untuk proses polimeran dan dos separuh,  $D_{1/2}$  untuk kadar polimeran lepasan bagi gel HEA and HEMA bertambah dengan banyaknya dengan pertambahan kepekatan petautsilang melebihi yang diperolehi daripada kepekatan monomer dimana factor korelasi dos petautsilang lebih tinggi daripada factor korelasi dos monomer. Nilai  $D_0$  dan  $D_{1/2}$  adalah lebih

tinggi bagi polimer gel HEA dengan 3% gelatin berbanding dengan 5% gelatin, menunjukkan pempolimeran dan kadar pempolimeran lepasan polymer gel HEA bertambah dengan pengurangan kepekatan gelatin. Penggunaan ko-monomer dalam polymer gel HEA and HEMA berkurangan secara mono-eksponen dengan dos terserap dalam julat dos di antara 0 dan 20 Gy dan memenuhi persamaan absorbed dose in the dose ranges between dalam bentuk  $y = y_0 - A(1 - e^{-D/D_0})$ . Keputusan



menunjukkan bahawa penggunaan petautsilang adalah lebih tinggi berbanding penggunaan monomer.

Kadar santaian spin-spin resonans magnet nuclear,  $R_2$  untuk air di sekeliling pembentukan polimer telah digunakan untuk menyelidiki secara tak terus menggunakan darjah pempolimeran dan kadar pempolimeran lepasan bagi polimer gel HEA and HEMA. Sambutan dos terhadap perubahan kadar santaian,  $\Delta R_2$  adalah juga fungsi mono-eksponen dan kadar pempolimeran lepasan adalah juga fungsi eksponen. Keputusan mengenai kepekan dos,  $D_0$  untuk perubahan kadar santaian  $\Delta R_2$ dan dos separoh,  $D_{1/2}$  untuk kadar pempolimeran lepasan polimer gel HEA dan HEMA mempunyai haluan yang sama dengan kaedah spektroskopi Raman.

Sebuah pengimbas kilinik MRI telah digunakan bagi mendapatkan film radiology fentom polimer gel untuk simulasi plan rawatan radioterapi yang dianalisis dengan menggunakan sebuah densitometer. Ketumpatan optik polimer gel didapati bertambah dengan dos terserap dan berkurangan dengan pertambahan kedalaman fentom. Peta hubungan dos-kedalaman bagi polimer gel HEA telah dihasilkan untuk kepekatan ko-monomer HEA dan BIS yang berbeza. Keputusan menunjukkan bahawa untuk plan rawatan radiotrepi pembetulan dos tumour dalam badan perlu dilakukan dengan mengetahui amaun dos dikenakan, isipadu tumour, jarak diantara kulit dan tumour dan kesetaraan tisu badan. Peratus dos kedalaman telah ditentusahkan dan didapati bersetuju dengan pengukuran dengan menggunakan kebok pengion.



Pengukuran secara tak langsung gel polimer HEA dan HEMA menggunakan NMR telah menunjukkan dos kepekaan yang lebih berbanding pengukuran secara langsung menggunakan spektroskopi Raman. Secara amnya, dos kepekaan dan dos separa untuk gel polimer HEA adalah lebih tinggi daripada HEMA, menunjukkan bahawa gel polimer HEA lebih radiosensitif berbanding gel polimer HEMA pada dos yang tertentu. Peta kedalaman dos telah diperolehi dengan mengunakan gel polimer HEA bersama dengan imbasan MRI yang menjurus kepada pengenalan persamaan padanan di antara dose dan kedalaman di dalam gel polimer HEA.



#### ACKNOWLEDGEMENTS

I would like to express my utmost gratitude to Prof. Dr. Elias Saion, Chairman of the Supervisory Committee who has been very helpful in providing me intellectual guidance, as well as to the other members of the Committee, namely Associate Prof. Zainal Abidin B Sulaiman, Associate Prof. Zaki Abd Rahman and Dr. Nooriah Mod Ali who are sincerely helped me throughout my studies.

