

MESH QUALITY IMPROVEMENT BY RE-TRIANGULATION SURFACE MESHES ON 3-DIMENSIONAL CAD MODEL OF A HUMAN WRIST JOINT

Ву

LEONG MUN TEIK

Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia, in Fulfilment of the Requirements for the Degree of Master of Science

November 2018

FK 2018 192

All material contained within the thesis, including without limitation text, logos, icons, photographs and all other artwork, is copyright material of Universiti Putra Malaysia unless otherwise stated. Use may be made of any material contained within the thesis for non-commercial purposes from the copyright holder. Commercial use of material may only be made with the express, prior, written permission of Universiti Putra Malaysia.

Copyright © Universiti Putra Malaysia



Abstract of thesis presented to the Senate of Universiti Putra Malaysia in fulfilment of the requirement for the degree of Master of Science

MESH QUALITY IMPROVEMENT BY RE-TRIANGULATION SURFACE MESHES ON 3 DIMENSIONAL CAD MODEL OF A HUMAN WRIST JOINT

By

LEONG MUN TEIK

November 2018

Chairman: Tang Sai Hong, PhD Faculty: Engineering

With the recent advances computing technologies nowadays, reverse engineering is rapidly developing and has been strongly established many years in biomedical industry. Three dimensional geometric modeling is now being extensively used in many applications such as surgical planning, rapid prototyping, medical implants design, numerical simulation and etc. Thus, mesh quality is very crucial especially in finite element analysis in order to produce high accuracy results. Re-triangulation surface method is employed to improve the mesh quality of the model with certain parameters. The purpose of this study are a) to construct a complex three dimensional geometric CAD model of human wrist joint which contains cortical and cancellous bones using image-based processing method, b) to investigate the effects of triangle reduction, mesh smoothing and size of triangle mesh on the accuracy and mesh quality of the wrist bones model and c) to optimize the mesh quality using response surface methodology (RSM). A three dimensional CAD model of a human wrist joint was constructed after conversion model to non-uniform rational B-spline (NURBS). Re-triangulation process was carried out by manipulating different values of the parameters like geometrical error, smoothing factor and control edge length of triangle mesh along with mesh quality analysis in order to get high quality of mesh on the triangular surface wrist joint model. Lastly, optimization was performed via RSM to optimize the high quality mesh on the triangular surface model. In the findings, triangle reduction with geometrical error of 0.05 mm had reduced the number of triangles of cortical and cancellous bones to 74.81 % and 75.34 % respectively while obtained 70.05 % and 68.69 % of high quality of mesh on the surface model respectively. In term of accuracy, no significant changed in surface area and volume. For mesh smoothing effect, smoothing factor of 0.8 was selected to obtain 87.53 % and 86.68 % of high quality of mesh on cortical and cancellous bones respectively. For control size of triangle mesh, 0.5 mm of control edge length of triangle was taken to produce 92.35 % and 92.09 % for cortical and cancellous bones respectively. In term of accuracy of the model, the surface area and volume of the cortical and cancellous bones had no significant

changed with less than 0.15 % and 0.25 % compared to the initial bones model. In RSM optimization, the optimum mesh quality on cortical and cancellous bones were 90.74 % and 89.67 % respectively. In conclusions, the mesh quality and accuracy of the model show promising results with the process of re-triangulation surface and the high quality mesh of optimum models were obtained using RSM.



Abstrak tesis yang dikemukakan kepada Senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Master Sains

PENINGKATAN KUALITI JARINGAN DENGAN TRIANGULASI SEMULA JARINGAN SEGI TIGA PADA 3-DIMENSI CAD MODEL TULANG PERGELANGAN TANGAN MANUSIA

Oleh

LEONG MUN TEIK

November 2018

Pengerusi: Tang Sai Hong, PhD Fakulti : Kejuruteraan

Dengan kemajuan teknologi pengkomputeran pada masa kini, kejuruteraan balikan berkembang dengan pesat dan stabil dalam industri bioperubatan. Model 3 dimensi (3D)- geometri digunakan secara meluaskan dalam aplikasi seperti perancangan operasi, prototaip pantas, reka bentuk implant perubatan, simulasi berangka dan lain-lainnya. Dengan itu, kualiti jaringan memainkan peranan penting terutamanya dalam analisis unsur terhingga untuk menghasilkan keputusan yang mempunyai ketepatan yang tinggi. Kaedah triangulasi semula segi tiga pada permukaan dapat meningkatkan kualiti jaringan model dengan parameter tertentu. Tujuan kajian ini adalah a) untuk membina model 3 dimensi CAD kompleks pergelangan tangan manusia yang mengandungi tulang kortikal dan kanselus dengan menggunakan kaedah pemprosesan berasaskan imej, b) untuk menyiasat kesan pengurangan segitiga, melicinkan jaringan dan saiz jaringan segi tiga pada ketepatan dan kualiti jaringan darimodel tulang pergelangan tangan dan c) untuk mengoptimumkan kualiti jaringan dengan menggunakan kaedah gerak balas permukaan (RSM). CAD Model geometri tiga dimensi pergelangan tangan manusia dibina selepas diikuti dengan penukaran model kepada B-spline rasional yang tidak seragam (NURBS). Proses triangulasi semula dilakukan dengan memanipulasi nilai-nilai parameter yang berbeza termasuk ralat geometri, faktor pelicinan dan panjang pinggir segi tiga kawalan serta analisis kualiti jaringan untuk mendapatkan kualiti jaringan yang tinggi (ukuran bentuk segi tiga ≥ 0.8 merupakan ukuran kualiti jaringan yang tinggi) pada model sendi pergelangan. Akhir sekali, pengoptimuman dilakukan melalui RSM untuk mengoptimumkan kualiti jaringan segi tiga di permukaan model. Dalam kajian ini, pengurangan bilangan segi tiga, ralat geometri sebanyak 0.05 mm telah mengurangkan bilangan segitiga bagi tulang kortikal dan kanselus sebanyak 74.81 % dan 75.34 % masing-masing manakala 70.05 % dan 68.69 % menunjukkan kualiti jaringan pada model permukaan masing-masing. Dari segi ketepatan, tiada perubahan yang ketara di kawasan permukaan dan isi padunya.

Untuk kesan melicinkan jaringan, faktor pelicinan 0.8 dipilih untuk mendapatkan kualiti jaringan yang tinggi sebanyak 87.53 % dan 86.68 % bagi tulang kortikal dan kanselus. Bagi kawalan saiz segi tiga, panjang pinggiran kawalan 0.5 mm telah diambil untuk menghasilkan 92.35 % dan 92.09 % mewakili peratusan kualiti jaringan yang tinggi bagi tulang kortikal dan tulang kanselus. Dari segi ketepatan model, kawasan permukaan dan isi padu tulang kortikal dan kanselus menpunyai perubahan kurang daripada 0.15 % dan 0.25 % berbanding dengan model awal. Dalam pengoptimuman RSM, kualiti jaringan optimum bagi tulang kortikal dan kanselus adalah sebanyak 90.74 % dan 89.67 %. Kesimpulannya, kualiti jaringan dan ketepatan model menunjukkan hasil yang menjanjikan dengan proses triangulasi semula dan optimal model yang berkualiti tinggi didapati.



ACKNOWLEDGEMENTS

I would like to take this opportunity to express my sincere appreciation to my supervisor Associate Prof. Dr. Tang Sai Hong for his dedicated supervision and invaluable guidance throughout the research. Special thanks are extended to my co-supervisors Prof. Dr. Manohar Arumugam and Prof. Dr. Mohd. Khairol Anuar b. Mohd. Arrifin for their favorable helps and superb tolerance in the work.

Besides, I gratefully acknowledge to all those who had contributed to the success of this work directly or indirectly include all the staffs of Engineering Department and my family members for their continuously support and understanding especially my girlfriend Yew Sook Yan for taking care of me and always by my side whenever I feel lost and sad.

I would also like to apologize to those whom I brought troublesome to them for this 8 years master study.

Finally, I would like to thanks for the financial support from the University Putra Malaysia and the CT scan of human wrist bone from Hospital Serdang for the research purpose.

This thesis was submitted to the Senate of Universiti Putra Malaysia and has been accepted as fulfilment of the requirement for the degree of Master of Science. The members of the Supervisory Committee were as follows:

Tang Sai Hong, PhD

Associate Professor Faculty of Engineering Universiti Putra Malaysia (Chairman)

Manohar Arumugam, PhD

Professor Faculty of Medicine and Health Sciences Universiti Putra Malaysia (Member)

Mohd Khairol Anuar b. Mohd Arrifin, PhD

Profesor Ir. Faculty of Engineering Universiti Putra Malaysia (Member)

ZALILAH MOHD SHARIFF, PhD

Professor and Dean School of Graduate Studies Universiti Putra Malaysia

Date:13 February 2020

Declaration by Graduate Student

I hereby confirm that:

- this thesis is my original work;
- quotations, illustrations and citations have been duly referenced;
- this thesis has not been submitted previously or concurrently for any other degree at any other institutions;
- intellectual property from the thesis and copyright of thesis are fully-owned by Universiti Putra Malaysia, as according to the Universiti Putra Malaysia (Research) Rules 2012;
- written permission must be obtained from supervisor and the office of Deputy Vice-Chancellor (Research and Innovation) before thesis is published (in the form of written, printed or in electronic form) including books, journals, modules, proceedings, popular writings, seminar papers, manuscripts, posters, reports, lecture notes, learning modules or any other materials as stated in the Universiti Putra Malaysia (Research) Rules 2012;
- there is no plagiarism or data falsification/fabrication in the thesis, and scholarly integrity is upheld as according to the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) and the Universiti Putra Malaysia (Research) Rules 2012. The thesis has undergone plagiarism detection software.

-	
Cin	noturo
Sig	nature:

Date:

Name and Matric No.: Leong Mun Teik

Declaration by Members of Supervisory Committee

This is to confirm that:

- the research conducted and the writing of this thesis was under our supervision;
- supervision responsibilities as stated in the Universiti Putra Malaysia (Graduate Studies) Rules 2003 (Revision 2012-2013) are adhered to.

Signature: Name of Chairman of Supervisory Committee:	Assoc. Prof. Dr. Tang Sai Hong
Signature: Name of Member of Supervisory Committee:	Prof. Dr. Manohar Arumugam
Signature: Name of Member of Supervisory Committee:	Prof. Dr. Mohd. Khairol Anuar b. Mohd. Arrifin

TABLE OF CONTENTS

	Page
ABSTRACT	i
ABSTRAK	iii
ACKNOWLEDGEMENTS	V
APPROVAL	vi
DECLARATION	viii
LIST OF TABLES	xiii
LIST OF FIGURES	XV
LIST OF ABBREVIATIONS	xix

CHAPT		
1		
·	 1.1 Human Wrist Joint 1.1.1 Anatomy of the Wrist Joint 1.1.2 Common Wrist Problem 1.2 Computer-aided Reverse Engineering 	1 2 2 3
	 1.3 Three Dimensional Geometric Modeling 1.4 Type of Elements 	4 5
	1.5 Problem Statements1.6 Objectives1.7 Second Studies	5 7 7
	1.7 Scope of Study 1.8 Overview of the Study	7 8
2	LITERATURE REVIEW	
	2.1 Introduction2.2 Computer-aided Reverse Engineering	9 9
	2.2.1 Medical Reverse Engineering Methods 2.2.2 Reverse Engineering Software	10 12
	Classification 2.2.3 Biomechanics and Medical Applications	13
	2.3 Geometric Modeling 2.3.1 Human Wrist Joint	13 14
	2.3.2 Biological2.4 Mesh Quality Assessment of A Triangular Mesh	15 15
	 2.5 Re-triangulation (Re-meshing) Surface 2.6 Optimization Study via Response Surface Mathadalague (RSM) 	17 18
	Methodology (RSM) 2.7 Summary	20
3	METHODOLOGY	
	 3.1 Introduction 3.2 Reconstruction of the Human Wrist Joint Model 3.2.1 Image Data Acquisition 3.2.2 Segmentation 	23 25 26 26