Also I would like to show my kind appreciation to my friends and lab-mates Mr. Mohammad A., Iskander S., Azhar A. and Yousof M. Also sincere thanks and acknowledge to Mr. Mohammad Zain and Mr. Ruslim for their assistance and encouragement.

Thanks are expressed to Nuclear Energy Agency Malaysia-Bangi (NEAM) for allowing me to irradiate my research samples. I extend my words to the SDDL staff, namely Mr. Taiman Kadni and Mrs. Noorhayati.

I would like to express my words of thanks to Biomedical Imaging, Universiti Malaya Medical Centre for allowing me to get MRI scanning for my sample.

I should thank my mother for my upbringing and for the support of my receiving high education and also I would like to thank my wife and my son Mohammad for their patience, encouragement and understanding



I certify that an Examination Committee met on 3<sup>rd</sup> October to conduct the final examination of Khalid Ahmed Majali Raba'eh on his Doctor of Philosophy thesis entitled "Synthesis and Characterization of Polyhydroxyethylacrylate and Polyhydroxyethylmethacrylate Gel Dosimeters" in accordance with Universiti Pertanian Malaysia (Higher Degree) Act 1980 and Universiti Pertanian Malaysia (Higher Degree) Regulations 1981. The Committee recommends that the student be awarded the degree of Doctor of Philosophy.

Members of the Examination Committee were as follows:

#### Zaidan Abd. Wahab, PhD

Associate Professor Faculty of Science Universiti Putra Malaysia (Chairman)

#### Wan Md.Zin Wan Yunus, PhD

Professor Faculty of Science Universiti Putra Malaysia (Internal Examiner)

#### W. Mahmood Mat Yunus, PhD

Professor Faculty of Science Universiti Putra Malaysia (Internal Examiner)

#### Abd. Aziz Tajuddin, PhD

Professor Faculty of Science Universiti Sain Malaysia (External Examiner)

HASSANA MOHD. GHAZALI, Ph D

Professor / Deputy Dean School of Graduate Studies Universiti Putra Malaysia

Date: 22 November 2007



This thesis was submitted to the Senate of Universiti Putra Malaysia and has been accepted as fulfillment of the requirement for the degree of Doctor of Philosophy. The members of the Supervisory Committee were as follows:

#### Elias Saion, PhD

Professor Faculty of Science Universiti Putra Malaysia (Chairman)

#### Zainal Abidin Sulaiman, PhD

Associate Professor Faculty of Science Universiti Putra Malaysia (Member)

#### Mohamad Zaki Abd Rahman, PhD

Associate Professor Faculty of Science Universiti Putra Malaysia (Member)

#### Nooriah Mod Ali, PhD

Doctor Nuclear Energy Agency Malaysia-Bangi (NEAM) (Member)

#### AINI IDERIS, PhD

Professor and Dean School of Graduate Studies Universiti Putra Malaysia

Date: 13 December 2007



#### DECLARATION

I declare that the thesis is my original work except for quotations and citations which have been duly acknowledged. I also declare that it has not been previously, and is not concurrently, submitted for any other degree at universiti Putra Malaysia or at any other institution.

#### KHALID AHMED MAJALI RABA'EH

Date: 2007



# TABLE OF CONTENTS

# Page

DEDICATION	iii
ABSTRACT	iv
ABSTRAK	viii
ACKNOWLEDGEMENTS	xii
APPROVAL	xiii
DECLARATION	XV
LIST OF TABLES	xxi
LIST OF FIGURES	xxii
LIST OF ABBREVIATIONS	xxxii

#### CHAPTER

#### **INTRODUCTION**

1.1	Radiotherapy treatment planning	1
1.2	Polymer gel dosimeters	2
1.3	Statement of the problem	4
1.4	Significant of the study	5
1.5	Objectives of the study	6
1.6	Outline of the thesis	7