		3.2.3 3D Surface Rendering and	28
	2.2	Stereolithography Conversion	20
	3.3	Three Dimensional CAD Model	30
		3.3.1 Mesh Surface Repair, Smoothing and	32
		Refinement	~ (
		3.3.2 NURBS Fitting and CAD Model	34
		Conversion	
	3.4	Re-triangulation	36
		3.4.1 Effect of Triangle Reduction	36
		3.4.2 Effect of Mesh Smoothing	38
		3.4.3 Effect of Control length of Triangle Mesh	39
	3.5	Optimization via Response Surface Methodology	41
		(RSM)	
		3.5.1 Analysis of Variance (ANOVA)	44
	3.6	Summary	46
4	RESU	JLTS AND DISCUSSION	
	4.1	Introduction	47
	4.2	Reconstruction of 3 D Human Wrist Joint Model	47
	4.3	Re-triangulation Surface For Cortical Bones and	49
		Cancellous Bones	
		4.3.1 Effect of Triangle Reduction	53
		4.3.1.1 Mesh Quality Evaluation	54
		4.3.1.2 Accuracy of Model Based on	60
		Surface Area and Volume	
		4.3.2 Effect of Mesh Smoothing	63
		4.3.2.1 Mesh Quality Evaluation	63
		4.3.2.2 Accuracy of Model Based on	66
		Surface Area and Volume	00
		4.3.3 Effect of Control Length of Triangle Mesh	68
		4.3.3.1 Mesh Quality Evaluation	68
		4.3.3.2 Accuracy of Model Based on	74
		Surface Area and Volume	74
	4.4	Response Surface Methodology (RSM)	77
	4.4	4.4.1 Cortical Bones	79
			79
		4.4.1.1 Development of Regression Model	79
			00
		4.4.1.2 Parameter Study	86
		4.4.1.3 Optimization of Mesh Quality	90
		4.4.2 Cancellous Bones	92
		4.4.2.1 Development of Regression	92
		Model	00
		4.4.2.2 Parameter Study	99
	4 -	4.4.2.3 Optimization of Mesh Quality	104
	4.5	Summary	105

5	CONCLUSION AND RECOMMENDATION FOR FUTURE RESEARCH	107
REFER	RENCES	109
APPEN	IDICES	115
BIODATA OF STUDENT		
LIST O	F PUBLICATIONS	



 (\mathbf{G})

LIST OF TABLES

	Table		Page
	3.1	Threshold values range for each properties	27
	3.2	Properties of cortical and cancellous bones in CAD model before re-triangulation	36
	3.3	Level of the re-triangulation variables for cortical and cancellous bones	42
	3.4	Design matrix of experiment for cortical and cancellous bones	45
	4.1	Number of triangles and percentage of mesh in different quality parameter	53
	4.2	Number of triangles for geometric error 0.01 mm – 1.00 mm	57
	4.3	Percentage of high quality mesh for geometry error 0.01 mm – 1.00 mm	57
	4.4	Number of triangles for geometric error 0.05 – 0.25 mm	58
	4.5	Percen <mark>tage of high quality mesh for geometric erro</mark> r 0.05 – 0.25 mm	58
	4.6	Percentage of high quality mesh for SF from 0.1 to 1.0	64
	4.7	Percentage of high quality mesh for CL from 0.50 to 2.50 mm	69
	4.8	Percentage of high quality mesh for CL from 0.50 to 2.50 mm	70
	4.9	Lowest and highest range of level for the parameters	79
	4.10	Design matrix of experiments and their respective simulation values and predicted values	80
	4.11	Sequential model sum of squares	81
	4.12	Analysis of variance (ANOVA) for response surface quadratic model	82
	4.13	Optimization criteria for re-triangulation process	91

4.14	Result of model validation at optimum condition	91
4.15	Design matrix of experiments and their respective simulation values and predicted values	93
4.16	Sequential model sum of squares	94
4.17	Analysis of variance (ANOVA) for response surface quadratic model	95
4.18	Optimization criteria for re-triangulation process	104
4.19	Result of model validation at the optimum condition	104



 \bigcirc

LIST OF FIGURES

Fiç	gure		Page
1		Palmar view of the right wrist showing anatomical directions and rotations	1
1	1.2	a) wrist joint features b) bones c) X-ray image view	2
1		A flowchart for modeling 3D triangle mesh models with different scan data input a)Point cloud data as the input and b) 2D scan images as the input	4
1	1.4	Type of different elements available	5
2		Comparison processes between class production and reverse engineering	9
2		MRE methods-Fundamental processes and information flow	11
2	2.3	Quality parameter of triangular mesh	17
з	3.1	Overall work flow for the study	23
3	3.2	Work flow for reconstruction of the wrist joint model	25
3		Highlighted areas according to the range of threshold values for the cortical bones	27
3		Orange and blue segmented lines represents cortical and cancellous bones respectively	29
з	3.5	Palmer view of the 3D geometric wrist joint model	29
3		Palmer view of cortical bones and cancellous bones of the 3D geometric wrist joint model	30
З	3.7	Chart of construction of 3D NURBS CAD model	31
з	3.8	Rough and bad triangular surface mesh (highlighted)	33
(6) 3		Comparison between a) before and b) after mesh surface repair, smoothing and refinement	34
3.	.10	NURBS patches on the wrist joint model	35
3	.11	Grids generated on the wrist bones model	35

3.12	Chart of triangle reduction in re-triangulation process	37
3.13	Chart of mesh smoothing in re-triangulation process	39
3.14	Chart of mesh refinement in re-triangulation process	40
3.15	Chart of optimization via RSM	42
4.1	(a) Bad edges of triangles(b) Intersection of triangles	48
4.2	Triangular surfaces on CAD model	48
4.3	CAD model for (a) cortical bones (b) cancellous bones	49 50
4.4	Histogram of mesh quality for cortical bones of the initial model	51
4.5	Histogram of mesh quality for cancellous bones of the initial model	51
4.6	Hamate's initial mesh model for (a) Cortical bone (b) Cancellous bone	52
4.7	Histogram of mesh quality for cortical bones when GE = 0.05 mm	54
4.8	Histogram of mesh quality for cancellous bones when $GE = 0.05 \text{ mm}$	55
4.9	Hamate's mesh model when GE = 0.05 mm for (a) cortical bone (b) cancellous bone	55
4.10	Correlation between reduction in the number of triangles and percentage of high quality mesh of cortical and cancellous bones for geometric error 0.01 – 1.00 mm	56
4.11	Correlation between reduction in the number of triangles and percentage of high quality mesh of cortical and cancellous bones for geometric error 0.05 – 0.25 mm	59
4.12	Surface area of bones versus geometric error from 0.00 to1.00 mm	60
4.13	Volume of bones versus geometric error from 0.00 to 1.00 mm	61

	4.14	Surface area of bones versus geometric error from 0.05 to 0.25 mm	62
	4.15	Volume of bones versus geometric error from 0.05 to 0.25 mm	62
	4.16	Percentage of high quality mesh of bones versus smoothing factor	64
	4.17	Histogram of mesh quality for cortical bones when GE = 0.05 mm and SF= 0.80	65
	4.18	Histogram of mesh quality for cancellous bones when $GE = 0.05 \text{ mm}$ and $SF=0.80$	65
	4.19	Hamate's mesh model when GE= 0.05 mm and SF =0.80 for a) cortical bone b) cancellous bone	66
	4.20	Surface areas of bones versus smoothing factor	67
	4.21	Volume of bones versus smoothing factor	68
	4.22	Percentage of high quality mesh versus control length (0.50 to 2.50 mm)	69
	4.23	Percentage of high quality mesh versus control length (0.20 to 0.50 mm)	71
	4.24	Histogram of mesh quality for cortical bones when GE = 0.05 mm, SF =0.80 and CL=0.50 mm	72
	4.25	Histogram of mesh quality for cancellous bones when GE = 0.05 mm, SF =0.80 and CL=0.50 mm	72
	4.26	Hamate's mesh model when GE= 0.05 mm, SF =0.80 and CL=0.50 mm for a) cortical bone b) cancellous bone	73
	4.27	Close-up view of cortical bones (GE= 0.05 mm, SF =0.80 and CL=0.50 mm)	73
	4.28	Close-up view of cancellous bones (GE= 0.05 mm, SF =0.80 and CL=0.50 mm)	74
\bigcirc	4.29	Surface areas of bones versus control length (0.00 to 2.5 mm)	75
	4.30	Volume of bones versus control length (0.00 to 2.5 mm)	75
	4.31	Surface areas of bones versus control length (0.00 to 0.50 mm)	76

4.32	Volume of bones versus control length (0.00 to 0.50 mm)	77
4.33	Predicted versus actual percentage of high quality mesh	84
4.34	Normal probability plot of the residuals	85
4.35	Plot of the residuals versus the predicted response	85
4.36	Perturbation plot	86
4.37	a) Contour plot and b) 3D response plot of mesh quality (effect of GE (A) and SF (B), CL = 0.85 mm)	87 87
4.38	a) Contour plot and b) 3D response plot of mesh quality (effect of SF (B) and CL (C), GE = 0.35 mm)	88 89
4.39	a) Contour plot and b) 3D response plot of mesh quality (effect of GE (A) and CL (C), SF = 0.65)	89 90
4.40	Predicted versus actual percentage of high quality mesh	97
4.41	Normal plot of residuals	97
4.42	Plot of the residuals versus the predicted response	98
4.43	Perturbation plot	99
4.44	a) Contour plot and b) 3D response plot of mesh quality (effect of GE (A) and SF (B), CL = 0.85 mm)	100 100
4.45	a) Contour plot and b) 3D response plot of mesh quality (effect of SF (B) and CL (C), GE = 0.35 mm)	101 102
4.46	a) Contour plot and b) 3D response plot of mesh quality (effect of GE (A) and CL (C), SF = 0.65)	103 103

LIST OF ABBREVIATONS

	mm	Millimetres
	λ	Wavelength
	%	Percentage
	R ₁	Radius of inscribed circle
	R ₂	Radius of ascribed circle
	2D	Two dimensional
	3D	Three dimensional
	GE	Geometrical error
	SF	Smoothing factor
	CL	Control edge length
	CAD	Computer-Aided Design
	CAM	Computer-Aided Manufacturing
	CAE	Computer-Aided Engineering
	CARE	Computer-Aided Reverse Engineering
	MRE	Medical reverse engineering
	FEA	Finite Element Analysis
	CFD	Computational Fluid Dynamics
	NURBS	Non-uniform Rational B-spline
	STL	Stereolithography
	VRML	Virtual Reality Modeling Language
	DXF	Drawing Exchange Format

- RSMResponse Surface MethodologyCTComputerized TomographyREReverse engineeringRPRapid prototypingIGESInitial Graphics Exchange SpecificationVDAVerband der Automobilindustrie
- STEP Standard for the Exchange of Product Data
- DICOM Digital Imaging and Communications in Medicine
- ROI Range of interest
- NC Numerical control
- RSM Response Surface Methodology
- ANOVA Analysis of Variance
- CCD Central Composite Design
- k Number of control variables
- F Ratio between the mean square
- p Probability of error value
- R² Coefficient of determination
- S/N Signal to noise ratio

CHAPTER 1

INTRODUCTION

1.1 Human Wrist Joint

The human wrist joint is an essential joint of the upper extremity and plays a significant role in maintaining a normal daily life. It links the forearm to the hand. Unlike others bones joint like hip, elbow, shoulder, ankle and knee, wrist joint is one of the most complex joint in the anatomy of human. A healthy wrist joint should able to perform a normal functional range of motion. These movements of the wrist joint are separated into three categories which flexion-extension, radial-ulna deviation and forearm pronation-supination. Figure 1.1 illustrates these three degrees of freedom.

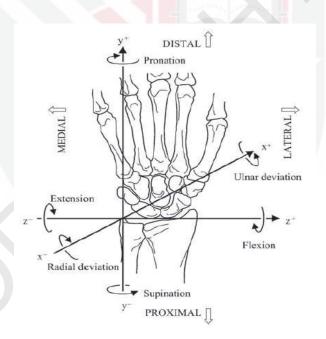


Figure 1.1 : Palmar view of the right wrist showing anatomical directions and rotations (SirkettMullineux *et al.*, 2004)

1.1.1 Anatomy of Wrist Joint

Wrist joint comprises of multiple articulations of the eight carpal bones with the distal radius and ulna. The carpal bones are separated into two rows, which are the proximal and distal. The proximal row is formed by scaphoid, lunate, pisiform and triquetrum while the distal row consists of trapezoid, trapezium, hamate and capitate (Bajuri & Kadir, 2012; Gislason et al., 2009).

The wrist consists of three main joints which are midcarpal joint, radiocarpal joint and distal radioulnar joint. The most movement and critical articulation in the joint is the radiocarpal joint, which is a synovial articulation formed by the distal end of the radius and the scaphoid, lunate and triquetrum (Bajuri & Kadir, 2012; Shepherd & Johnstone, 2002, 2005).