### 2 LITERATURE REVIEW

2.1	Background of Polymer gel dosimeter.			
	2.1.1 Fricke gel dosimeters.	8		
	2.1.2 Polymer gel dosimeters	9		
	2.1.3 Polymerization of polymer gels.	11		
2.2	Synthesis of polymer gel dosimeter.	14		
2.3	Irradiation of polymer gels.	15		
2.4	Characterization of polymer gel dosimeters.	16		
	2.4.1 Raman spectroscopy.	16		
	2.4.2 NMR measurements of polymer gels	25		
	2.4.3 MR imaging of polymer gels	38		
	2.4.4 CT imaging of polymer gels	47		
	2.4.5 Spectrophotometer measurements of polymer			
	gels	50		
2.5	Application of polymer gels	51		
	2.5.1 Intensity-Modulated Radiation Therapy (IMRT)	52		
	2.5.2 Brachytherapy	52		
	2.5.3 Stereotactic Radiosurgery and Radiotherapy	53		
	2.5.4 Carbon ion radiotherapy	54		
	2.5.5 Boron neutron capture therapy	55		



# THEORETICAL STUDIES

3.1	Type of Ionizing Radiation.	56
	3.1.1 Direct ionization	56
	3.1.2 Indirect ionization	57
32	Physical Principle of Radiation Action	58
5.2	3 2 1 Photoelectric effect	50 59
	3.2.1 Compton scattering	60
	3.2.2 Pair production	61
33	Absorption Coefficient	63
3.4	Absorbed dose	65
3.5	Radiation Effects	66
5.5	3.5.1 Jons and excited molecules	66
	3.5.2 Radiolysis	68
	3.5.3 Recombination	68
	3.5.4 Polymerization	60 69
	3.5.5 Cross-linking	69
	3.5.6 Chain Seission	70
	3.5.7 Role of radical scavengers and oxygen	70
36	Raman Spectroscony	71
5.0	3.6.1 Vibrations of molecules	73
	3.6.2 Interaction of radiation with vibration atom in a	15
	molecule	75
	3 6 3 Raman Effect	75 77
	3.6.4 Intensity of Raman line	82
37	Nuclear Magnetic Resonance (NMR)	82
5.7	3.7.1 Magnetization procession	87
	3.7.2 Relavation time	89
	3.7.2 Magnetic Resonance Imaging (MRI)	93
38	Ontical density	96
5.0	Optical density.	20
MA	FERIALS AND METHOD	
4.1	Sample preparation.	97
	4.1.1 Synthesis of hydroxyethylacrylate (HEA) gel	
	dosimeters.	97
	4.1.2 Synthesis of hydroxyethylmethacrylate	
	(HEMA) gel dosimeters.	100
4.2	Irradiation of Polymer gels.	101
4.3	Raman spectroscopy measurements.	103
4.4	Nuclear Magnetic Resonance (NMR) measurements.	106
4.5	Magnetic Resonance Imaging (MRI) scanning.	107
4.6	Densitometer.	110
RES	ULTS AND DISCUSSION	
5.1	Michanisim of Polymerization process in HEA gels	113
5.2	Direct characterization of HEA gels using Raman	l
	scattering method	115
	5.2.1 Raman intensity spectra of HEA polymer gel	
	dosimeters	115
	5.2.2 Raman intensity at different BIS concentrations	i 
	and 5% gelatin	116