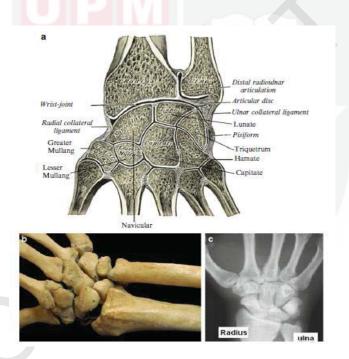


Figure 1.2 : (a) Wrist joint features; (b) the bones; and (c) the X-ray view (Pal, 2014)

1.1.2 Common Wrist Problems

The most common causes of wrist pain are due to highly frequency, duration and intensity activities. For examples, certain leisure, and working activities such as typing, sewing, cooking, and etc. in longer period and same routine of movements may be the factors that cause in wrist pain. Wrist injuries that caused by sudden impacts may leads to bone fracture. Besides that, wrist injuries are

very common in many sports; either involves repetitive stress or impacts. These sports can be consisting of boxing, rugby, badminton, tennis, golf, bowling and etc. (Pereira, 2015). Also, some wrist fractures are caused by osteoporosis. In other hand, sprains and strains, tendinitis, arthritis and gout are the common causes of wrist pain.

Meanwhile, Rheumatoid Arthritis is the most common skeletal disease occurred in the wrist joint (Bajuri *et al.*, 2011; Stegeman *et al.*, 2005). Patients with this wrist disease suffered severe pain, deformity and unable to perform normal range of motion. Due to the weakened and damaged ligaments, articular cartilages, tendons, joint capsule and together with eroded bones which unable to full support within the bones, eventually the wrist joint becomes unstable (Bajuri, et al., 2011; Shepherd & Johnstone, 2002; Stegeman, et al., 2005).

1.2 Computer-aided Reverse Engineering

The process of engineering mainly focuses in designing, manufacturing, assembling and maintaining systems and products. Engineering can be divided into two types: forward engineering (FE) and reverse engineering (RE). The definition of the terms FE and RE are strongly dependent on the end-use applications and the field of study. Forward engineering usually can be defined as the conventional process of building an original part or total product with own ideas, innovative and logically. Meanwhile, reverse engineering is another way round. It can be defined as a process of duplicating and existing part, subassembly or product, without any technical details such as drawings, bill-of-material, or without engineering data (Chikofsky & Cross, 1990; Hieu, et al., 2010; Raja & Fernandes, 2007; Wang, 2011).

Reverse engineering is a multidisciplinary applied science and almost can be applicable to every case of fields (Wang, 2011). It is now widely used in many areas such as industrial, design and manufacturing, automotive, artistic and architectural, software engineering and biomedical (Raja & Fernandes, 2007; Šagi *et al.*, 2015; Wang, 2011). In terms of cost and time consuming, this method is more preferable than the conventional engineering because it is less expensive and time saving in designing part especially in creating a complex geometrical model (Raja & Fernandes, 2007; Šagi, et al., 2015). According to authors, the definition of computer-aided reverse engineering is a technique to create a geometric 3-D model by digitizing the scanned data to form multiple 3-D points or re-triangulate mesh from the scanned object (Raja & Fernandes, 2007). This process can be described as follow in Figure 1.3.

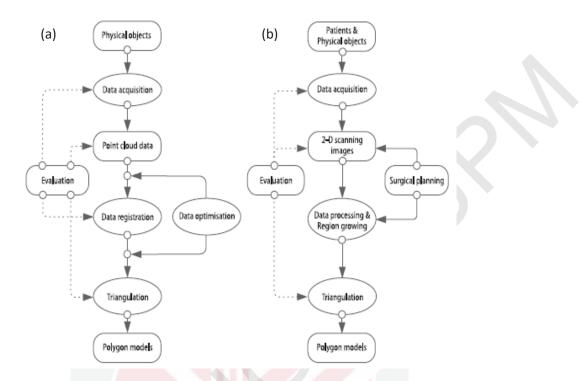


Figure 1.3 : A flowchart for modeling 3D triangular mesh models with different scan data input. (a) Point cloud data as the input. (b) 2-D scan images as the input (Raja & Fernandes, 2007)

1.3 Three Dimensional Geometric Modeling

A three dimensional (3D) geometric model is a digital representation consists of geometry data information formed in virtual environment which can be then used by computer-aided design, manufacturing and engineering (CAD/CAM/CAE) applications (Relvas *et al.*, 2011; Šagi, et al., 2015). 3D geometric modeling has been widely used in biomedical with the aid of reverse engineering. Generally, patient data or biomedical objects are required in the modeling of 3D geometric models. The reconstruction of 3D models normally involved anatomical structure, tissues organs, medical implants, surgical planning and biomedical research (Hieu *et al.*, 2010; Šagi, et al., 2015).

Before 3D geometric modeling of the object is ready for visualization, data exchange or manufacturing applications, the geometrical model has to be discretized into a 3D polygons mesh or NURBS mesh either from the input of point clouds or 2D image planes. For data exchange, different output files are converted for different applications purposes. (Bénière *et al.*, 2013; Hieu, *et al.*, 2010).

1.4 Type of Elements

There are many type elements available such as triangle and quadrilateral as surface mesh in 2D while tetrahedron, hexahedron, pyramid, prism with triangular base and arbitrary polyhedron as solid mesh in 3D. Figure 1.4 shows different type of elements available.

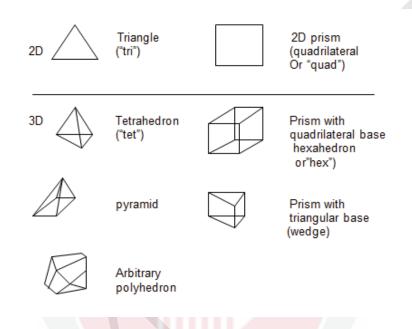


Figure 1.4 : Type of different elements available (Bakker, 2013)

Triangle is the simplest polygon that formed with three vertices and three edges connected to each other. Triangular surface mesh is more prefer in geometric modeling because of its properties to represent geometries of objects (Hieu, *et al.*, 2010). Besides that, it can easily converts to tetrahedral mesh. Due to its simple, flexible and quite strong adaptability to complicated boundaries properties, tetrahedral mesh are widely used to modeling complex geometries objects for numerical simulations (Sun *et al.*, 2010).

1.5 Problem Statements

The human wrist joint is one of the most complex joint bones that play a significant role in maintaining normal daily life activities. Although there have been extensive research into the anatomy of the wrist and its separates components, the biomechanics of the wrist still has a long way to study and understood deeply. Developing a 3 dimensional wrist joint remains high

challenges due to the complex geometry, large amount of articulations, nonlinear properties of supporting soft tissue structures and the inter-relationship between all of these components. Therefore, there was noticeably lack of literature concerning wrist joint finite element modeling compared to other simple joint bones. Additionally, software and hardware computational speed was one of the factors leads to less research studies on this field for past decades (Gíslason *et al.*, 2010).

With the advanced technology recently, reverse engineering was introduced to the biomechanical industry, creating a full, geometrically accurate and models are more feasible using medical image processing method. However, (Hieu, *et al.*, 2010) claimed that it was hard to adequately meet the requirements in data processing and geometrical modeling works with a single software. Consequently, it depends on the end-use application on the selection of the software because the processes of geometrical modeling and data exchange among the packages are very complex (Hieu, *et al.*, 2010).

The authors claimed that converting triangular surface mesh to tetrahedral (solid mesh) outside finite element solver was way easily and better control of the density and quality of the surface mesh. Besides, less works to be done after imported the model into finite element solver. Hence, this made the process more time saving without losing the geometrical integrity (Gíslason, *et al.*, 2010).

A tetrahedral mesh is basically formed by using a triangular mesh boundary and fill in with volume. If a self-intersection occurred in the boundary of triangular mesh, the mesh could not performed a well-defined volumetric mesh, and the tetrahedral mesh generator may create severely distorted elements or even fail to create a mesh at all. Therefore, it is necessarily to remove a self-intersection in a triangular mesh (Yamakawa & Shimada, 2009).

Moreover, most of scanned geometry model generated by using image-based method were saved in stereolithography (STL) file format often contained irregular, highly skewed and too dense of triangles. Such triangulation effectively prevents the creation of a good volume mesh. Improper surface mesh could not be used in numerical analysis such as finite element analysis (FEA) and computational fluid dynamics analysis (CFD) because of the mesh quality of the triangles were not sufficient to run an accurate simulation analysis (Magne, 2007).

1.6 Objectives

The aim of the study is to develop a complex 3D geometric CAD model of human wrist joint with high quality triangular surface meshes for future numerical simulation research purpose.

The objectives of this study are as follows:

- 1. To construct 3D human wrist joint CAD model which contained cortical and cancellous bones using image-based processing method.
- 2. To investigate the effects of triangle reduction, mesh smoothing and control size of triangle mesh with respect to the accuracy and mesh quality of the wrist joint model.
- 3. To optimize high quality triangular mesh using response surface methodology (RSM).

1.7 Scope of Study

First, all of the experiments in this research were performed using computational commercials software only. The commercials software that are 3D Doctor (Able Software Corp), Geomagic studio (Raindrop Inc.), Materialise 3-matic (Materialise, NV Belgium) and Design Expert 6.0 (Stat-Ease). No experiment in vivo was tested in the research. Only CT-scan data of a human wrist joint was used as resource in developing a 3D geometric wrist joint model. The CT-scan data was provided from Hospital Serdang, Selangor. The human wrist joint was assumed to be natural and healthy. The reconstruction of the geometric wrist joint model was only involved bones. Other tissues like cartilages and ligaments were neglected. The geometric wrist joint model was a triangular surface mesh model which means it was a shell model. Algorithms development and generation of volumetric mesh were not involved in this research. Mainly, this research was focused on calculations of mesh quality based on radius ratios of the triangle quality metric which found in computer software (Materialise 3-Matic). The re-triangulation parameters that are used in the study are geometrical error. smoothing factor and control length of a triangle which also provided in the computer software (Materialise 3-Matic). In order to preserve for good quality mesh, the parameters setting for re-triangulation process was set at 0.4 in the Materialise 3-Matic software so that mesh quality below 0.4 will not create on the 3D CAD model. Mesh quality of a triangle below radius ratios of 0.4 (<0.4) is considered low quality mesh while mesh quality of a triangle equal or above 0.7 to 1.0 (0.7 \leq mesh quality \leq 1.0) is considered as high quality mesh. Mesh convergence study was out of the scope of this study. For future research, this model can be used for finite element analysis simulation by converting it into volumetric mesh model.

1.8 Overview of the Study

In chapter one, a brief introduction is described about the human wrist joint, computer-aided reverse engineering, three dimensional geometric modeling, definition of triangulation mesh and mesh quality. In chapter two, previous studies related to the geometrical modeling using reverse engineering method and its biological applications are reviewed. Besides that, this chapter is also reviewed some previous works related on modeling of human wrist joint and other joint like knee, hip, ankle, shoulder, etc. On the other hand, mesh quality assessment of a triangular mesh, re-triangulation method and optimization study via response surface methodology are discussed in details.

Next, in chapter three it begins with a brief introduction about the research methodology and then by describing the work flow of reconstruction of human wrist joint model. In the subsequent experiments, three dimensional CAD modeling using NURBS fitting method after the surface model is repaired, smoothed and refined. After that, Re-triangulation process is taken place with the effects of triangle reduction, mesh smoothing and control size of triangle mesh. Optimization via response surface methodology is employed in the final of this chapter.

In chapter 4, results throughout the study are discussed in particular. It begins with the reconstruction of 3D human wrist bones model. Then it follows by the discussion about the influences of triangle reduction, mesh smoothing and control size of triangle mesh in aspects of mesh quality and validation of the model based on surface area and volumes after re-triangulation process process. Lastly, findings in the development of regression model, parameter study and optimization of mesh quality via response surface methodology for each cortical and cancellous bones are discussed in details.

In the final chapter, conclusion of the study is made and possible recommendation for future research is listed.