5.2	3 Dose sensitivity, $D_0$ versus BIS concentration at 5% gelatin	120			
5.2	Raman intensity at different BIS concentrations				
5 3	and 3% gelatin	121			
5.2.	at 3% gelatin $(D_0)$ versus BIS concentration	124			
5.2	6 Rate of elapsed polymerization at different BIS				
	concentration and 5% Gelatin	125			
5.2.	.7 Half dose, $D_{1/2}$ of rate of elapsed	120			
	polymerization versus BIS at 5% gelatin	129			
5.2.	.8 Rate of elapsed polymerization at different BIS concentration and 3% gelatin	131			
5.2	.9 Half dose, $D_{1/2}$ of rate of elapsed				
	polymerization versus BIS at 3% gelatin	133			
5.2	10 Raman intensity at different concentrations of				
	HEA monomer and 5% gelatin	134			
5.2	.11 Dose sensitivity, $D_0$ versus concentrations of				
	HEA monomer at 5% gelatin	137			
5.2.	.12 Raman intensity at different concentrations of				
5.0	HEA monomer and 3% gelatin	138			
5.2	13 Dose sensitivity, $D_0$ versus concentration of				
5 2	HEA monomer at 3% gelatin	141			
5.2.	14 Kate of elapsed polymerization at different	1 4 0			
5 2	15 Half dosa D of rate of alapsed	142			
5.2.	15 Hall dose, $D_{1/2}$ of fate of etapsed				
5 0	polymerization versus HEA at 5% gelatin	144			
3.2.	concentration of HEA and 3% gelatin	145			
52	17 Half dose D of rate of elansed	145			
5.2.	$D_{1/2}$ of fact of etapsed	1/18			
5 2	18 Consumption of gross linker (PIS) and	140			
3.2.	monomer (HEA)	149			
Dir	ect characterization of HEMA gels using Raman	117			
scat	ttering method	150			
5.3	.1 Raman intensity spectra of HEMA polymer gel				
	dosimeters.	150			
5.3	2 Change of Relative Raman Intensity at different				
	BIS concentrations and 5% Gelatin	151			
5.3	.3 Dose Sensitivity, $D_0$ versus BIS concentration				
	at 5% Gelatin	154			
5.3	4 Rate of elapsed polymerization versus BIS				
	concentration at 5% gelatin	155			
5.3.	.5 Half dose, $D_{1/2}$ of rate of elapsed				
	polymerization versus BIS concentration at 5%				
	gelatin	158			
5.3.	6 Change of relative Raman intensity versus				
E 0	concentration of HEMA monomer at 5% gelatin	159			
3.3	Dose Sensitivity, $D_0$ versus concentrations of UEMA monomer at 5% coloring	1.00			
	mental monomer at 5% geraun	162			



5.3

	5.3.8	Rate of elapsed polymerization versus concentration of HEMA at 5% gelatin.	163
	5.3.9	Half Dose, $D_{1/2}$ of rate of elapsed	
		polymerization versus concentration of HEMA	166
	5 2 10	monomer at 5% gelatin	100
	5.5.10	Monomer (HEMA)	1(7
54	Indired	$\Delta \alpha$ the characterization of HEA and dosimeter by	16/
Ј.т	NMR 1	method	168
	5.4.1	Change of $\Delta R_2$ versus BIS concentration at 5%	100
		gelatin	169
	5.4.2	Dose Sensitivity, $D_0$ versus BIS concentration	10)
		at 5% gelatin	172
	5.4.3	Change of $\Delta R_2$ versus BIS concentration at 3%	
		gelatin	173
	5.4.4	Dose Sensitivity, $D_0$ versus BIS concentration	
	- A -	at 3% gelatin	176
	5.4.5	Rate of elapsed polymerization versus BIS $\frac{1}{2}$	
	516	Unif dage D of rate of clarged	177
	5.4.6	Half dose, $D_{1/2}$ of rate of elapsed	
		polymerization versus BIS concentration at 5%	100
	5 A 7	gelatin.	180
	5.4.7	Rate of elapsed polymerization versus BIS	181
	518	Half dosa D of rate of alapsed	101
	5.4.0	That dose $D_{1/2}$ of face of elapsed	
		polymerization versus BIS concentration at 3%	184
	540	genuin. Change of $AP_{\rm e}$ versus concentration of $HEA$	
	5.4.9	monomer at $5\%$ gelatin	185
	5410	Dose sensitivity $D_0$ versus concentration of	
	2.1.10	HEA monomer at 5% gelatin.	188
	5.4.11	Change of $\Delta R_2$ versus concentration of HEA	100
		monomer at 3% gelatin.	189
	5.4.12	Dose sensitivity, $D_0$ versus concentration of	102
		HEA monomer at 3% gelatin.	192
	5.4.13	Rate of elapsed polymerization versus	193
		concentration of HEA monomer at 5% gelatin	175
	5.4.14	Half dose $D_{1/2}$ of rate of elapsed	
		polymerization versus HEA concentration at	
		5% Gelatin.	195
	5.4.15	Rate of elapsed polymerization versus	
		concentration of HEA monomer at 3% gelatin.	196
	5.4.16	Half dose $D_{1/2}$ of rate of elapsed	
		polymerization versus concentration of HEA	
	т 1 <sup>.</sup>	monomer at 3% gelatin	199
5.5	Indirec	ct Characterization of HEMA polymer gels by	200
	NMK	Change of AD years DIS concentration of 50/	200
	3.3.1	Change of $\Delta K_2$ versus BIS concentration at 5%	



			gelatin	200
		5.5.2	Dose sensitivity $D_0$ versus BIS concentration at 5% galatin	202
		553	Rate of elapsed polymerization versus BIS	203
		0.0.0	concentration at 5% gelatin.	204
		5.5.4	Half dose $D_{1/2}$ of rate of elapsed	
			polymerization versus BIS concentration at 5%	
			gelatin.	207
		5.5.5	Change of $\Delta R_2$ versus HEMA concentration at	200
			5% gelatin.	208
		5.5.6	Dose sensitivity $D_0$ versus concentration of	211
		<b>-</b> -	HEMA monomer at 5% gelatin.	211
		5.5.7	Rate of elapsed polymerization versus	212
		558	Half dose D of rate of elansed	
		5.5.0	That dose $D_{1/2}$ of fate of elapsed	
			polymerization versus concentration of HEMA	215
	56	Chara	cterization of HFA polymer gel dosimeters for	
	5.0	radiot	nerany.	016
		5.6.1	MRI scans at different beam doses and phantom	216
			depths.	016
		5.6.2	Optical density versus depth at different dose	216
			beams for given HEA polymer gel	222
		5.6.3	Optical density versus depth at different	
			polymer gel concentrations for given dose beam	225
		561	Source. Change in Optical Density versus Dese at	-
		5.0.4	Different Concentrations of co-monomer (BIS	
			and HEA)	228
		5.6.5	Change in an absorbed dose versus depth at	
			different concentrations of co-monomers	231
		5.6.6	Rate of elapsed Polymerization	233
		5.6.7	Crossed dose map	236
	5.7	Depth and io	dose measurements by polymer gel dosimeter	238
6	CON	CLUSI	ON AND FUTURE WORKS	
U	61	Conclu	ision	240
	6.2	Future	works	245
REFERE	NCES			246
APPEND	APPENDIX		255	
BIODAT	A OF TH	E AUTH	IOR	261
LIST OF	LIST OF PUBLICATIONS 26			262



# LIST OF TABLES

<b>Table</b> 2.1	Vibrational band assignments for acrylamide (AAm) bis-acrylamide (BIS) and polyacrylamide gel (PAG)	<b>Page</b> 16
2.2	Composition of the different gel batches	23
2.3	Dose constants $(D_0)$ obtained from FT-Raman spectroscopy	25
2.4	The parameters of the model of fast exchange of magnetization obtained for the different formulations of polymer gel dosimeters. All formulations contained 3% of the monomer indicated in addition to 3% of BIS. The concentrations of the gelling agent were 1% for agarose and 5% for gelatin	32
2.5	Composition and measurement results of the various polymer gel dosimeters used by percentage of the final weight. $r_2$ , standard error and <i>P</i> -value are taken from the regression program in Microsoft Excel	48
3.1	Common NMR active isotope	83
4.1	Various compositions of the different gels at a given BIS and 3% gelatin	98
4.2	Various compositions of the different gels at a given HEA and 3% gelatin	98
4.3	Various compositions of the different gels at a given BIS and 5% gelatin	98
4.4	Various compositions of the different gels at a given HEA and 5% gelatin	99
4.5	Various compositions of the different gels at a given BIS and 5% gelatin	99
4.6	Various compositions of the different gels at a given BIS and 5% gelatin	100
4.7	Various compositions of the different gels at a given HEA and 5% gelatin	101