REFERENCES

- Ahn, D.G., Lee, J.Y., & Yang, D.Y. (2006). Rapid prototyping and reverse engineering application for orthopedic surgery planning. *Journal of mechanical science and technology*, 20(1), 19-28.
- Alaswad, A., Benyounis, K. Y., & Olabi, A. G. (2011). Employment of finite element analysis and Response Surface Methodology to investigate the geometrical factors in T-type bi-layered tube hydroforming. *Advances in Engineering Software, 42*(11), 917-926.
- Alsufyani, N., Hess, A., Noga, M., Ray, N., Al-Saleh, M., Lagravère, M., & Major, P. (2016). New algorithm for semiautomatic segmentation of nasal cavity and pharyngeal airway in comparison with manual segmentation using conebeam computed tomography (Vol. 150).
- Anderson, D. D., Goldsworthy, J. K., Wendy, L., Rudert, M. J., Tochigi, Y., & Brown, T. D. (2007). Physical Validation of a Patient-Specific Contact Finite Element Model of the Ankle. *Journal of Biomechanics*, 40(8), 1662-1669.
- Anuar, N., Mohd Adnan, A. F., Muhammad Naziz, S., Aziz, N., & Taha, R. (2013). Optimization of Extraction Parameters by Using Response Surface Methodology, Purification, and Identification of Anthocyanin Pigments in Melastoma malabathricum Fruit (Vol. 2013).
- Bajuri, M. N., Abdul Kadir, M. R., & Yahya, M. Y. (2011). Biomechanical Analysis on the Effect of Bone Graft of the Wrist after Arthroplasty. In: Osman N.A.A., Abas W.A.B.W., Wahab A.K.A., Ting HN. (eds) 5th Kuala Lumpur International Conference on Biomedical Engineering 2011. IFMBE Proceedings, vol 35. Springer, Berlin, Heidelberg.
- Bajuri, & Kadir. (2012). Computational biomechanics of the wrist joint. Springer Science & Business Media.
- Bakker, A., 2013. Lecture 7 Meshing, Applied Computational Fluid Dynamics. http://www.bakker.org/dartmouth06/engs150/07-mesh.pdf. (last accessed: 05.1.16).
- Bardyn, T., Reyes, M., Larrea, X., & Büchler, P. (2010). Influence of Smoothing on Voxel-Based Mesh Accuracy in Micro-Finite Element.
- Baş, D., & Boyacı, İ. H. (2007). Modeling and optimization I: Usability of response surface methodology. *Journal of Food Engineering*, *78*(3), 836-845.
- Bénière, R., Subsol, G., Gesquière, G., Le Breton, F., & Puech, W. (2013). A comprehensive process of reverse engineering from 3D meshes to CAD models. *Computer-Aided Design*, 45(11), 1382-1393.

- Bezerra, M. A., Santelli, R. E., Oliveira, E. P., Villar, L. S., & Escaleira, L. A. (2008). Response surface methodology (RSM) as a tool for optimization in analytical chemistry. *Talanta*, *76*(5), 965-977.
- Botsch, M., Pauly, M., Rossl, C., Bischoff, S., & Kobbelt, L. (2006). Geometric modeling based on triangle meshes. Paper presented at the ACM SIGGRAPH 2006 Courses, Boston, Massachusetts.
- Burkhart, T. A., Andrews, D. M., & Dunning, C. E. (2013). Finite element modeling mesh quality, energy balance and validation methods: A review with recommendations associated with the modeling of bone tissue. *Journal of Biomechanics*, 46(9), 1477-1488.
- Chen, X., Du, W., & Liu, D. (2008). Response surface optimization of biocatalytic biodiesel production with acid oil (Vol. 40).
- Cheng, Y. L., & Chen, S. J. (2006). Manufacturing of Cardiac Models Through Rapid Prototyping Technology for Surgery Planning. *Materials Science Forum*, 505-507, 1063-1068.
- Chikofsky, E. J., & Cross, J. H. (1990). Reverse engineering and design recovery: a taxonomy. *IEEE Software*, 7(1), 13-17.
- Daskalaki, A., Lobos, C., Payan, Y., & Hitschfeld, N. (2010). Techniques for the Generation of 3D Finite Element Meshes of Human Organs.
- Djoudi, F. (2013). 3D reconstruction of bony elements of the knee joint and finite element analysis of total knee prosthesis obtained from the reconstructed model. *Journal of Orthopaedics, 10*(4), 155-161.
- Doyle, B., Sun, Z., Jansen, S., & Norman, P. (2015). Commentary: Computational Modeling of Contemporary Stent-Grafts. *Journal of Endovascular Therapy*, 22(4), 591-593.
- Dúbravčík, M., & Kender, Š. (2012). Application of Reverse Engineering Techniques in Mechanics System Services. *Procedia Engineering*, 48, 96-104.
- Garimella, R. V., Shashkov, M. J., & Knupp, P. M. (2004). Triangular and quadrilateral surface mesh quality optimization using local parametrization. *Computer Methods in Applied Mechanics and Engineering*, 193(9), 913-928.
- Gelaude, F., Vander Sloten, J., & Lauwers, B. (2006). Semi-automated segmentation and visualisation of outer bone cortex from medical images. *Computer Methods in Biomechanics and Biomedical Engineering*, *9*(1), 65-77.

- Gislason, M. K., Nash, D. H., Nicol, A., Kanellopoulos, A., Bransby-Zachary, M., Hems, T., Stansfield, B. (2009). A three-dimensional finite element model of maximal grip loading in the human wrist. *Proceedings of the Institution of Mechanical Engineers, Part H: Journal of Engineering in Medicine, 223*(7), 849-861.
- Gíslason, M. K., Stansfield, B., & Nash, D. H. (2010). Finite element model creation and stability considerations of complex biological articulation: the human wrist joint. *Medical engineering & physics*, *32*(5), 523-531.
- González-Carbonell, R. A., Ortiz-Prado, A., Jacobo-Armendáriz, V. H., Cisneros-Hidalgo, Y. A., & Alpízar-Aguirre, A. (2015). 3D patient-specific model of the tibia from CT for orthopedic use. *Journal of Orthopaedics*, 12(1), 11-16.
- Hieu, L.C., Sloten, J.V., Hung, L.T., Khanh, L., Soe, S., Zlatov, N., Phuoc, L.T., Trung, P.D. (2010). Medical Reverse Engineering Applications and Methods. Paper presented at the In: 2nd international conference on innovations, recent trends and challenges in mechatronics, mechanical engineering and new high-tech products development MECAHITECH, Bucharest.
- Khuri, A., & Mukhopadhyay, S. (2010). Response Surface Methodology (Vol. 2).
- Knupp, P. M. (2001). Algebraic Mesh Quality Metrics. SIAM J. Sci. Comput., 23(1), 193-218.
- Lobos, C., Payan, Y., & Hitschfeld, N. (2009). Techniques for the generation of 3D Finite Element Meshes of human organs.
- Magne, P. (2007). Efficient 3D finite element analysis of dental restorative procedures using micro-CT data. *Dental Materials*, 23(5), 539-548.
- Maintz, T. (2005). Digital and Medical Image Processing. Utrecht University.
- Myers, R. H., Montgomery, D. C. (2002). Response Surface Methodology: Process and Product Optimization Using Designed Experiments. 2nd ed. New York: John Wiley & Sons.
- Mohammad, V., Chee Kai, C., & Siaw Meng, C. (2012). Improving the process of making rapid prototyping models from medical ultrasound images. *Rapid Prototyping Journal*, 18(4), 287-298.
- Mohan, S. K., Viruthagiri, T., & Arunkumar, C. (2014). Statistical optimization of process parameters for the production of tannase by *Aspergillus flavus* under submerged fermentation. *3 Biotech, 4*(2), 159-166.
- Montgomery, D. (2000). Design and Analysis of Experiments, 5th edition., *Wiley, New York*.
- Morten Enemark, L., Mark de, Z., Michael Skipper, A., & John, R. (2012). On validation of multibody musculoskeletal models. *Proceedings of the Institution*

of Mechanical Engineers, Part H: Journal of Engineering in Medicine, 226(2), 82-94.