# LIST OF FIGURES

Figure		Page
2.1	Chemical structures of some monomers used for polymer gel dosimeters.	11
2.2	Chemical structures of acrylamide (AAm) and $N,N'$ methyelene-BIS-acrylamide (BIS).	13
2.3	Chemical structure of polyacrylamide Gel (PAG)	14
2.4	FT-Raman spectra of polymerized PAG samples with absorbed radiation dose.	17
2.5	Variation of integrated peak areas of the acrylamide (1285 cm <sup><math>-1</math></sup> ) and bis-acrylamide (1256 cm <sup><math>-1</math></sup> ) vinyl $\delta$ CH2 vibrational bands with absorbed radiation dose.	18
2.6	Correlation of the vinyl CH bending mode of bis (1256 cm <sup><math>-1</math></sup> ) and acrylamide (1285 cm <sup><math>-1</math></sup> ): ( <i>a</i> ) lines between points as a visual aid only; ( <i>b</i> ) data fitted to exponential.	20
2.7	Polymer formation observed in FT-Raman spectra of irradiated PAG. 2936 cm <sup>-1</sup> CH2 stretching mode of polyacrylamide.	21
2.8	Integrated peak intensity of the 2936 cm <sup><math>-1</math></sup> CH2 stretch in polyacrylamide as a function of dose: ( <i>a</i> ) lines between points as a visual aid only, ( <i>b</i> ) data fitted to exponential.	22
2.9	FT-Raman spectra for one of the HEA gels. Spectra corresponding to each absorbed dose were obtained.	24
2.10	The consumption of BIS and HEA as a function of absorbed dose, measured using FT-Raman spectroscopy.	24
2.11	The dose dependence of the water-proton NMR transverse relaxation rate $R2$ , combining the data from three separately prepared PAG gels, over the range (a) 0-20 (b) 0 to 8Gy.	27
2.12	Effect of temperature on the $R_2$ -dose–response curve of PAG gel (After Maryanski et al 1997).	27
2.13	Dose–R2 plot obtained at various scanning temperatures for the PAG gel dosimeter (After De Deene et al., 2005).	28
2.14	The dependence of the dose sensitivity on the scanning temperature for the PAG gel dosimeter (After De Deene et al., 2005).	29