- Mourabet, M., Abdelhadi, E. R., El Boujaady, H., Bennani-Ziatni, M., & Abderrahim, T. (2014). Use of response surface methodology for optimization of fluoride adsorption in an aqueous solution by Brushite (Vol. 217).
- Ohtake, Y., Belyaev, A., & Bogaevski, I. (2001). Mesh regularization and adaptive smoothing. *Computer-Aided Design*, *33*(11), 789-800.
- Pal, Ravi, Bhargava, & Chandrasekhar. (2006). Computer-Aided Reverse Engineering for Rapid Replacement Parts: A Case Study (Vol. 56).
- Pal, S. (2014). The Wrist Joint and Its Artificial Replacement Design of Artificial Human Joints & Organs (pp. 159-166). *Boston, MA: Springer US*.
- Peng, L., Junfang, N., Yong, Z., Wen, Z., & Dinghua, J. (2011). Construction of 3D Finite Element Model of Upper End of Tibia (Vol. 1).
- Pereira, E. (2015). Evaluation of the Painful Wrist. In W. B. Geissler (Ed.), *Wrist and Elbow Arthroscopy: A Practical Surgical Guide to Techniques* (pp. 29-35). New York, NY: Springer New York.
- Pham D., Hieu L. (2008) Reverse Engineering–Hardware and Software. In: Raja V., Fernandes K. (eds) Reverse Engineering. Springer Series in Advanced Manufacturing. Springer, London
- Qin, H., & Terzopoulos, D. (1997). Triangular NURBS and their dynamic generalizations. *Computer Aided Geometric Design*, 14(4), 325-347.
- Raja, V., & Fernandes, K. J. (2007). Reverse engineering: an industrial perspective: Springer Science & Business Media.
- Relvas, C., Ramos, A., Completo, A., & Simões, J. A. (2011). Accuracy control of complex surfaces in reverse engineering. *International Journal of Precision Engineering and Manufacturing*, 12(6), 1035-1042.
- Roy, S. (2013). *15.* A Review on Automated Brain Tumor Detection and Segmentation from MRI of Brain.
- Šagi, G., Lulić, Z., & Mahalec, I. (2015). Reverse Engineering. In J. Stjepandić, N. Wognum & W. J.C. Verhagen (Eds.), *Concurrent Engineering in the 21st Century: Foundations, Developments and Challenges* (pp. 319-353). Cham: Springer International Publishing.
- Salamatinia, B., Mootabadi, H., Bhatia, S., & Abdullah, A. Z. (2010). Optimization of ultrasonic-assisted heterogeneous biodiesel production from palm oil: A response surface methodology approach. *Fuel Processing Technology*, 91(5), 441-448.

- Shepherd, & Johnstone. (2002). Design considerations for a wrist implant. *Medical engineering & physics, 24*(10), 641-650.
- Shepherd, & Johnstone. (2005). A new design concept for wrist arthroplasty. Proceedings of the Institution of Mechanical Engineers, Part H: Journal of Engineering in Medicine, 219(1), 43-52.
- Shuit, S. H., Lee, K. T., Kamaruddin, A. H., & Yusup, S. (2010). Reactive Extraction of *Jatropha curcas L*. Seed for Production of Biodiesel: Process Optimization Study. *Environmental Science & Technology*, 44(11), 4361-4367.
- SirkettMullineux, Giddins, & Miles. (2004). A kinematic model of the wrist based on maximization of joint contact area. *Proceedings of the Institution of Mechanical Engineers, Part H: Journal of Engineering in Medicine, 218*(5), 349-359.
- Stegeman, M., Rijnberg, W. J., & van Loon, C. J. M. (2005). Biaxial total wrist arthroplasty in rheumatoid arthritis. Satisfactory functional results. *Rheumatology International*, 25(3), 191-194.
- Sun, Bao, & Liu. (2010, 10-12 Dec. 2010). Smoothing Algorithm for Tetrahedral Meshes by Error-Based Quality Metric. International Conference on Computational Intelligence and Software Engineering.
- Sun, W., Darling, A., Starly, B., & Nam, J. (2004). Computer aided tissue engineering: overview, scope and challenges. *Biotechnology and applied biochemistry*, *39*(1), 29-47.
- Thornburg, H. (2012). Overview of the PETTT Workshop on Mesh Quality/Resolution, Practice, Current Research, and Future Directions *50th AIAA Aerospace Sciences Meeting including the New Horizons Forum and Aerospace Exposition*: American Institute of Aeronautics and Astronautics.
- Wang, W. (2011). Reverse engineering—technology of reinvention. *Boca Raton: CRC Press.*
- Yamakawa, S., & Shimada, K. (2009). Removing self intersections of a triangular mesh by edge swapping, edge hammering, and face lifting *Proceedings of* the 18th International Meshing Roundtable (pp. 13-29): Springer.
- Yazdanpanah, M., Khanmohammadi, M., Mehdinavaz Aghdam, R., Shaabani Lakeh, K., & Rajabi, M. (2014). Optimization of electrospinning process of poly(vinyl alcohol) via response surface methodology (RSM) based on the central composite design (Vol. 3).
- Zheng, Y., Lewis, R. W., & Gethin, D. T. (1996). Three-dimensional unstructured mesh generation: Part 2. Surface meshes. *Computer Methods in Applied Mechanics and Engineering*, 134(3), 269-284.

Zong, Z., Lin, X., & Niu, J. (2015). Finite element model validation of bridge based on structural health monitoring—Part I: Response surface-based finite element model updating. *Journal of Traffic and Transportation Engineering (English Edition),* 2(4), 258-278.