- 2.15  $R_2(1/T_2)$  changes as a function of the absorbed dose for different 30 polymer gel dosimeter formulations having gelatin as the gelling agent.
- 2.16  $R_2(1/T_2)$  changes as a function of the absorbed dose for different 30 polymer gel dosimeter formulations having agarose as the gelling agent.
- 2.17  $T_2$  at 64MHz as a function of dose for different initial co-monomer 32 concentrations (2, 3 and 4%) and fixed gelatin concentration (5%) (After Lepage et al, 2001b).
- 2.18  $T_2$  at 64 MHz as a function of the absorbed radiation dose for 33 different gelatin concentrations (3, 5 and 7%) and fixed monomer concentration (3% AA and 3% BIS). (After Lepage et al, 2001b).
- 2.19 Dependence of gel's sensitivity on its pH (After Murphy et al., 2000) 34
- 2.20 The influence of pH on the baseline  $R_2$  ( $R_2$  at 0 Gy) (After Murphy 35 et al., 2000).
- 2.21 Dose– $R_2$  plot as a function of post-irradiation time (After De Deene 36 *et al* 2000b).
- 2.22  $R_2$  as a function of time after manufacture for gelatin gels containing 37 various amounts of sodium azide. Graph (*a*) is for monomer/polymer gels containing 6% gelatin while (*b*) is for monomer/polymer gels containing 12% gelatin (After De Deene *et al* 2000b).
- 2.23 (b) Shows a T2-weighted spin-echo image (TE = 200 ms) of PAG 39 gel, and a photograph of it is shown in (a) (After Maryanski et al 1994).
- 2.24  $T_2$ -calculated map (axial section) of the phantom that contains test 40 objects and the first batch of VIPAR gels. The dose that each gel has absorbed is presented in figure next to the  $T_2$ -calculated map. As the absorbed dose is increased the gels appear darker ( $T_2$  is decreased).
- 2.25 Relaxation Rate  $(R_2)$  of VIPAR gels as a function of dose up to 11 40 Gy.
- 2.26  $T_2$ -maps (coronal slices along the beam paths) of the VIPAR gels 41 irradiated with (*a*) the 5 mm cone and (*b*) the 10 mm cone. The slice thickness was 10 mm.
- 2.27  $T_2$ -maps (axial slices) of the gels irradiated with (*a*) the 5 mm cone 42 and (*b*) the 10 mm cone. The centre of the slice in both gels was placed 5 cm from the tube apex (i.e. at the iso-centre during the irradiation process). The slice thickness was 10 mm



- 2.28 Relative depth dose data for the 5 mm cone ( $\diamondsuit$ ) and the 10 mm 43 cone ( $\blacklozenge$ ) derived using the VIPAR gel-MRI method. The 10 mm beam data are normalized to the maximum value (%). The dose at  $D_{\text{max}}$  for the 5 mm beam was found to be 0.64 times the dose at  $d_{\text{max}}$  for the 10 mm beam and, therefore, the 5 mm beam data are normalized to the value of 64%. Percentage depth doses for the 10 mm cone ( $\blacksquare$ ) and for a 10 × 10 cm<sup>2</sup> field (•), derived using the Pin-Point ion chamber, are also presented.
- 2.29 Relative iso-dose lines (20, 30, 50, 70, 80, 95%) resulting from the 44 analysis of the  $T_2$ -maps presented in Figure 28: (*a*) for the 5 mm cone and (*b*) for the 10 mm cone.
- 2.30 Central gel depth dose curves (circles) compared with Monte Carlo 45 calculations (full curve).
- 2.31 (b) Iso-dose contours obtained by treatment planning system (TPS) 46 (dotted line) and polymer gel-MRI (solid line) referring to (a) the central axial plane of the patient plan (After Sandilos et al., 2004).
- 2.32 Spin-echo image of a polymer gel plastic phantom irradiated with 47 two square x-ray beams to 15 Gy from the bottom and side of the image; TE = 300 ms, TR = 2000 ms
- 2.33 CT-dose response for gels with varying concentrations of 50 acrylamide (AA) plus *N*,*N*'-methelyne-bis-acrylamide with gelatin (a) and agarose (b), and varying gelatin concentration (c).
- 2.34 Variation of the extinction coefficient ( $\alpha$ ) reported vs. the absorbed 51 dose.
- 2.35 Imaging of a brachytherapy phantom. (After Deene et al., 2001b). 53
- 3.1 The decay scheme of  ${}^{60}$ Co isotope. 58
- 3.2 Schematic diagram of Compton scattering. 60
- 3.3 Schematic diagram of Pair Production process for γ-radiation being 63 interfered in the nucleus field and orbital electron to produce triplet particles.
- 3.4 The total mass absorption coefficient of photon of energies 65 below 100 MeV in iodine.
- 3.5 The process of permanent main-chain scission of poly- 71 isobutylene.
- 3.6 Vibrational modes where the arrows on the worksheet represent "inplane" vibrations, and the plus (+) and minus (-) symbols represent "out-of-plane" vibrations.

